

# Beat-to-beat variability of repolarisation and drug-induced torsades de pointes in the canine heart

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Beat-To-Beat Variability of  
Repolarisation and  
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in the Canine Heart

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# Beat-To-Beat Variability of Repolarisation and Drug-Induced Torsades de Pointes in the Canine Heart

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Morten Bækgaard Thomsen



*Promotor:*

Prof. dr. Marc A. Vos

*Co-promotores:*

Dr. Paul G.A. Volders

Dr. Jørgen Matz (Denmark)

*Beoordelingscommissie:*

Prof. dr. Harry A.J. Struijker Boudier (voorzitter)

Prof. dr. Maurits A. Allesie

Prof. dr. Harry J.G.M. Crijns

Prof. dr. Dan M. Roden (Vanderbilt University Medical Center, USA)

Prof. dr. Christian Torp-Pedersen (Copenhagen University Hospital, Denmark)

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# Content

7	<b>Chapter 1:</b> General introduction
35	<b>Chapter 2:</b> Electrophysiological Safety of Sertindole in Dogs with Normal and Remodeled Hearts
57	<b>Chapter 3:</b> Increased Short-Term Variability of Repolarization Predicts <i>d</i> -Sotalol-Induced Torsades de Pointes in Dogs
75	<b>Chapter 4:</b> Decreasing the Infusion Rate Reduces the Proarrhythmic Risk of NS-7
93	<b>Chapter 5:</b> Sudden Cardiac Death in Dogs with Remodeled Hearts is Associated with Larger Beat-To-Beat Variability of Repolarization
113	<b>Chapter 6:</b> Beat-to-Beat Variability of Repolarization Determines Proarrhythmic Outcome in Dogs Susceptible to Drug-Induced Torsades de Pointes
131	<b>Chapter 7:</b> General Discussion
153	English Summary
157	Nederlandse Samenvatting
161	Dansk Resumé
165	Acknowledgements
169	Curriculum vitae
171	Publications



# General Introduction

## *Content:*

Drug-induced proarrhythmia  
Current state of non-clinical proarrhythmia assessment  
Available test systems  
Need for additional proarrhythmia parameters  
Aim of the thesis

This chapter is the basis of a review in preparation by: Morten B. Thomsen<sup>1,2</sup>,  
Jørgen Matz<sup>3</sup>, Paul G.A. Volders<sup>2</sup> and Marc A. Vos<sup>1</sup>

1. Department of Medical Physiology, Heart Lung Center Utrecht, University Medical Center Utrecht, Utrecht, Netherlands.
2. Department of Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands.
3. Center of Excellence, Cardiovascular Research, H. Lundbeck, Copenhagen, Denmark.



## Drug-induced proarrhythmia

A large number of pharmaceutical compounds have been associated with torsades de pointes arrhythmias.<sup>1,2</sup> The spectrum of drugs involves antiarrhythmic drugs, non-antiarrhythmic cardiovascular drugs and non-cardiovascular drugs.<sup>3</sup> On the electrocardiogram, torsades de pointes appears as a polymorphic tachycardia characterised by a distinctive pattern of undulating peaks of sequential QRS complexes and T waves that twist around the baseline.<sup>4</sup> It is a well-known side-effect of class-III antiarrhythmic drugs that prolong cardiac repolarisation.<sup>5,6</sup> These drugs mainly reduce outward repolarising potassium currents at the level of the single myocytes. This is the therapeutic action by which refractoriness of the atria and ventricles is prolonged, however reducing repolarisation current in the ventricles is not without risk. If the individual threshold of repolarisation reserve<sup>7</sup> is surpassed, there is an increased risk of ensuing torsades de pointes arrhythmia.

The SWORD study provides an example where *d*-sotalol, a class-III antiarrhythmic drug was administered to reduce arrhythmogenic mortality in patients with myocardial infarction.<sup>8</sup> Surprisingly, *d*-sotalol caused an increase in mortality, presumably due to proarrhythmia, although very little objective data supports torsades de pointes as the explanation.<sup>9</sup> The objective of the DIAMOND-CHF trial was to study changes in overall mortality by dofetilide, another class-III antiarrhythmic drug, in patients with congestive heart failure.<sup>10</sup> The study identified 25 episodes of torsades de pointes in the 762 enrolled patients (3.3%), but no change in overall mortality was identified. Similar proarrhythmic actions of other class-III antiarrhythmic drugs have been reported, e.g. ibutilide (8.3%, 1-2 mg/day i.v.<sup>11</sup>), azimilide (0.9%, 100-125 mg/day p.o.<sup>12</sup>), and sotalol (1.8-4.1%, 160-320 mg/day p.o.<sup>13,14</sup>).

Non-cardiovascular agents have also been implicated in proarrhythmic mortality, including psychiatric drugs, antibiotics and antihistamines among others.<sup>3</sup> The reported incidence of torsades de pointes is rarely larger than a few tens in millions of patients exposed to these drugs.<sup>15</sup> However, this is likely to be an underestimate due to the difficulties of recognising torsades de pointes in the general population. Symptoms of torsades de pointes include palpitations, dizziness, syncope and death. Whether an episode of torsades de pointes will be identified and reported to the relevant centres is influenced by many factors, including the underlying disease of the patient and the amount of attention there is on the drug and its potential proarrhythmic properties.<sup>1,16,17</sup> With such a low incidence of torsades de pointes in

the patient population treated with such a drug, it is very unlikely that the arrhythmia will be recognised during clinical trials. These trials are generally not powered to identify such a risk. Nevertheless, it is not acceptable that a number of patients die due to e.g. antihistamine treatment targeting a disease that may not be life threatening.

Of 2194 cases of drug-induced torsades de pointes reported to the American Food and Drug Administration, only 26% was associated with cardiac agents.<sup>5,18</sup> Of the other drug classes with proarrhythmic side-effects, central nervous compounds comprised 22%, anti-infectives 19%, and antihistamines 12%. Many drugs have been withdrawn from the market and a large number of promising compounds have been stopped during development due to suspected or confirmed proarrhythmia.<sup>19</sup> Since patients are receiving medicine for a non-cardiovascular disease, the majority of the arrhythmia-induced syncope and deaths occur outside the continuous monitoring environment of the cardiac ward of a hospital. The chance of being resuscitated out-of-hospital and survive to leave hospital after cardiac arrest has been estimated to be only 1%.<sup>20,21</sup>

In 1988 prenylamine, an antianginal drug, was the first non-antiarrhythmic drug to be withdrawn from European markets due to its potential to cause torsades de pointes.<sup>5</sup> Since then, additional 8 marketed drugs have been withdrawn due to concerns over proarrhythmia (Table 1). That torsades de pointes is a reasonably modern problem is shown by the 2194 cases reported to the Food and Drug Administration: 7% were reported between 1969 and 1988 in contrast to 93% between 1989 and 1998, when the database was analysed.<sup>22</sup> The surveillance of drugs on the market by regulatory authorities mainly relies on medical personnel voluntarily reporting adverse events and mandatory reporting from the pharmaceutical companies.<sup>23</sup> In contrast to randomised clinical trials, the post-marketing surveillance is hampered by bias. For example, there are problems of selective reporting of patients exposed to new drugs or the compliance of the patients to take the drugs. Furthermore, certain patient groups, e.g. psychiatric patients, are more prone to sudden cardiac death unrelated to their therapy,<sup>24</sup> but likely due to their underlying disease. On the other hand, the spontaneous reporting system can detect very rare side-effects, especially when databases are pooled internationally. As such, it is very potent in alerting on potential adverse effects, however the reporting is not sensitive enough to verify the presence of the side-effect. Validation of a potential side-effect includes the disappearance of the side-effect upon withdrawal of the drug as well as reappearance upon rechallenge.

Authenticating the presence of an adverse effect is helped by elucidation of putative mechanisms and by the demonstration of the side-effect in a susceptible animal model or patient group. For example, the assessment of proarrhythmic potential of drugs could be performed in a patient group with congenital long-QT syndrome, which are known to be susceptible. This however is still considered unethical.

Thus, identifying the proarrhythmic drug as early as possible is important, however, it took almost ten years after the withdrawal of prenylamine before the preclinical approach to the assessment of proarrhythmic latency of a (potential) drug received intense attention from regulatory authorities.

**Table 1.** Drugs suspended or withdrawn from the European markets due to concerns over QT prolongation and torsades de pointes.

Drug	Year of withdrawal	Drug indication
Prenylamine	1988	Angina pectoris <sup>112</sup>
Terodiline	1991	Bladder incontinence <sup>112-114</sup>
Terfenadine	1998	Allergic rhinitis <sup>112,113,115</sup>
Sertindole*	1998	Schizophrenia <sup>112,113,116</sup>
Astemizole	1999	Allergic rhinitis <sup>112,113</sup>
Grepafloxacin	1999	Bacterial infections <sup>112,113</sup>
Cisapride	2000	Motility-related gastrointestinal disorders <sup>117</sup>
Droperidol	2001	Postoperative nausea and psychosis <sup>118</sup>
Levacetylmethadol	2001	Opiate dependence <sup>119</sup>

\*Sertindole was reintroduced under restricted use in 2002.

### Current state of non-clinical proarrhythmia assessment

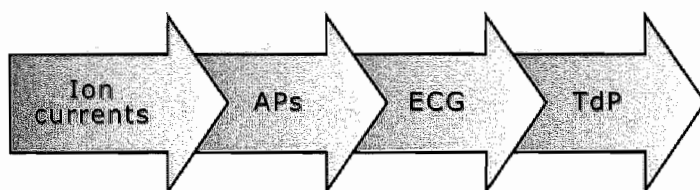
In 1997 the European Medicinal Agency released a document addressing the testing of compounds to identify repolarisation-prolonging products.<sup>25</sup> It included some recommendations for the test of future non-cardiovascular drugs. At that moment (1997) two types of investigations were suggested before the drug was clinical exposed. It included 1) electrocardiogram (ECG) and blood pressure recordings from conscious dogs and, 2) recordings of action potentials from any appropriate isolated tissue.

Two years later, a survey from 74 laboratories in 54 pharmaceutical industries documented large inconsistencies in the approach to cardiac safety.<sup>26</sup> The ECG was evaluated from dogs in all laboratories whereas 26% also collected rat ECG



data. Both anaesthetised and conscious models were employed, and usually a study consisted of three or more doses tested in 3 or 4 animals. In vitro cardiac electrophysiology of non-cardiovascular compounds was done in 56% of the companies. Usually Purkinje fibres and papillary muscles from dogs, rabbits, guinea pigs or sheep were used for assessing changes in the action potential. Concentrations were based on expected plasma concentrations (37%) or they were chosen without knowledge of therapeutic potency (30%).

As a consequence of this inconsistent approach, a meeting between researchers, industry and regulatory authorities was organised under the auspices of the European Society of Cardiology, leading to a document in which the inclusion of cell lines expressing cloned channels as well as isolated cells, tissue or heart and whole animals was proposed.<sup>3</sup> During accumulation of data from the successively higher levels of complexity, risk/benefit assessments should determine the continuation of development.



**Figure**

Levels of complexity available in the cardiac safety assessment of potential drugs. Specific ion currents can be measured at the level of the single cell, either in freshly isolated ventricular cardiomyocytes or in non-cardiac cell lines transfected with a human cardiac ion channels. Twenty-some different ion currents make up the action potentials (APs), which can differ according to tissue - regionally within the heart and among species. Action potentials can be acquired from single myocytes, multicellular preparations or from the beating heart. The various action potentials from different locations in the heart are the basis of the surface electrocardiogram (ECG). Finally, pathological stress can be added to all levels predisposing the material to vulnerable stimuli, thereby amplifying the outcome. For example, the ECG of a predisposed animal shows torsades de pointes (TdP) upon proarrhythmic stimuli more often than the naïve animal. See text for details.

An important aspect of the aforementioned approach is that decisions should be made only when sufficient data is available and only when several levels of complexity are addressed. Often decisions are based upon data gathered from too simplistic sources, which at best can give indications and provide directions for studies at other levels. While the Figure is built up of arrows pointing to higher levels of complexity, it should not be perceived as a flowchart for study planning. Similarly, the Figure does not imply that altering an ion current will start a train of

events culminating in torsades de pointes. Thus, although a potential drug might attenuate or augment any given ion current, it does not necessarily precipitate into cardiac proarrhythmic death.

Presently, an international guideline is being developed describing studies assessing the potential for delayed ventricular repolarisation by human pharmaceuticals (ICH S7B).<sup>27</sup> According to this guideline substances should be identified for their potential to delay ventricular repolarisation in general and to estimate the human risk of drug-induced prolongation of ventricular repolarisation. It proposes four levels of approaches to this evaluation:

- Ionic currents
- Action potential parameters
- ECG parameters
- Proarrhythmic effects

This recommended strategy has some resemblance to the Figure, although the authors of the draft guideline hesitate to recommend proarrhythmia studies. Based on the available information, an integrated risk assessment can be performed, considering potency of test substance, safety margins, predictive value of the assay and knowledge on drug metabolites and interactions. At this point, the guideline does not directly recommend the assessment of proarrhythmic risk of potential drugs. Although the guideline acknowledges that this is a logical step, the experimental modelling of clinical conditions predisposing the vulnerable patient to arrhythmia is considered to be complicated.<sup>27</sup>

Underlying the development of the guideline is the perception that prolongation of the human QT interval is harmful. At present, there are many experimental reports showing that a delayed repolarisation per se is not necessarily associated with proarrhythmia.<sup>28-33</sup> The role of animal models with increased susceptibility to torsades de pointes is far more important than expressed in the guideline. The various proarrhythmic animal models that are presently available<sup>34,35</sup> will supply valuable additional information to the results generated in the non-predisposed tissue.

## Available test systems

The battery of preclinical methodologies to evaluate potential drug-induced antagonised repolarisation and proarrhythmia is extensive but still limited in its power. Their aim should be to guide the execution of clinical experiments and to explain mechanisms behind the clinical findings.

### *Ion-current assays*

Several different ion channels have been found in the human heart, but to date most if not all drugs associated with torsades de pointes have been found to decrease at least one common current, the rapidly activating, delayed rectifying potassium current ( $I_{Kr}$ ). Although the proarrhythmic drugs may affect other cardiac currents, block of  $I_{Kr}$  seems to have a central aspect.  $I_{Kr}$  is an outward potassium current that is important in the repolarisation of the myocyte.<sup>36</sup> The current is conducted by a pore-shaped protein in the myocyte membrane that changes conformation upon alternations in the membrane voltage. In the human heart, the protein is encoded by HERG.<sup>37</sup> The protein may associate with an additional smaller, regulatory subunit MiRP1 to form native  $I_{Kr}$ <sup>38</sup> although this is disputed by others.<sup>39,40</sup> The current can be studied in isolated myocytes ( $I_{Kr}$  assays) or reproduced by expressing the protein encoded by HERG in a cell line ( $I_{HERG}$  assays).<sup>41</sup> Other ion currents frequently studied are the L-type calcium current ( $I_{Ca,L}$ ), the sodium current ( $I_{Na}$ ) and the slowly activating, delayed rectifying potassium current ( $I_{Ks}$ ). The clinical findings that certain congenital long QT syndromes, those involving  $I_{Na}$  and  $I_{Ks}$  demonstrates the possibility that torsades de pointes and sudden cardiac death can occur by mechanisms unrelated to defective  $I_{Kr}$ . Thus, these other ion currents should not be overlooked in the assessment of proarrhythmia.

Large varieties of potencies are found among the drugs blocking  $I_{Kr}$  (Table 2). Dofetilide is a very potent blocker with half maximal block ( $IC_{50}$ ) reported at 3.9 nM (rabbit<sup>42</sup>), 32 nM (guinea pig<sup>43</sup>), 46 nM (dog<sup>44</sup>) and 9.5-47 nM ( $I_{HERG}$ <sup>45-47</sup>). A rather weak  $I_{Kr}$  blocker associated with prolongation of the QT interval is the antibiotic, grepafloxacin.<sup>48-50</sup> Although  $IC_{50}$  values between 27 and 50  $\mu$ M (Table 2) have been reported, the drug was withdrawn from the market in 1999 due to several cases of torsades de pointes and sudden cardiac deaths.<sup>49,51</sup> Between these extremes are a variety of both proarrhythmic compounds and drugs not associated with torsades de pointes. For example, the  $I_{Ca,L}$  blocker verapamil is blocking  $I_{HERG}$  and  $I_{Kr}$  ( $IC_{50}$  = 94 - 1000 nM<sup>52,53</sup>) but is not reported to cause arrhythmia. Clearly, studies incorporating

higher levels of organisation or complexity are needed to elucidate the mechanism behind the differential proarrhythmic properties of these drugs. In essence, there is no relation between the potency of a drug to block  $I_{\text{HERG}}$  or  $I_{\text{Kr}}$  and its proarrhythmic potential.

A recent comparison between the  $I_{\text{HERG}}$  assay and action potential prolongation in canine Purkinje fibres examined ten drugs with or without clinically associated QT prolongation and torsades de pointes.<sup>53</sup> The  $\text{IC}_{50}$ s on  $I_{\text{HERG}}$  ranged between 16 nM and >300  $\mu\text{M}$ , however only 4 drugs prolonged the action potential in a concentration-dependent manner. For the other drugs there was not correlation between  $I_{\text{HERG}}$  block and action potential prolongation, which was partly explained by the ability of the drugs to influence multiple channels.

Hence, ion-current assays at best may explain findings found in more integrated systems (e.g. whole animals or clinic). At worst, they cause abandoning of the development of potential unique treatments of hitherto poorly manageable diseases.

#### *Action potential assays*

A result of opening a cardiac ion-channel is that charged ions flow through, causing the voltage gradient across the cell membrane to change. This usually starts a process that leads to closing of the channel and to opening of other ion channels. Alongside the voltage-gated channels are ion pumps and -exchangers that contribute to the movement of ions across the cell membrane. This complicated sequence of events is the basis of the action potential, where the myocyte initially depolarises and later, through repolarisation, returns to a resting potential. Collectively, this cycle is called the action potential which has the sole purpose is to coordinate contraction of the cell and thus of the heart.<sup>54,55</sup>

By altering the properties of one or more ion channels involved in this cycle, the action potential can be changed. For example, treatment with  $I_{\text{Kr}}$  blockers cause a delay in the repolarisation phase of the action potential and its duration prolongs. Drugs affecting several ion channels will result in more complex changes in action potential shape, usually with concentration-dependent aspects.

**Table 2.** A selection of drugs capable of acutely antagonising  $I_{\text{HERG}}$  and/or  $I_{\text{Kr}}$ 

	Clinically reported Tdp <sup>3,5,1,120</sup>	$I_{\text{HERG}}$	$\text{IC}_{50}$	$I_{\text{Kr}}$	References
<i>Class-III antiarrhythmic drugs:</i>					
Azimilide	+	560 nM	390 - 2000 nM		121-125
Dofetilide	+	9.5 - 47 nM	3.9 - 46 nM		42-47,126,127
<i>Withdrawn drugs:</i>					
Terfenadine	+	9 - 213 nM	50 - 150 nM		53,126,128-130
Astemizole	+	0.9 - 1.2 nM	1.5 nM		128,132,137,140
Grepafloxacin	+	37500 - 50000 nM	27200 nM		141-143
Cisapride	+	6.5 - 44 nM	9 - 15 nM		53,126,129-131,137,139,144-148
<i>Marketed drugs:</i>					
Amiodarone	+	1000 nM	1000 - 10000 nM		149-153
Sertindole*	+	5 - 64 nM	107 nM		44,45,129,139
Verapamil	-	94 - 830 nM	1000 nM		52,53,131,154-156
Loratidine	-	173 nM			132,136
Moxifloxacin	-	41200 - 129000 nM	750 nM		53,141,143,157

There is no clear association between the potency of the block and their association with clinical torsades de pointes.  $\text{IC}_{50}$  is the concentration of a given drug that inhibits the given current 50% in vitro. The plasma concentration of the drugs after therapeutic dosing varies considerably, which should be considered when comparing drugs. For a comprehensive table, please refer to reference <sup>51</sup> or to [www.fenichel.net](http://www.fenichel.net). \*, Sertindole was reintroduced under restricted use in 2002.

Differences in the ion-channel inventories responsible of the action potentials can result in gender, species and regional differences in action potentials.<sup>56-63</sup> Action potentials can be assessed from single cells, freshly isolated from various regions of the heart, but also from Purkinje fibres, papillary muscles and ventricular strips or slabs of tissue. In the testing of potential drugs, canine or rabbit Purkinje fibres are most commonly used, whereas the electrophysiology of rats and mice is regarded not to be representative of that of the human.

A comparative study testing 12 drugs for their effects on the action potential of canine Purkinje fibres included 5 of the  $I_{Kr}$  blockers from Table 1 (terfenadine, sertindole, grepafloxacin, cisapride and moxifloxacin).<sup>64</sup> Later on, the same laboratory reported data on 10 additional  $I_{Kr}$  blockers (including dofetilide and verapamil of Table 1).<sup>53</sup> With the exception of verapamil and terfenadine, they all prolonged the action potential in a dose-dependent manner. No relation between the  $IC_{50}$  of  $I_{HERG}$  or  $I_{Kr}$  of Table 1 and the action potential prolongation reported is present. Dofetilide at twice the  $IC_{50}$  (100 nM) prolonged the action potentials by up to 180 ms whereas cisapride at 1000 times  $IC_{50}$  (10  $\mu$ M) prolonged the action potentials by less than 40 ms.<sup>53,64</sup> Thus, there are clear discrepancies in how different drugs exert their electrophysiological effects. This will certainly translate into considerably proarrhythmic differences, stressing the importance of assessing electrophysiological and proarrhythmic properties of drugs at several levels of complexity.

In summary, taking the step to a more complex level of investigation from single-current measurements to analysing the action potential reveals that prolongation of repolarisation is determined by more factors than elucidated in an ion-current assay. Results from one level cannot forecast the results of the other level and more information is available for the risk assessment.

### *Assessing electrocardiograms*

The combined signal of cardiac action potentials throughout the heart can be recorded on the body surface as the ECG. Different species shows different ECG patterns and induced changes in action potential morphology of a significant amount of cardiac tissue will manifest as variations in the ECG. When action potentials are prolonged due to repolarisation delaying drugs (e.g.  $I_{Kr}$  blockers), the time interval between the start of the Q-wave and the end of the T-wave of the ECG will expand.

Measuring this interval - especially the end of the T-wave - is not straightforward. The T-wave usually ends gradually towards the isoelectric line of the ECG, thus no clear ending is defined. It is merely traditionally and not very scientifically grounded, that this critical measurement is defined at complete return to baseline. For example, the action potentials are often measured to 95% of full repolarisation to avoid this problem. Manual readings from paper tracings have a repeatability of about 25 ms in good hands, but even the best readers demonstrate occasional major errors.<sup>65</sup> Other strategies have been proposed, involving the area of the T-wave, superposition of several ECG leads or pattern recognition, which may prove to be more reproducible.

A number of confounding factors can influence comparisons between QT intervals. Best known is the influence of heart rate, which is inversely related to the QT interval. More than 20 different formulas are available that change a measured QT interval into the interval that would have been present at a heart rate of 60 beats per minute.<sup>66</sup> None of these formulas are perfect. At present, individual correction formulas seem to be the best choice, although it requires substantial baseline measures to cover a wide range of heart rates.<sup>67</sup> Even though relations between heart rate and QT interval vary substantially between individuals in a population, the intraindividual relationship is very stable over time.<sup>68</sup> The heart-rate influence is especially important if the drug tested is causing an altered heart rate and a QT prolongation. Another way of circumventing this problem is pacing the heart at a constant rate, although this is not always technically convenient. Another factor influencing the QT interval is the concentrations of electrolytes in the blood. For example thiazide and loop diuretics can cause hypokalemia thereby slowing repolarisation. Vice versa, infusion of potassium reduces drug-induced QT prolongation in healthy subjects.<sup>69</sup>

In the intact animal, blood samples can be gathered to analyse plasma concentrations of administered drugs and possible metabolites. It is often easier to relate this concentration to the expected clinical therapeutic plasma concentration than to relate the in-vitro concentration of a perfusion fluid. The perfusion fluid in an in-vitro setup differs from the in-vivo plasma in many ways, however the most important factor seems to be drug binding to the surface of plasma proteins. This can in some cases result in >99% of drug confined to plasma protein with only <1% freely dissolved in the plasma. Often disregarded in this context is that the ion channels of the myocytes are not in direct contact with the plasma, but have both vascular endothelium and extracellular matrix of varying distance between. This latter environment can

possibly accumulate considerable but unknown amounts of the drug.<sup>70,71</sup> In the in-vitro setup, the ion channels are directly exposed to the perfusion fluid.

Since, by definition, torsades de pointes is preceded by a prolongation of the QT interval, it makes sense to test a potential drug for QT prolonging effects. However there are examples of drugs that cause significant QT prolongation without being associated with torsades de pointes. Pentobarbital is one drug causing prolongation of the QT interval, but the anaesthetic is not proarrhythmic in dogs or humans.<sup>72</sup> Another well-known example is chronic amiodarone administration, which inflicts pronounced QT prolongation in animals and in patients. However, very few reports of torsades de pointes are available.<sup>14,30,73</sup>

### *Proarrhythmic animal models*

As indicated, torsades de pointes is a rare phenomenon. Patients with congenital long-QT syndromes can live for decades without experiencing the arrhythmia. The incidence of proarrhythmic side-effects of drugs is low: in the order of a few tens in millions of treated patients. It is unlikely that the arrhythmia will be registered during the clinical trials of the drugs. To circumvent this problem, several investigators have developed animal models in which torsades de pointes can be induced more easily. Although the regulatory authorities do not acknowledge these models as representative for clinical situations with a high risk of torsades de pointes, the draft guideline ICH S7B encourages scientists to develop and verify these models. At present, reproducible drug-induced torsades-de-pointes-like polymorphic tachycardias have been reported in methoxamine-treated rabbits, in dogs with atrioventricular block, in an isolated perfused rabbit-heart model and in transmural slices of canine ventricle, among others. These models are well established and should, in our believe, receive much higher recognition from regulatory authorities like the American Food and Drug Administration, the European Medicinal Agency and the Japanese Ministry of Health and Welfare.

Retrogradely perfused hearts from rabbits are reasonably devoid of the influence of metabolic, humoral and nervous systems.<sup>74</sup> The isolated heart is either left to beat spontaneously or it is paced. Proarrhythmic challenges utilised in this model involve bradycardia and hypokalemia.<sup>75,76</sup> Electrical monitoring is performed through monophasic action potential catheters on the heart and/or from electrocardiographic electrodes surrounding the heart. Administration of various agents affecting  $I_{Kr}$  can show morphological changes in the action potential (e.g. prolongation, triangulation,



humps resembling early afterdepolarisations), temporal instability of repolarisation duration, ectopic activity and/or arrhythmia morphologically resembling torsades de pointes recorded on the surface ECG of patients.<sup>74-77</sup> Furthermore, it seems to be possible to identify many drugs associated with torsades de pointes in humans or in whole-animal models,<sup>28,29</sup> although comparisons between patient-plasma concentrations and in-vitro perfusion concentrations are difficult. Also, drugs with little association to clinical torsades de pointes have limited effects in this model.<sup>28</sup>

Arterially perfused tissue from the left ventricle of canine hearts has successfully answered a variety of electrophysiological questions. The small transmural slabs of tissue are usually impaled with microelectrodes at the endo-, midmyo- and epicardium, but also action potentials measured by optical mapping techniques have been used. Furthermore, the entire electrical field across the ventricular wall can be recorded and has some resemblances to surface ECG monitoring of the intact heart. Hypokalemia or epicardial extrastimuli in combination with  $I_{Kr}$  block can precipitate polymorphic tachyarrhythmia in the tissue slab.<sup>78-81</sup> The combination of  $I_{Kr}$  and  $I_{Ks}$  block induces early afterdepolarisations on the transmembrane action potentials, triggered beats and occasionally polymorphic tachyarrhythmia.<sup>82</sup> Also non-cardiovascular drugs like cisapride which is associated with QT prolongation and torsades de pointes in patients have been tested in this system and shown to prolong repolarisation, augment heterogeneity of regional repolarisation gradients and induce arrhythmia in the ventricular tissue samples.<sup>83</sup> Arrhythmia caused by challenging repolarisation with  $I_{Kr}$  block was prevented by pentobarbital despite action potentials were prolonged further. This exemplifies that there are circumstances under which prolongation of action potentials may not be proarrhythmic.

Recently, this multicellular model has been extended to pathological conditions, where the tissues were retrieved from dogs with pacing-induced heart failure.<sup>84</sup> In the absence of any drugs, single extrastimuli could induce polymorphic tachycardia in tissue derived from heart-failure dogs, whereas in control tissue the arrhythmia was not observed. Thus, a pathological predisposition and a subtle proarrhythmic challenge on top is enough to cause serious myocardial events.

Torsades de pointes in a whole animal model, using anaesthetised rabbits sensitised by continuous infusion of the  $\alpha_1$ -adrenergic agonist methoxamine in addition to a class-III drug, was first reported in the early nineties.<sup>31,85</sup>  $\alpha_1$ -Adrenergic blockers immediately suppress the ventricular tachyarrhythmia seen in the model, indicating the importance of the adrenergic aspect of the model.<sup>85</sup> It is not clear by what mechanism methoxamine brings the heart into a vulnerable state in which the

class-III antiarrhythmic drug can exert its proarrhythmic potential. Especially the rabbit seem more susceptible to  $\alpha_1$ -adrenoceptor-induced elevations in intracellular calcium concentrations, an early step towards triggered activity,<sup>86</sup> which is a candidate explanatory mechanism for the observations in this model.<sup>87</sup> A substantial battery of agents has been tested in this model, including classical  $I_{Kr}$  blockers which all give rise to torsades-de-pointes-like arrhythmia.<sup>31,87-91</sup> The high reproducibility of arrhythmia has supported the search for novel parameters predicting torsades de pointes. An experimental drug named W-7 prevents torsades in this model without interfering with the  $\alpha_1$ -adrenergic stimulation and without shortening repolarisation.<sup>92</sup> Using this drug as a tool, a change in relative amplitude of the different notches of the rabbit T-wave was suggested as a precursor of torsades de pointes.<sup>93</sup>

Also dogs seem to be more susceptible to torsades de pointes when the  $\alpha$ -adrenergic system is stimulated. When anaesthetised dogs with bradycardia due to complete heart block are challenged with  $\alpha$ -adrenergic agonists and  $I_{Kr}$  blockers, they often show polymorphic ventricular tachycardia resembling torsades de pointes.<sup>94,95</sup>

The canine model of complete atrioventricular block expresses ventricular remodelling occurring as a response to bradycardia-induced volume overload. After ablation of the electrical conduction from atria to ventricles, the slower idioventricular rhythm of the ventricles causes a momentary decrease in cardiac output. This is compensated by an increase in stroke volume accompanied by eccentric hypertrophy of the ventricles and longitudinal growth of the myocytes.<sup>96,97</sup> Furthermore, the altered ion-channel densities of the myocytes attenuate repolarisation and make the dogs more susceptible to repolarisation-dependent arrhythmia like torsades de pointes.<sup>96,98,99</sup> This ventricular remodelling process takes 2 to 5 weeks.<sup>100</sup> In the anaesthetised animals, endocardial biventricular monophasic action potentials and ECG can be recorded whereas a recording in the conscious animal is restricted to ECG recorded on Holter devices or by telemetry. Cardiac pacing can be performed to stabilise the heart rhythm or to promote arrhythmia. A number of class-III antiarrhythmic drugs have been administered to the anaesthetised dogs with chronic atrioventricular block to assess mechanisms involved in the precipitation of torsades de pointes.<sup>30,97,101-104</sup> Also, for considering cardiac adverse effects of various non-cardiovascular drugs, conscious dogs have received drugs orally.<sup>105-109</sup>

Thus, although important information can be gathered from in-vitro assays, data from the intact animal is indispensable for making a qualified risk/benefit analysis of a potential new drug. Since torsades de pointes and not a delayed ventricular

repolarisation is the culprit adverse effect, a sound cardiac safety assessment of a drug should involve a proarrhythmic assay. Intact predisposed animals or hearts are superior models, merely because torsades de pointes are absent at lower levels of complexity (Figure).

### **Need for additional proarrhythmic parameters**

As illustrated above,  $I_{Kr}$  block, action potential or QT-interval prolongation are not irrevocably connected to proarrhythmic mortality.<sup>3,15,51,110,111</sup> When assessing the proarrhythmic potential of a drug, multiple strategies are available. However, at present, no single approach is perfect. Since drug-induced torsades de pointes are rare, multiple tactics should be employed to scrutinise early signs of the arrhythmia. Additionally it may be desirable to induce the arrhythmia in an appropriate animal model. Many early markers of proarrhythmia have been proposed. As with the QT prolongation, these other markers are not perfect either.

A number of drugs have been administered to the electrically remodelled dogs with chronic atrioventricular block, to assess mechanisms associated with the arrhythmia. Since only some of the tested drugs cause torsades de pointes, comparisons between proarrhythmic indicators can be performed in this model. From published data in Table 3, five class-III antiarrhythmic drugs are listed which all were tested in the model. Alongside the incidence of torsades de pointes are three reasonably established proarrhythmic signs, which in some cases are successful, but in other cases fail to correctly predict the proarrhythmic outcome. A comparable increase in the QT interval ( $>100$  ms) is seen for all the five drugs in Table 3, although the incidences of torsades de pointes are quite different. Amiodarone and *d*-sotalol show no arrhythmia although they exhibit both physiological and statistical significant prolongation of the QT interval. The absence of arrhythmias may be based on a modest increase in the interventricular dispersion of repolarisation, which does not reach the same levels as with the other three drugs. Also the incidence of extrasystoles tends to be higher in the proarrhythmic drugs. Together with Table 2, this illustrates the advantage of assessing several proarrhythmic signals for any given drug before concluding on its proarrhythmic profile.

**Table 3.** Five different class-III antiarrhythmic drugs tested in anaesthetised dogs with chronic atrioventricular block.

	TdP incidence	QT interval, ms	Dispersion of repolarisation, ms	Drug-induced extrasystoles	Reference
<i>d</i> -Sotalol	0 of 14	390 ± 50 → 495 ± 80 *	50 ± 25 → 80 ± 45 *	5 of 14	102
Almokalant	9 of 14	415 ± 35 → 545 ± 115 *	40 ± 20 → 110 ± 60 *	13 of 14	102
Amiodarone	0 of 7	340 ± 40 → 470 ± 75 *	40 ± 20 → 75 ± 35 *	0 of 7	30
Dofetilide	6 of 9	405 ± 65 → 505 ± 95 *	55 ± 25 → 110 ± 25 *	8 of 9	101
Azimilide	5 of 9	400 ± 65 → 500 ± 78 *	55 ± 25 → 110 ± 50 *	7 of 9	101

Incidences of torsades de pointes are quantified as number of dogs showing torsades relative to the total group investigated. Likewise with the presence of extrasystoles. Changes in QT intervals and interventricular dispersion of repolarisation are indicated by baseline values and drug values. Doses were: *d*-Sotalol: 2 mg/kg in 5 minutes i.v.; almokalant: 0.12 mg/kg in 5 minutes i.v.; amiodarone: 40 mg/kg/day p.o.; dofetilide: 25 µg/kg in 5 minutes i.v.; azimilide: 5 mg/kg in 5 minutes i.v. \*,  $P < 0.05$  versus baseline. See references for details.

In summary, when assessing the proarrhythmic potential of candidate drugs one should involve several lines of investigation. All four levels of complexity (Figure) should be addressed before estimating the electrophysiological and proarrhythmic potential of a drug. Available proarrhythmic models will not only add a level of complexity to the study, but can be used to evaluate predictive signs of proarrhythmia.

The present draft of the international guideline (ICH S7B) for the non-clinical evaluation of cardiac side-effects of new drugs covers only recommendations of assessing prolongation of ventricular repolarisation, whereas proarrhythmia and torsades de pointes are the relevant events explaining adverse effects and mortality in the treated patients.<sup>27</sup> The guideline fails to recognise the available animal models that provides important information of the proarrhythmic potential of drugs. Furthermore, there is a need for additional surrogate markers for torsades de pointes that could assist the risk assessment of new drugs. Potentially, this could also benefit patients when it is feasible to identify the individual prone to develop proarrhythmia.

### **Aim of the thesis**

Previous studies from our group have demonstrated a greatly enhanced susceptibility to drug-induced torsades de pointes in dogs with chronic complete atrioventricular block. We used this model to investigate predictive indicators of torsades de pointes. In the first study (chapter 2), we assess several doses of the same proarrhythmic drug. Unexpectedly, the well-known electrophysiological markers for torsades de pointes did not associate well with the proarrhythmic outcome. The hypothesis is proposed that novel electrophysiological repolarisation-dependent characteristics could be identified that have closer relation with the incidence of torsades de pointes. It is the aim of this thesis to propose and investigate these new proarrhythmic markers.

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# Electrophysiological Safety of Sertindole in Dogs with Normal and Remodeled Hearts

Morten B. Thomsen<sup>1</sup>, Paul G.A.Volders<sup>1</sup>, Milan Stengl<sup>1</sup>, Roel L.H.M.G. Späthjens<sup>1</sup>, Jet D.M. Beekman<sup>1</sup>, Ulrike Bischoff<sup>2</sup>, Morten A. Kall<sup>3</sup>, Kristen Frederiksen<sup>3</sup>, Jørgen Matz<sup>3</sup> and Marc A. Vos<sup>1</sup>

1. Department of Cardiology, Cardiovascular Research Institute Maastricht, Academic Hospital Maastricht, Netherlands.
2. GENION, Evotec QAI AG, Hamburg, Germany.
3. H. Lundbeck A/S, Copenhagen, Denmark.



**Abstract**

Inhibition of the potassium current  $I_{Kr}$  and QT prolongation are associated with drug-induced torsades de pointes arrhythmias (TdP) and sudden cardiac death. We investigated the cardiac electrophysiological effects of sertindole, an antipsychotic drug reported to prolong the QT interval in schizophrenic patients. In cell cultures, sertindole appeared a selective blocker of  $I_{HERG}$  over other ion currents. For  $I_{HERG}$ , the  $IC_{50}$  was  $64 \pm 7$  nM, whereas  $I_{SCN5A}$ ,  $I_{Ca,L}$ ,  $I_{Ca,T}$ ,  $I_{KCNQ1/KCNE1}$  and  $I_{Kv4.3}$  were blocked in the micromolar range. In canine ventricular myocytes, the  $IC_{50}$  for  $I_{Kr}$  inhibition by sertindole was  $107 \pm 21$  nM. Action potentials in these cells prolonged in a reverse-rate and concentration-dependent manner at 10 to 300 nM sertindole. In vivo, sertindole was administered to anesthetized dogs at clinically relevant (0.05 to 0.20 mg/kg) and high doses (1.0 to 2.0 mg/kg) i.v. At 0.05 to 0.20 mg/kg sertindole (plasma concentrations: 30 to 157 nM),  $QT_c$  was prolonged by 1 to 5 % in normal dogs and by 9 to 20% in dogs with remodeled hearts due to chronic AV block (CAVB). TdP was not induced at these doses in normal dogs or in CAVB dogs with reproducible induction of TdP by dofetilide in previous experiments. At 1.0 to 2.0 mg/kg sertindole (plasma concentrations: 0.5 to 3.1  $\mu$ M),  $QT_c$  prolonged by 6 to 11% in normal dogs and by 22% in dofetilide-sensitive CAVB dogs. TdP occurred in three of five animals in the latter group. Thus, at high i.v. doses sertindole can pose a serious proarrhythmic risk when electrical remodeling of the ventricles is present. At clinically relevant doses, however, sertindole does not cause TdP in anesthetized dogs with normal or remodeled hearts.

## Introduction

An estimated 1% of the population suffers from various degrees of schizophrenia with a significant burden on the health budget due to long-term hospitalization of these patients.<sup>1</sup> The average schizophrenic patient has a 10-year shorter duration of life than the rest of the population and suicidal rates are as high as 10%.<sup>1</sup> Treatment of these patients is not optimal since 30% respond poorly or not at all to available drugs and non-compliance is high, in part due to neurological side effects.<sup>2</sup> 5-chloro-1-(4-fluorophenyl)-3-(1-(2-(2-imidazolidinon-1-yl)-ethyl)-4-piperidyl)-1*H*-indole (sertindole) is an antipsychotic compound synthesized in the mid-1980s and introduced on the European market in 1996. Clinical phase III trials showed therapeutic effectiveness against both positive and negative symptoms of schizophrenia,<sup>3</sup> whereas extrapyramidal symptoms were absent.<sup>4</sup> Sertindole has a high affinity for several serotonin and dopamine receptor subtypes and  $\alpha_{1A}$ -adrenergic receptors.<sup>5-7</sup> Furthermore, a high inhibitory effect on the current mediated by the potassium channel encoded by HERG has been shown in vitro.<sup>8</sup> HERG blocking properties with  $IC_{50}$ s ranging from low nanomolar to low micromolar are common for most antipsychotic drugs<sup>9-11</sup> and may explain the drug-induced QT prolongation caused by some of them.<sup>12</sup>

In 1998, sertindole was withdrawn from the market due to concern about the high ratio of proven or suspected ventricular arrhythmias and sudden deaths in patients.<sup>13</sup> QT<sub>c</sub> intervals were prolonged in 4 to 5% of patients receiving sertindole,<sup>14</sup> and prolongation of action potential duration was confirmed in isolated feline<sup>15</sup> and rabbit hearts.<sup>16</sup> After reevaluation of the existing data, and based on new preclinical, clinical and epidemiological information, the concern about cardiac risk was outweighed by the therapeutic benefits of sertindole. This led to the reintroduction of sertindole on the European market in 2002 along with a prospective surveillance study of all patients taking the drug.<sup>17</sup>

In the present study we investigated the cardiac electrophysiological effects of sertindole in vitro and in vivo to provide an ionic basis for repolarization prolongation by the drug in relation to possible proarrhythmic actions in intact dogs.

## Methods

Animal handling was in accordance with the 'European Directive for the Protection of Vertebrate Animals Used for Experimental and Other Scientific Purposes (86/609/EU)'. The 'Committee for Experiments on Animals' of Maastricht University approved all experiments.

*Measurements on ion currents in cell cultures*

Chinese hamster ovary cells were stably transfected with human cloned HERG ( $I_{\text{HERG}}$ ; GENION, Hamburg, Germany) and SCN5A ( $I_{\text{SCN5A}}$ ; obtained from Dr. R. Kallen, University of Pennsylvania, Philadelphia, PA) representing the rapidly activating delayed rectifier potassium current and fast inward sodium current, respectively. Maximal outward  $I_{\text{HERG}}$  and peak  $I_{\text{SCN5A}}$  were measured. KCNQ1 and KCNE1 were stably co-transfected in Chinese hamster ovary cells ( $I_{\text{KCNQ1/KCNE1}}$ ; GENION) representing the slowly activating delayed rectifier potassium current. Human embryonic kidney 293 cells transiently expressing Kv4.3 $_{\Delta 2-39}$  ( $I_{\text{Kv4.3}}$ ) were used to assess the transient outward potassium current. Calcium-current experiments were performed on a NG-108-15 neuroblastoma-glioma hybrid cell line expressing endogenous L- and T-type calcium channels. Standard voltage-clamp protocols, electrodes, superfusion and internal solutions were used. Ion currents were measured at control and after 5-minutes incubation of sertindole at various concentrations. Each data point consisted of measurements from three to eight cells.  $\text{IC}_{50}$  values were obtained by fitting the data to a two-parameter sigmoidal curve ( $I = c^n / (c^n + \text{IC}_{50}^n)$ ).

*Experiments in isolated canine ventricular myocytes*

Twelve mongrel dogs (body weight:  $29 \pm 5$  kg, 8 males) were sacrificed for myocyte isolation. Thoracotomy was performed under anesthesia. Heparin (10.000 IU) was administered i.v. to avoid intracoronary clotting. After quick excision, the heart was placed in cold oxygenated cardioplegic solution and the coronary circulation was cannulated via the aorta. The heart was mounted to a constant-pressure Langendorff-like setup and perfused for 5 minutes using a Tyrode's solution with nominal  $[\text{Ca}^{2+}]$ . Collagenase A (Roche Diagnostics, Mannheim, Germany) in 0.5  $\mu\text{M}$   $\text{Ca}^{2+}$  Tyrode with 0.5 mg/ml bovine serum albumin perfused the heart for 30 to 35 minutes, followed by 0.2 mM  $\text{Ca}^{2+}$  Tyrode for 5 minutes to washout the collagenase. Midmyocardial cells were harvested from the free wall of both ventricles, gently minced, filtered, washed and stored in 0.2 mM  $\text{Ca}^{2+}$  at room temperature until use within 24 hours after isolation.

Myocytes were selected for experiments if they had sharp striations, clear contours and transparent cytoplasm without granulations or blebs. Further criteria for action-potential experiments included a stable resting membrane potential below -70 mV and a 'spike-and-dome' morphology of the action potential.

Whole-cell currents were recorded (AxoPatch 1D; Axon Instruments, Union City,

CA) using borosilicate glass patch pipettes filled with internal solution (125 mM K-aspartate, 20 mM KCl, 1.0 mM  $\text{MgCl}_2$ , 5 mM MgATP, 5 mM HEPES, 10 mM EGTA; pH adjusted to 7.2 with KOH) having a resistance between 1.0 and 3.0 M $\Omega$ . Cells were superfused with a standard buffer solution (145 mM NaCl, 5.4 mM KCl, 1.0 mM  $\text{MgCl}_2$ , 11 mM glucose, 10 mM HEPES, 1.8 mM  $\text{CaCl}_2$ , 5  $\mu\text{M}$  nifedipine; pH adjusted to 7.4 with NaOH, 37°C). Sertindole was dissolved in dimethyl sulfoxide. The rapidly activating delayed rectifier potassium current  $I_{\text{Kr}}$  was measured as the tail current fraction fully blocked by 2  $\mu\text{M}$  almokalant.<sup>18</sup>

Transmembrane action potentials (TAP) were recorded (AxoClamp 2B; Axon Instruments) using sharp glass microelectrodes filled with 3 M KCl and with a resistance between 20 and 60 M $\Omega$ . Cells were superfused with the same solution as in the whole-cell current experiments except that nifedipine was left out. Addition of 2  $\mu\text{M}$  almokalant to the superfusate was used to fully block  $I_{\text{Kr}}$ . Action potentials were recorded at each cycle length (CL) of 300, 400, 500, 1000 and 2000 ms. Action potential duration at 95% of repolarization ( $\text{APD}_{95}$ ) is presented as the average of five beats >100 beats after a change in pacing CL.

#### *In-vivo experiments*

Twenty-four anesthetized dogs (body weight:  $29 \pm 4$  kg, 11 males) were used for these experiments. In 13 animals complete AV block was induced.<sup>19</sup> After  $4 \pm 1$  weeks of AV block (chronic AV block; CAVB), the dogs were subjected to a TdP-susceptibility test using the  $I_{\text{Kr}}$  blocker dofetilide. Only if a dog showed reproducible TdP upon 25  $\mu\text{g/kg/5}$  minutes dofetilide, it was selected for the sertindole experiments. Thus, dofetilide was used as the positive reference compound. The average time between two experiments in a dog was  $2 \pm 1$  weeks.

Anesthesia, perioperative care, signal processing, data recording and off-line analysis have been described elsewhere.<sup>19</sup> Standard and precordial ECGs were recorded. In addition, biventricular endocardial monophasic-action-potential (MAP) recordings were made (EP Technologies, Sunnyvale, CA).

RR and QT intervals in lead II, left- and right-ventricular MAP duration (LV MAPD and RV MAPD, respectively) at 100% repolarization were measured off-line and averaged from five consecutive beats. The interventricular dispersion of repolarization ( $\Delta\text{MAPD}$ ) was calculated as the difference between the LV and RV MAPD. QT intervals were corrected for heart rate ( $\text{QT}_c$ ) according to Van de Water's formula.<sup>20</sup> The number of ectopic beats, defined as short-coupled beats arising from a new ventricular focus before complete repolarization of the previous beat, was counted during 10 minutes after administration of the drug. Both single and multiple

ectopic beats were counted. The latter are considered more proarrhythmic. TdP was defined as a polymorphic ventricular tachycardia consisting of five or more beats twisting around the isoelectric line of the ECG in the setting of a prolonged QT interval.

Sertindole (mol. wt. 441 g/mol) was dissolved in 0.1 M HCl and diluted in 10% hydroxypropyl cyclodextrin and 0.05 M phosphatebuffer (1:1). pH was adjusted to 7.4. The solution was filtered through a 22- $\mu$ m pore filter prior to use. Sertindole was administered over 5 minutes through a cephalic vein and blood samples were taken from the contralateral cephalic vein to measure plasma concentrations.

#### *Plasma analysis*

Blood samples were obtained 5, 10 and 25 minutes after drug administration and plasma was stored at -20°C until analysis at H. Lundbeck A/S (Copenhagen, Denmark). Sertindole plasma samples were extracted by solid mixed phase extraction. The sample extracts were analyzed by a normal phase high-performance liquid chromatography method with a mobile phase consisting of heptane, 2% piperidine in 2-propanol, and water (100:20:0.45) and quantified by fluorescence detection with excitation/emission wavelengths at 260 and 340 nm, respectively. The method had a mean recovery of 90% with a quantification limit of 0.5 ng/ml. Total plasma concentrations (free + bound) are reported.

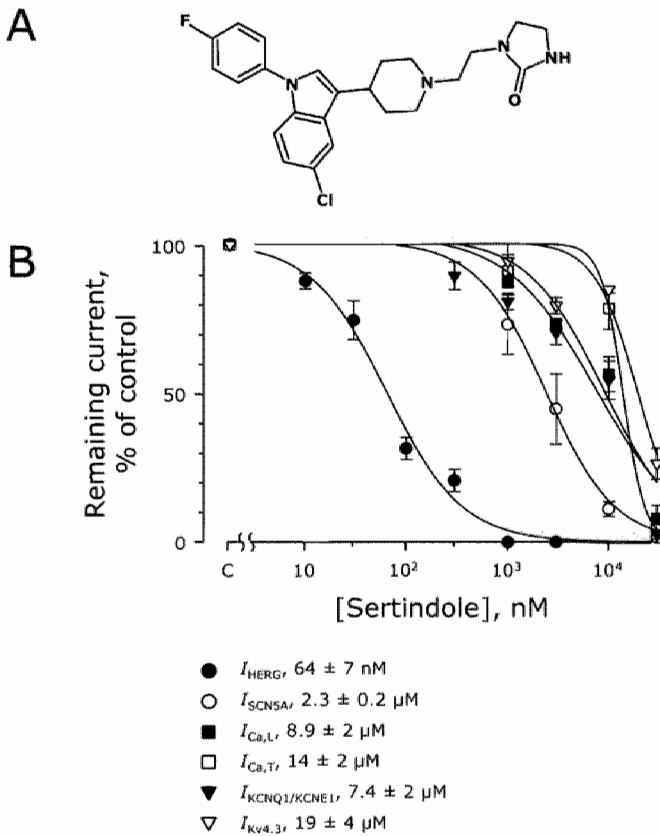
#### *Statistical analysis*

Electrophysiological parameters were compared with control employing (repeated-measures) ANOVA followed by Bonferroni's test. Comparisons between controls were performed with an unpaired Student's *t* test. Data are reported as mean  $\pm$  SEM.  $P < 0.05$  was considered statistical significant.

## Results

### *Sertindole is selective for $I_{HERG}$*

In Figure 1A the molecular structure of sertindole is shown. Figure 1B shows concentration-response curves for the various cardiac ion channels expressed endogenously or by transfection in cell cultures. Sertindole inhibited  $I_{HERG}$  in a concentration-dependent manner over the range of 10 to 1000 nM, with 50% block at  $64 \pm 7$  nM.  $I_{KCNQ1/KCNE1}$  was inhibited by  $10 \pm 5\%$  at 300 nM sertindole ( $IC_{50}$ :  $6.9 \pm 2 \mu M$ ), whereas other currents ( $I_{SCN5A}$ ,  $I_{CaL}$ ,  $I_{CaT}$ ,  $I_{Kv4.3}$ ) were only inhibited at micromolar concentrations. Representative examples of the six currents are shown in Figure 2.

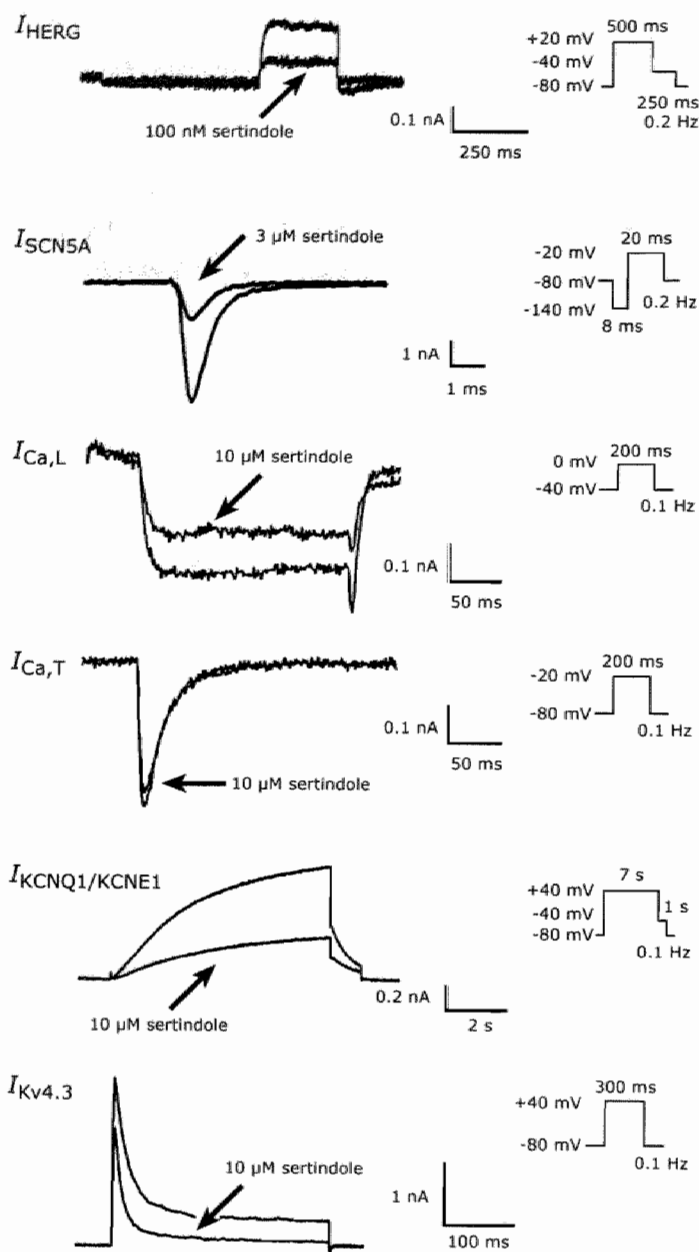


**Figure 1**

Selective block of  $I_{HERG}$  by sertindole.

**A:** Chemical structure of sertindole (mol. wt. 441 g/mol).

**B:** Composite data on blocking effects of sertindole on  $I_{HERG}$ ,  $I_{SCN5A}$ ,  $I_{Ca,L}$ ,  $I_{Ca,T}$ ,  $I_{KCNQ1/KCNE1}$  and  $I_{Kv4.3}$  in heterologous and endogenous expression systems. Data points represent the means for three to eight cells. Shown are the concentration-response curves, where the remaining current is plotted relative to its control level.  $IC_{50}$  values for the different currents are given in the legend. Hill coefficients are 1.16 for  $I_{HERG}$ , 1.27 for  $I_{SCN5A}$ , 1.15 for  $I_{Ca,L}$ , 3.98 for  $I_{Ca,T}$ , 0.99 for  $I_{KCNQ1/KCNE1}$  and 2.05 for  $I_{Kv4.3}$ .

**Figure 2**

Representative tracings of  $I_{HERG}$ ,  $I_{SCN5A}$ ,  $I_{Ca,L}$ ,  $I_{Ca,T}$ ,  $I_{KCNQ1/KCNE1}$ , and  $I_{Kv4.3}$  during treatment with sertindole. Concentrations of sertindole were chosen to indicate selectivity for  $I_{HERG}$  block. Insets, voltage-clamp protocols.

*Sertindole blocks  $I_{Kr}$  in canine ventricular myocytes*

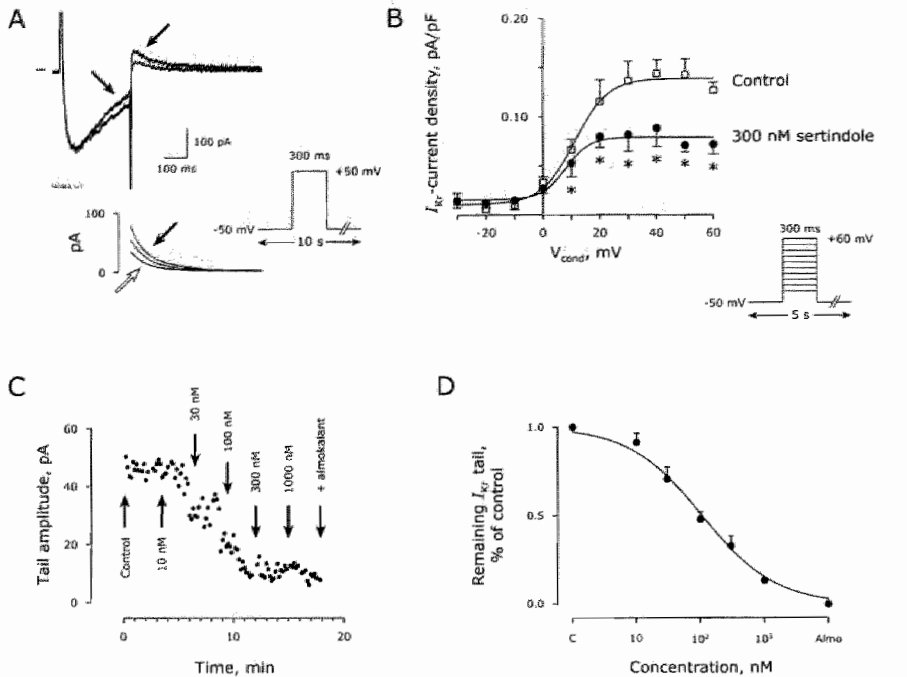
Activation of  $I_{Kr}$  occurred at depolarizations to higher than -10 mV and showed saturation at conditioning voltages ( $V_{cond}$ )  $\geq 20$  mV (Figure 3B). Maximal  $I_{Kr}$  density at control was  $0.14 \pm 0.07$  pA/pF. Boltzmann fit to the data revealed a half-maximal activation at  $11 \pm 1$  mV and a slope factor of  $5.9 \pm 0.9$  pA/pF/mV. Half-time for  $I_{Kr}$  deactivation upon repolarization to -50 mV was  $294 \pm 23$  ms.

An example of  $I_{Kr}$  recorded under control conditions and under the influence of 100 nM sertindole is shown in Figure 3A. Sertindole inhibited  $I_{Kr}$  tails in a concentration-dependent and voltage-independent manner. At 300 nM, the maximal  $I_{Kr}$  tail density had decreased to  $0.08 \pm 0.004$  pA/pF ( $57 \pm 4\%$ ;  $P < 0.05$ ; Figure 3B). Boltzmann fit of the remaining  $I_{Kr}$  at 300 nM sertindole showed a half-maximal activation at  $8 \pm 2$  mV ( $P = \text{NS}$  versus control) and a slope factor of  $4.2 \pm 1.4$  pA/pF/mV ( $P = \text{NS}$  versus control). Half-time for deactivation was  $273 \pm 48$  ms ( $P = \text{NS}$  versus control). Figure 3C shows an example of the effects of accumulating concentrations of sertindole to illustrate the concentration dependency of the drug on  $I_{Kr}$ . Using multiple voltage protocols to analyze the properties of  $I_{Kr}$  under the influence of sertindole, a concentration-response relationship was obtained (Figure 3D). Sertindole inhibited  $I_{Kr}$  in a concentration-dependent manner over the full range of 10 to 1000 nM, with 50% block at  $107 \pm 21$  nM ( $n_{cells} = 10$ ).

*Sertindole prolongs the transmembrane action potential*

TAP in normal canine ventricular myocytes prolonged from  $166 \pm 5$  to  $278 \pm 13$  ms by increasing pacing CL from 300 to 2000 ms ( $n_{cells} = 11$ ). Concentration-dependent prolongation of  $APD_{95}$  was observed for 10 to 300 nM sertindole, reaching statistical significance at 100 nM and higher, and for CL  $\geq 400$  ms (Figure 4). Under the influence of 300 nM sertindole,  $APD_{95}$  was prolonged to  $197 \pm 15$  ms (18 %) and  $345 \pm 44$  ms (24 %) at 300 and 2000 ms CL, respectively ( $P < 0.05$  for both CL), showing clear reverse rate dependence. Early afterdepolarizations or abnormal automaticity were not observed.



**Figure 3**

Effects of sertindole on  $I_{Kr}$  in normal canine ventricular myocytes.

- A:** Representative current recordings at control (arrows) and during 100 nM sertindole ( $C_m = 207$  pF). Left horizontal bar is at 600 pA. Below are illustrated second-order exponential fits of the tail currents at control (black arrow), full  $I_{Kr}$  block (white arrow) and for 100 nM sertindole. Current axis is enlarged, but time axis is identical to current trace in A.
- B:**  $I_{Kr}$  tail densities (difference currents at control and during 300 nM sertindole minus full block by almokalant;  $n_{cells} = 6$ ). \*,  $P < 0.05$  versus control. Inset, voltage-clamp protocol.
- C:** Tail-current amplitudes in a representative cell during increasing concentrations of sertindole ( $C_m = 191$  pF). Almokalant (2  $\mu$ M) provides full  $I_{Kr}$  block. Voltage-clamp protocol as in A.
- D:** Concentration-response curve of  $I_{Kr}$  inhibition by sertindole.  $IC_{50}$  value is  $107 \pm 21$  nM (Hill coefficient = 0.76,  $n_{cells} = 10$ ).

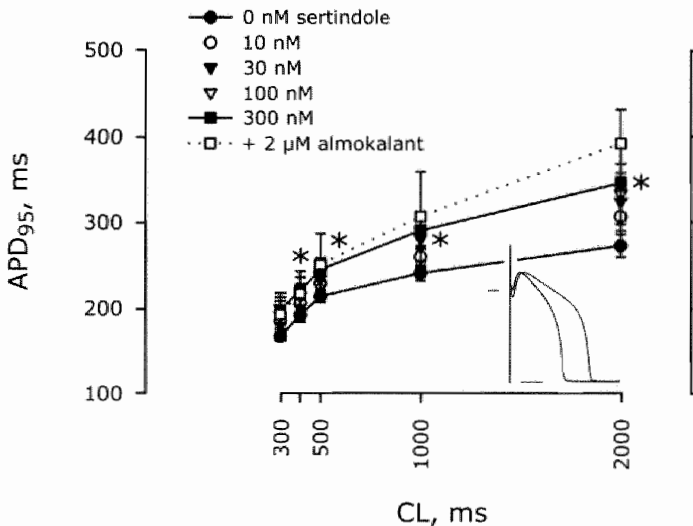
*Sertindole causes moderate prolongation of repolarization in normal hearts in vivo*

Cumulative doses of 0.05, 0.10, and 0.20 mg/kg sertindole (30-minutes intervals) were administered to five dogs. Plasma concentrations ranged from  $33 \pm 1$  nM after 0.05 mg/kg to  $157 \pm 18$  nM after 0.20 mg/kg. Reported plasma concentrations after human therapeutic dosing are  $22 \pm 12$  to  $158 \pm 63$  nM;<sup>21</sup> hence we considered these doses in the dogs to be clinically relevant. Representative examples of the electrophysiological effects are shown in Figure 5.  $QT_c$  interval did not prolong at

0.05 or 0.10 mg/kg sertindole. At 0.20 mg/kg  $QT_c$  prolonged from  $277 \pm 11$  to  $292 \pm 20$  ms (5%;  $P < 0.05$ ; Figure 6). At this dose, the RR interval increased from  $465 \pm 35$  to  $545 \pm 47$  ms (17%;  $P < 0.05$ ) and the QT interval from  $231 \pm 7$  to  $252 \pm 12$  ms (9%,  $P < 0.05$ ). The LV MAPD prolonged from  $191 \pm 8$  to  $213 \pm 9$  ms (10%;  $P < 0.05$ ) whereas the RV MAPD remained unchanged ( $181 \pm 9$  to  $197 \pm 7$  ms;  $P = \text{NS}$ ), leaving the interventricular dispersion of repolarization unaltered.

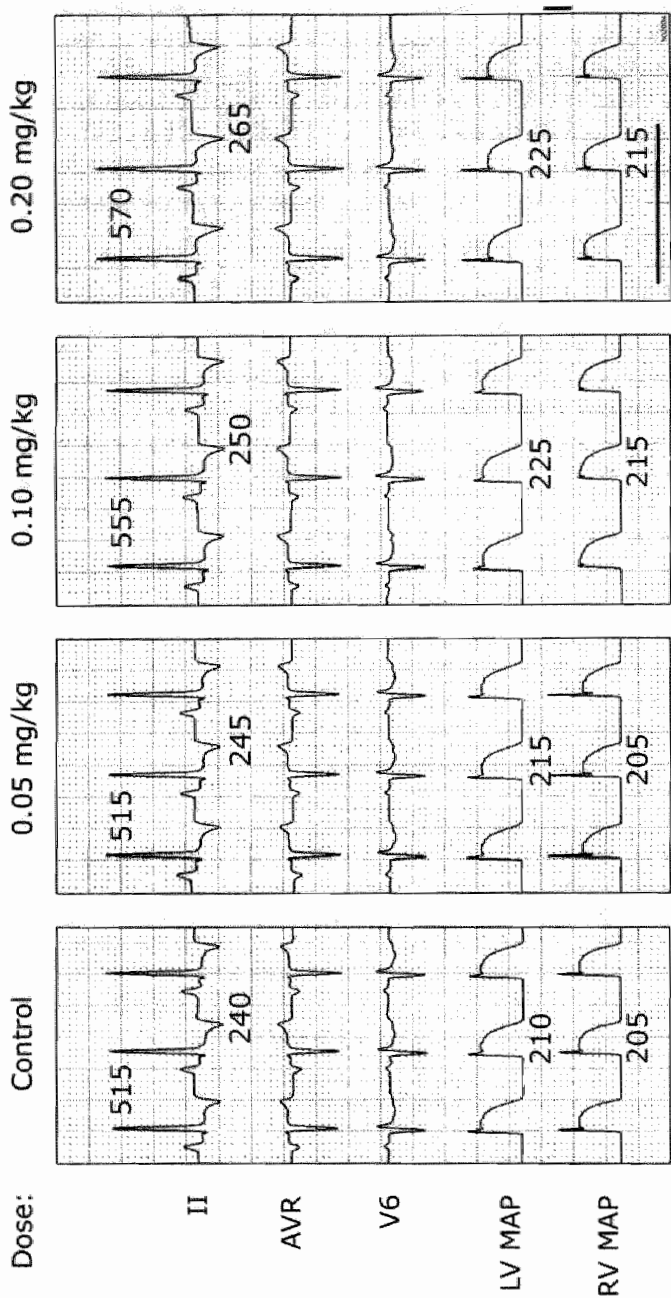
Cumulative doses of 0.5, 1.0, and 2.0 mg/kg sertindole (30-minutes interval) were administered to six other dogs. Plasma concentrations ranged from  $0.5 \pm 0.2$   $\mu\text{M}$  after 0.5 mg/kg to  $3.1 \pm 0.3$   $\mu\text{M}$  after 2.0 mg/kg. Twenty-four hours after the high dose-range experiments the mean plasma concentration was  $269 \pm 31$  nM. All high doses produced significant  $QT_c$  increases (Figure 6) with a maximal  $QT_c$  prolongation from  $294 \pm 8$  to  $326 \pm 19$  ms (11%;  $P < 0.05$ ) after 2.0 mg/kg sertindole. This involved a QT prolongation from  $251 \pm 10$  to  $289 \pm 24$  ms (15%;  $P < 0.05$ ), whereas RR interval remained unchanged. LV MAPD increased from  $214 \pm 11$  to  $264 \pm 28$  ms (23%;  $P < 0.05$ ) and RV MAPD from  $208 \pm 11$  to  $242 \pm 22$  ms (16%;  $P < 0.05$ ). The interventricular dispersion of repolarization was not changed ( $8 \pm 2$  to  $20 \pm 12$  ms;  $P = \text{NS}$ ).

Sertindole induced no changes in the PQ interval or QRS duration. Apart from the QT prolongation, no major changes were seen in the T-wave morphology at low or high doses of administration (Figure 5).



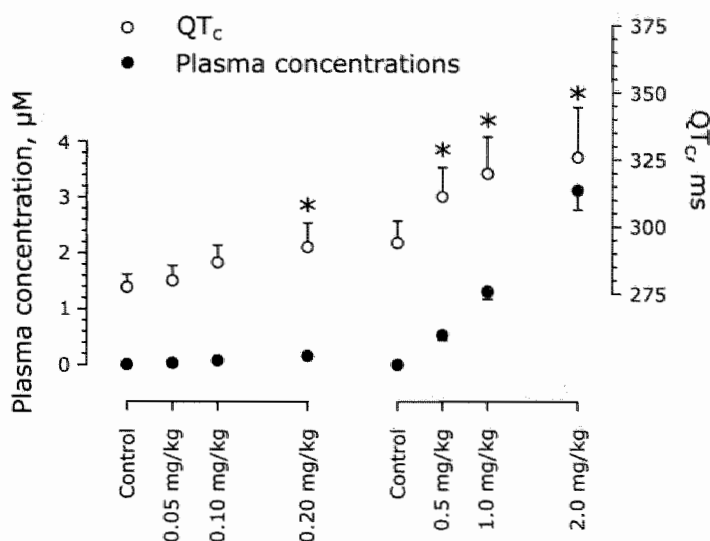
**Figure 4**

Transmembrane  $APD_{95}$  during sertindole treatment. Concentrations used were 10, 30, 100, and 300 nM. Pacing CL of 300, 400, 500, 1000, and 2000 ms were applied. Left and right vertical axes are identical. \*,  $P < 0.05$ , 100, and 300 nM versus control,  $n_{\text{cells}} = 9$ . Inset, representative action potentials at control and during 300 nM sertindole, CL = 2000 ms (0 mV level indicated; scale bar, 100 ms at  $-80$  mV).



**Figure 5**

Electrophysiological effects of cumulative doses of sertindole in an anesthetized normal dog. Three ECG leads, LV, and RV MAP recordings are shown in each panel. V6 refers to a precordial lead placed in the 6th intercostal space on the left lateral side of the thorax. RR intervals are above and QT times below lead II. MAPDs are below each signal. ECG calibrated to 1 mV/cm. Scale bar (right), 20 mV on the MAP signals. Horizontal scale bar, 1 second. In this example, the plasma concentrations measured at the time of these tracings (10 minutes after start of infusion) are 31, 77, and 121 nM after 0.05, 0.10, and 0.20 mg/kg, respectively.

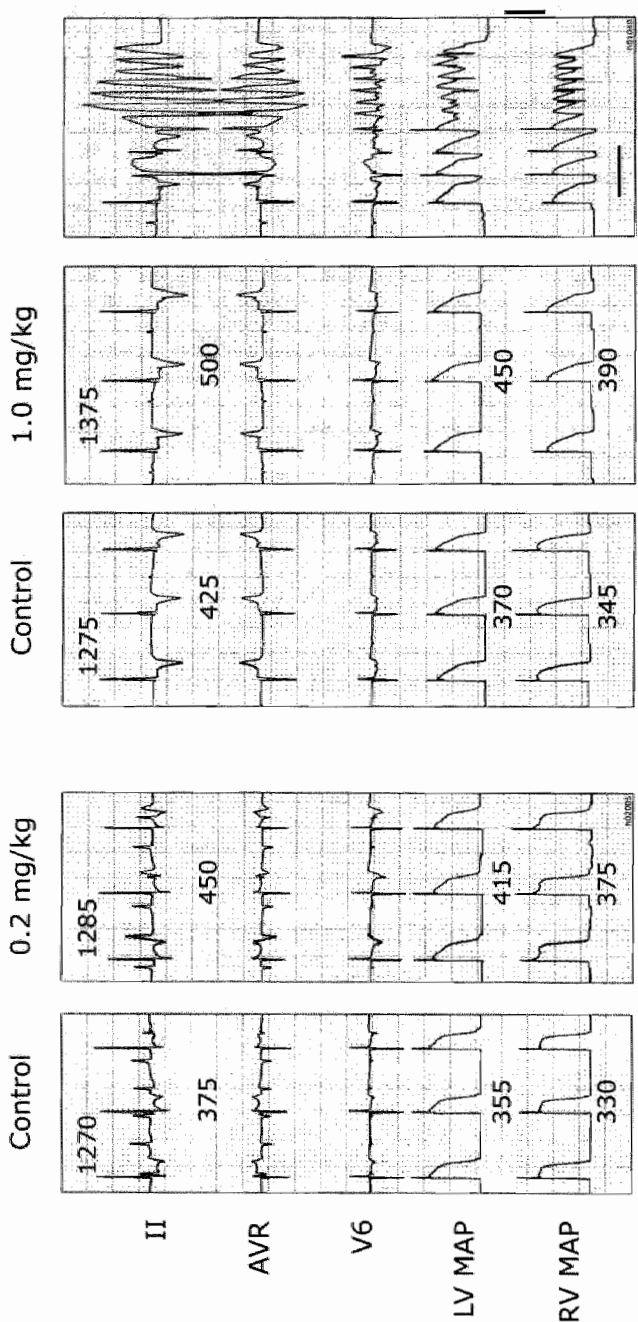


**Figure 6**

Relation between  $QT_c$  intervals and plasma concentrations of sertindole in anesthetized normal dogs. Cumulative doses of sertindole were administered i.v. as indicated ( $n_{\text{low doses}} = 5$  dogs,  $n_{\text{high doses}} = 6$  dogs). Plasma samples were obtained 10 minutes after start of drug infusion at each dose. \*,  $P < 0.05$  versus respective  $QT_c$  at control.

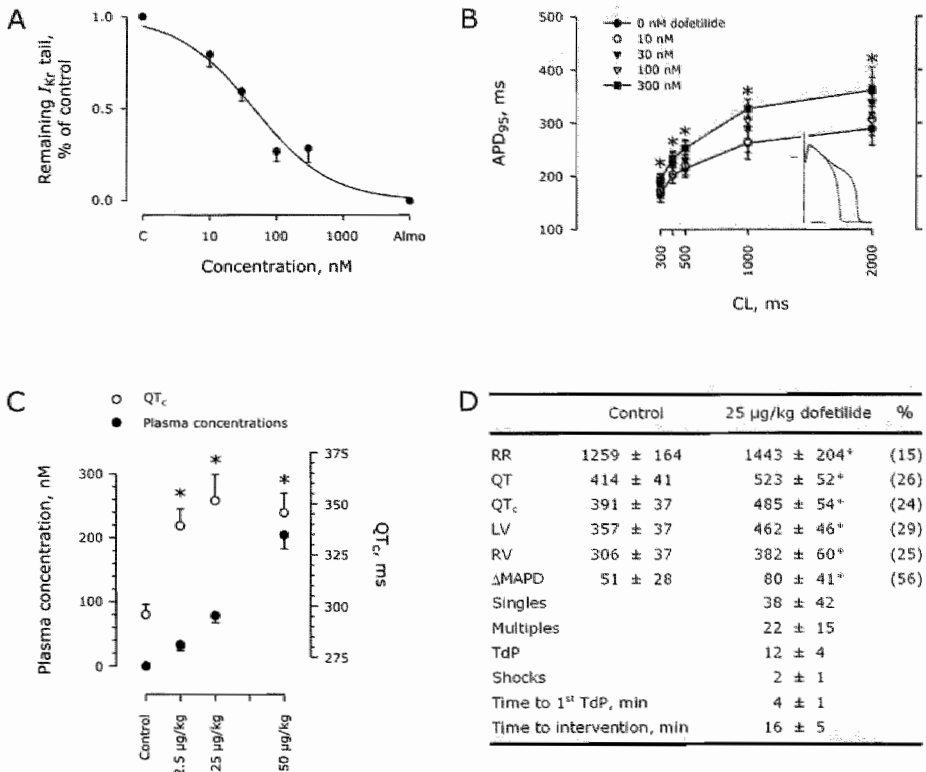
#### *Sertindole carries a proarrhythmic risk in electrically remodeled hearts*

Ten dofetilide-susceptible CAVB dogs received sertindole. In five animals 0.10 mg/kg was administered, followed by another 0.20 mg/kg after 30 minutes. The  $QT_c$  interval prolonged more than in normal dogs (e.g., 20% after 0.20 mg/kg in CAVB dogs versus 5% in normal dogs). Electrophysiological data from these experiments are summarized in Table 1. The five other dogs were tested with 1.0 mg/kg sertindole (Table 1). Sertindole prolonged repolarization in a dose-dependent manner, whereas the CL of the idioventricular rhythm only increased at the high dose (Table 1). The high dose of sertindole caused reproducible TdP in three of five dogs (Figure 7). In these three animals, the first TdP was seen on average  $7 \pm 2$  minutes after start of the 1.0 mg/kg sertindole infusion (range 6 to 9 minutes). The two dogs not responding with TdP received another 1.0 mg/kg, which caused TdP in one dog. During the 1-hour observation period after 1.0 mg/kg sertindole, a total of 19 TdP ( $6 \pm 2$ ,  $n_{\text{dogs}} = 3$ ) were seen of which four TdP had to be cardioverted electrically. Single ectopic beats ( $16 \pm 9$ ) occurred in all dogs at high dosing, while multiple ectopic beats ( $5 \pm 2$ ) were seen in four dogs. Interventricular dispersion of repolarization tended to increase, e.g., from  $45 \pm 6$  to  $79 \pm 19$  ms at 1.0 mg/kg ( $P = 0.09$ ).



**Figure 7**

Proarrhythmia by sertindole at high doses in an anesthetized CAVB dog. TdP (right-most panel) occurred at 6 minutes after infusion of 1.0 mg/kg sertindole. Proarrhythmia was not observed at the low dose of 0.2 mg/kg (second-left panel, 10 minutes) in this or all other CAVB dogs. Three ECG leads, LV and RV MAP recordings in each panel. RR intervals are above and QT time below lead II. MAPs are below each signal. ECG calibrated to 1 mV/cm. Scale bar (right), 20 mV on the MAP signals. Horizontal scale bar is 1 second.

**Figure 8**

Electrophysiological data on the positive reference compound dofetilide.

- A:** Concentration-response curve of the inhibition of  $I_{Kr}$  tails by dofetilide in normal canine ventricular myocytes ( $IC_{50}$  value  $46 \pm 9$ ; Hill coefficient, 0.76; mean  $C_m = 180 \pm 11$  pF;  $n_{cells} = 9$ ). Almokalant (Almo; 2  $\mu$ M) was used for full block of  $I_{Kr}$ .
- B:** Transmembrane APD<sub>95</sub> upon increasing concentrations of dofetilide. \*,  $P < 0.05$ , 100, and 300 nM versus control,  $n_{cells} = 5$ . Vertical axes are identical. Inset shows two representative action potentials at control and during 300 nM dofetilide, CL = 2000 ms (scale bar, 100 ms at -80 mV, 0 mV level indicated).
- C:** QT<sub>c</sub> prolongation by increasing doses of dofetilide i.v. to six anesthetized normal dogs and corresponding plasma concentrations. \*,  $P < 0.05$  versus control QT<sub>c</sub>. For comparison, plasma concentrations after oral administration to humans are 5 to 23 nM (plasma protein binding, 60-70%; volume of distribution, 3 l/kg<sup>33</sup>).
- D:** Electrophysiological effects of 25  $\mu$ g/kg dofetilide i.v. to the 10 anesthetized dogs with CAVB that were TdP-inducible and used for sertindole testing. Values in milliseconds and percentage increases in brackets. \*,  $P < 0.05$  versus control. Singles and multiples, numbers of single and multiple ventricular ectopic beats. TdP and shocks, number of TdP and electrical cardioversions. Times after start of dofetilide infusion.

**Table 1.** Electrophysiological data from anesthetized dogs with CAVB during treatment with sertiindole ( $n_{\text{dogs}} = 5$  in each group.).

	Control	0.10 mg/kg	%	0.20 mg/kg	%	Control	1.0 mg/kg	%
RR, ms	1240 ± 136	1271 ± 127	(2)	1235 ± 116	(0)	1442 ± 87	1562 ± 110*	(8)
QT, ms	385 ± 26	420 ± 22	(9)	458 ± 45*	(19)	408 ± 26	500 ± 39*	(23)
QT <sub>c</sub> , ms	364 ± 17	397 ± 15	(9)	438 ± 38*	(20)	370 ± 24	451 ± 34*	(22)
LV MAPD, ms	337 ± 20	372 ± 24	(10)	402 ± 43*	(19)	356 ± 19	447 ± 32*	(26)
RV MAPD, ms	309 ± 15	326 ± 19	(5)	354 ± 30*	(14)	311 ± 19	368 ± 27*	(18)
ΔMAPD, ms	28 ± 9	46 ± 6	(64)	48 ± 19	(72)	45 ± 6	79 ± 19	(76)
Reproducible TdP induction		0 of 5		0 of 5			3 of 5	

Percentages of increases from control to drug are depicted in brackets. Measurements were performed at 10 minutes after start of drug infusion or just prior to first TdP. There were no differences in control values for any parameter. \*,  $P < 0.05$  versus control.

*Electrophysiological data on the positive reference compound dofetilide*

Concentration-response studies of dofetilide on  $I_{Kr}$  in native ventricular myocytes revealed an  $IC_{50}$  of  $46 \pm 9$  nM (Figure 8A). Prolongation of TAP in the myocytes was reverse rate-dependent (Figure 8B). In normal anesthetized dogs, i.v. doses of 12.5, 25, and 50  $\mu\text{g/kg}$  dofetilide<sup>19</sup> caused significant  $QT_c$  prolongation (19% to 25%;  $P < 0.05$  versus control; Figure 8C). RR also increased, e.g., by 13% after 12.5  $\mu\text{g/kg}$  ( $P < 0.05$  versus control). Plasma concentrations of dofetilide are given in Figure 8C. Dofetilide (25  $\mu\text{g/kg}$ ) induced TdP in 10 of 13 anesthetized CAVB dogs (Figure 8D for  $n_{\text{dogs}} = 10$  used for sertindole testing in vivo).

## Discussion

The present study investigates the electrophysiological properties of sertindole from cloned cardiac ion channels to anesthetized dogs with normal and remodeled hearts. The results can be summarized as follows: 1) Sertindole is a selective blocker of  $I_{HERG}$  over other ion currents expressed in cell cultures. 2) Sertindole causes concentration-dependent block of native  $I_{Kr}$  and this translates into reverse-rate dependent lengthening of myocyte action potentials. 3) In anesthetized dogs, dose-dependent prolongation of in vivo repolarization by sertindole is observed. 4) Clinically relevant doses of sertindole do not cause TdP in anesthetized normal dogs or in CAVB animals with reproducible induction of TdP by dofetilide in previous experiments. 5) High doses of sertindole induce multiple ectopic beats and TdP in the majority of these CAVB dogs.

### *Normal and remodeled hearts*

To elucidate whether a drug is devoid of proarrhythmic properties, a reproducible animal model is essential. Testing drugs in normal hearts is necessary, but is not sufficient for the recognition of proarrhythmic effects in the diseased heart. We used the canine model with CAVB, known to have acquired QT prolongation. Creation of CAVB results in a bradycardia-induced volume overload. Hypertrophy is observed in ventricular myocytes<sup>22</sup> as well as in the whole heart.<sup>23,24</sup> Contractile remodeling in vivo restores initially-depressed cardiac output (compensated function), which is associated with an increased cytosolic  $\text{Ca}^{2+}$  transient in vitro.<sup>25,26</sup> Downregulation of  $I_{Ks}$  and  $I_{Kr}$ <sup>27,28</sup> and upregulation of the sodium-calcium exchanger<sup>26</sup> contribute to the electrical alterations in remodeled CAVB hearts. This ventricular remodeling



predisposes to TdP and sudden cardiac death.<sup>29</sup>

Whereas most class III antiarrhythmic drugs cause TdP in 2 to 5% of patients,<sup>12</sup> an incidence in the order of 56 - 67% is encountered in anesthetized CAVB dogs, making the model very sensitive.<sup>19,30</sup> In the present study, the non-cardiovascular drug sertindole was tested in a number of different ways and using a broad dose regimen. Based on earlier clinical reports of low proarrhythmia of sertindole in patients (0.3% cardiac mortality rate or ~10% of anti-arrhythmic drugs<sup>31</sup>), we anticipated a low TdP incidence in the CAVB dog. Serial testing in this model has shown reproducible induction of TdP.<sup>32</sup> Therefore, we chose to increase the sensitivity of the model and to evaluate the proarrhythmia of sertindole only in dogs that showed reproducible TdP after administration of 25 µg/kg dofetilide.

### *Cardiac safety of sertindole*

This is the first report on sertindole, in which both in vitro and in vivo investigations are combined. Sertindole caused prolongation of repolarization in both normal and CAVB dogs, although at variable degree, e.g., at 0.20 mg/kg, QT<sub>c</sub> interval increased by up to 5% in normal hearts and up to 20% in CAVB dogs. The plasma concentrations measured in dogs in this study at the low doses were comparable with plasma concentrations from human volunteers (4 to 20 mg/day sertindole p.o., range from 22 ± 12 to 158 ± 63 nM<sup>21</sup>). These doses did not cause TdP in dofetilide-sensitive CAVB dogs. Administration of 25 µg/kg dofetilide led to a plasma concentration of 79 ± 11 nM. Reported plasma concentrations from human volunteers receiving dofetilide ranged from 5 to 23 nM.<sup>33</sup>

Eckardt et al. reported a low torsadogenic potential of sertindole in isolated rabbit hearts.<sup>16</sup> They showed a 15 to 17% prolongation of the QT interval at a perfusion concentration of 1.5 µM sertindole without induction of TdP. In the present investigation in anesthetized dogs with normal hearts, 9% prolongation of the QT<sub>c</sub> interval was observed at 1.3 ± 0.1 µM. No TdP was observed, confirming the results from Eckardt et al.<sup>16</sup> Plasma protein binding in vivo and unknown levels of accumulation in cardiac tissue complicate comparisons between these models. Relating plasma concentrations to concentrations employed in the in vitro setting can only be done with great caution. Among the factors to be taken into account are plasma protein binding, tissue accumulation and the distance between the plasma protein and the receptor on the cardiomyocyte in situ. Plasma protein binding of sertindole in humans is high (>99%<sup>34</sup>), indicating a free plasma concentration of maximally 1 to 2 nM after therapeutic administration, based on the plasma concentrations in human volunteers.<sup>21</sup> The level of accumulation in cardiac tissue

is unknown, but a rather large volume of distribution is reported (20-40 l/kg<sup>34</sup>), indicating accumulation of sertindole in various tissues. In our dogs, maximal QT prolongation was already seen 5 to 10 minutes after the start of infusion of sertindole, suggesting a rapid inhibition of  $I_{Kr}$  once the drug is present in the circulation. The relative  $I_{Kr}$  block induced by sertindole in vivo or in the clinic could be underestimated when plasma concentrations are compared to in vitro concentrations.

Apart from an inhibition of  $I_{Kr}$ , sertindole has also been reported to block the human dopamine  $D_2$  and the 5-hydroxytryptamine<sub>2A</sub> receptors.<sup>5</sup> It does also show  $\alpha_{1A}$ -blocking properties in rat mesenteric arteries.<sup>7</sup> New studies are required to test possible additional electrophysiological properties of sertindole in the heart under conditions when physiological levels of these agonists are present.

### *Pharmacological implications*

Previous studies using chronic amiodarone administration have shown that TdP can be absent in CAVB dogs despite prolongation of the QT<sub>c</sub> interval by 21%.<sup>35</sup> The present study indicates again a poor association between the degree of QT<sub>c</sub> prolongation and the incidence of TdP (Table 1): at a comparable QT<sub>c</sub> after 0.2 and 1.0 mg/kg sertindole, TdP were only induced after the higher dose. This stresses not only the importance of testing several doses when assessing the proarrhythmic potential of a drug but also the relevance of addressing other proarrhythmic factors like ectopic beats and dispersion.

If our in vitro data from cell cultures and isolated canine myocytes would have determined the future for sertindole, the drug would have likely been abandoned from further development (e.g., based on the recommendations of the Policy Conference of the European Society of Cardiology<sup>12</sup>). The expansion of our study to in vivo testing showed a discrepancy between the in vitro finding of  $I_{Kr}$  inhibition and prolonged cellular repolarization and the absence of arrhythmias in normal anesthetized dogs. Our data strongly advocate the use of pathological animal models when testing for proarrhythmic properties of cardiovascular and noncardiovascular drugs.

A recent risk-benefit analysis of the preclinical and clinical data on sertindole by the European Committee for Proprietary Medicinal Products led to the reintroduction of sertindole to the European market in 2002.

### *Limitations*

Steady-state plasma concentrations were not obtained in this study, as opposed to previous clinical studies, and the pharmacokinetic difference between acute i.v. and repeated oral dosing should be considered when extrapolating our data to humans. Differences in accumulated tissue concentrations after acute i.v. versus chronic oral administration will likely exist. Furthermore, species differences between dogs and patients should be taken into account.

### *Conclusions*

In vitro studies clearly show sertindole's selective inhibition of  $I_{\text{HERG}}$  over other ion currents. Block of native  $I_{\text{Kr}}$  forms the ionic basis for action potential prolongation in canine ventricular myocytes and QT prolongation in vivo. At high i.v. doses, sertindole can pose a serious proarrhythmic risk when electrical remodeling of the ventricles is present, as in dogs with CAVB. At clinically relevant doses, sertindole does not cause TdP in anesthetized dogs with normal or remodeled hearts.

### **Acknowledgments**

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# Increased Short-Term Variability of Repolarization Predicts *d*-Sotalol-Induced Torsades de Pointes in Dogs

Morten B. Thomsen<sup>1,2</sup>, S. Cora Verduyn<sup>1</sup>, Milan Stengl<sup>1,2</sup>, Jet D.M. Beekman<sup>1,2</sup>,  
Geert de Pater<sup>1</sup>, Jurren van Opstal<sup>1</sup>, Paul G.A. Volders<sup>1</sup> and Marc A. Vos<sup>1,2</sup>

1. Department of Cardiology, Cardiovascular Research Institute Maastricht, Academic Hospital Maastricht, Netherlands.
2. Department of Medical Physiology, University Medical Center Utrecht, University of Utrecht, Netherlands.

**Abstract**

Identification of patients at risk for drug-induced torsades de pointes arrhythmia (TdP) is difficult. Increased temporal lability of repolarization has been suggested as valuable to predict proarrhythmia. The predictive value of different repolarization parameters, including beat-to-beat variability of repolarization (BVR), was compared in this serial investigation in dogs with chronic AV block.

In anesthetized dogs with electrically remodeled hearts, the dose-dependent difference in drug-induced TdP (*d*-sotalol, 2 and 4 mg/kg i.v. over 5 minutes, 25% and 75% TdP, respectively) could not be accounted for by prolongation of  $QT_c$  ( $410 \pm 37$  to  $475 \pm 60$  versus  $415 \pm 47$  to  $484 \pm 52$  ms, respectively). BVR was quantified by Poincaré plots at baseline and immediately before onset of *d*-sotalol-induced extrasystolic activity. TdP occurrence was associated with an increase in the short-term variability (STV) of the left ventricular monophasic action potential duration ( $3.5 \pm 1.5$  to  $5.5 \pm 1.6$  versus  $3.0 \pm 0.7$  to  $8.6 \pm 3.8$  ms, respectively), which was reversible when TdP was abolished by  $I_{K,ATP}$  activation. The absence of TdP despite  $QT_c$  prolongation after chronic amiodarone treatment could also be explained by an unchanged STV. In experiments with isolated ventricular myocytes, STV increased after  $I_{K_r}$  block and was highest in cells, which subsequently showed early afterdepolarizations.

Proarrhythmia is not related to differences in prolongation of repolarization but corresponds to BVR, here quantified as STV of the left ventricle. STV could be a new parameter to predict drug-induced TdP in patients.

## Introduction

Torsades de pointes arrhythmias (TdP) are repolarization dependent polymorphic ventricular tachyarrhythmias that can stop spontaneously or degenerate into ventricular fibrillation causing sudden death. One of the electrophysiological hallmarks of TdP is the prolonged QT interval often regarded as an unwanted adverse effect of drugs. However, it has been argued that QT time by itself is not a sensitive parameter to predict TdP, because similar, prolonged QT intervals may have distinct arrhythmogenic outcomes.<sup>1-7</sup> Numerous parameters and ideas have been suggested to be more valuable,<sup>1,2,8-11</sup> including the concept of diminished repolarization reserve.<sup>12</sup> Decreased repolarization force at times of additional demand can explain the higher likelihood for TdP. For the proarrhythmic action of class-III antiarrhythmic drugs, this can be viewed as the final hit in a predisposed heart, which unchallenged functions adequately. Thus, repolarization reserve can be regarded as the ability of a heart to withstand a challenge on repolarization. Creation of chronic AV block (CAVB) in the dog results in a high susceptibility for drug-induced TdP, most likely due to electrical remodeling.<sup>13,14</sup> In our opinion, this animal model should have a reduced repolarization reserve. In the past, the proarrhythmic potential of several different class III antiarrhythmic drugs was determined showing a comparable and prominent QT<sub>c</sub> prolongation for all drugs but a low TdP incidence after amiodarone (0%) and *d*-sotalol (0 to 5%) as compared to 56 to 67% TdP for other drugs tested.<sup>15</sup> This led us to perform the present serial investigation in anesthetized CAVB dogs, where the expected dose-dependent differential TdP occurrence after *d*-sotalol was used to compare the predictive value of different repolarization parameters including beat-to-beat variability of repolarization (BVR).

## Methods

Experiments were performed in eight adult mongrel dogs with CAVB (5 males). In a preliminary operation, the AV node was ablated as described previously.<sup>14</sup> Experiments reported here were started >5 weeks after ablation, which exceeded the completion of ventricular electrical remodeling and proarrhythmia.<sup>14</sup> Under complete anesthesia (induced by sodium pentobarbital, 20 mg/kg i.v. and maintained by halothane), two monophasic action potential (MAP) catheters were advanced to the endocardium of left (LV) and right ventricle (RV). *d*-Sotalol was administered in two doses (2 and 4 mg/kg i.v. over 5 minutes) in a serial random crossover design



( $2 \pm 1$  weeks between experiments). The natural sequence of events leading to drug-induced TdP in CAVB dogs can be divided into two phases; (1) prolongation of repolarization and (2) occurrence of (multiple) extrasystoles, which are often but not always followed by TdP.<sup>13</sup> Dogs were considered inducible when 3 or more episodes of TdP occurred after a dose of *d*-sotalol. The  $I_{K,ATP}$  opener, levcromakalim (10  $\mu\text{g/kg}$  i.v.) was administered in experiments with TdP to assess reversibility.

Transmembrane action potentials from enzymatically isolated myocytes from CAVB dogs<sup>16</sup> were recorded (15 cells, 9 dogs). Microelectrodes (20 to 60  $\text{M}\Omega$ ) filled with 3 M KCl and pacing frequencies of 0.5-1 Hz were used. Action potentials were recorded under conditions of no  $I_{Kr}$  block versus full  $I_{Kr}$  block.

### *Electrophysiological parameters*

Mean RR and QT intervals from lead II and duration of the two MAPs to 100% repolarization (MAPD) of 30 consecutive beats were determined. Measurements were done before *d*-sotalol administration and in a period during which prolongation of repolarization had reached a plateau but the first drug-induced extrasystole had not yet occurred. Interventricular dispersion ( $\Delta\text{MAPD} = \text{LV minus RV MAPD}$ ) and heart rate corrected QT interval ( $\text{QT}_c$ , van de Water's formula) were calculated. These temporally averaged electrophysiological measurements will be referred to as EP parameters to discern them from parameters of lability.

### *Lability parameters*

To assess BVR, Poincaré plots were drawn by plotting each value against the former value (Figure 1 for LV MAPD<sup>2,17,18</sup>). It was performed for RR and QT intervals and for LV and RV MAPD from 30 consecutive beats under stable idioventricular focus. The areas of the plots were determined and their dimensions calculated: The mean orthogonal distance from the diagonal to the points of the Poincaré plot was determined and referred to as short-term variability ( $\text{STV} = \sum |D_{n+1} - D_n| / [30 \cdot \sqrt{2}]$ , where *D* represents the duration of RR, QT or MAP). The average distance to the mean of the parameter parallel to the diagonal ( $\sum |D_{n+1} + D_n - 2D_{\text{mean}}| / [30 \cdot \sqrt{2}]$ ) was regarded as the long-term variability. This nomenclature is adopted from heart-rate variability investigations using Holter monitoring of humans over several hours, in which steady changes over time tend to follow the diagonal and sudden changes (e.g. an extrasystole) result in a deviation from the diagonal.<sup>18</sup>

The QT variability index ( $\text{QTVI}_{30}$ ) as proposed by Berger et al.<sup>11</sup> and  $\text{instability}_{30}$  as proposed by Hondeghem et al.<sup>1,2</sup> were calculated for QT and for LV and RV MAPD.

Because of the fast onset of extrasystolic activity, these were calculated for 30 beats only and not over the proposed 256 seconds and 3 minutes, respectively.

In addition to assessing lability of repolarization at the two time points in the *d*-sotalol experiments, we assessed STV in data gathered in a study<sup>3</sup> of 4 weeks of amiodarone treatment (40 mg/kg/day p.o.).

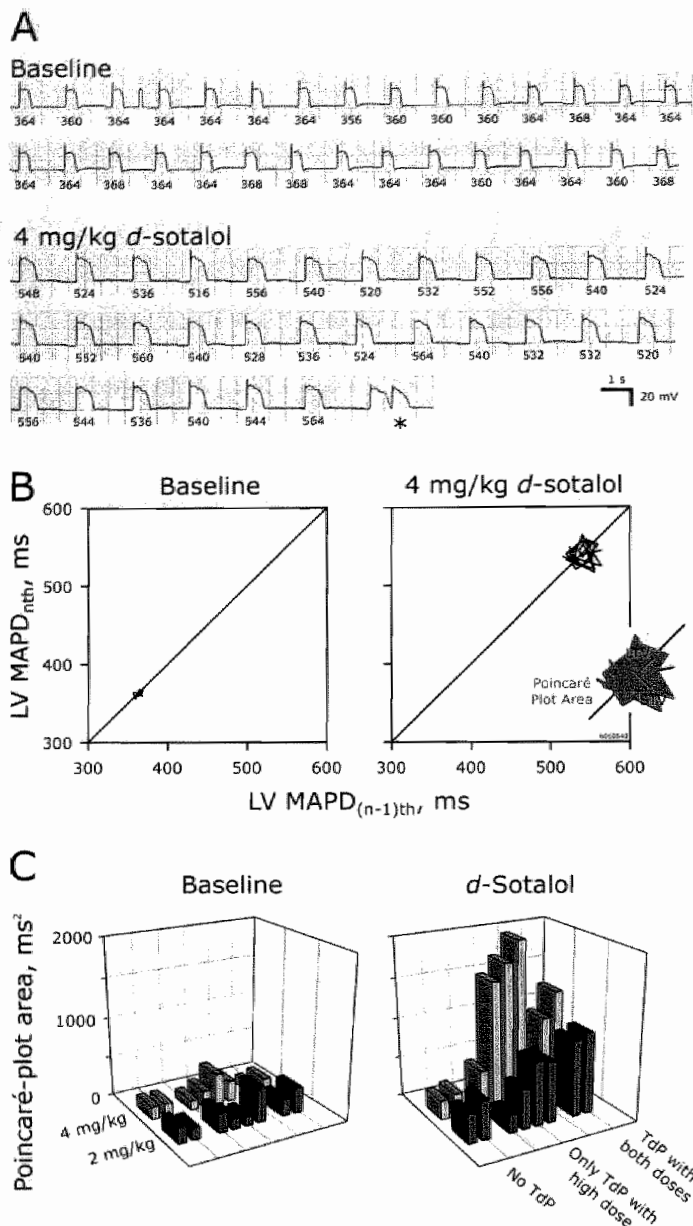
Transmembrane action potential durations to 95% repolarization were measured for 30 action potentials from isolated ventricular myocytes to calculate STV at baseline and before early afterdepolarizations (EADs) or at full  $I_{Kr}$  block.

### *Extrasystoles*

*d*-Sotalol-induced extrasystoles, defined as beats initiating before the end of the preceding T wave, were counted. Discrimination was made between couplets (Figure 2A) and multiples (Figure 2B), because the latter are considered more proarrhythmic.<sup>15</sup>

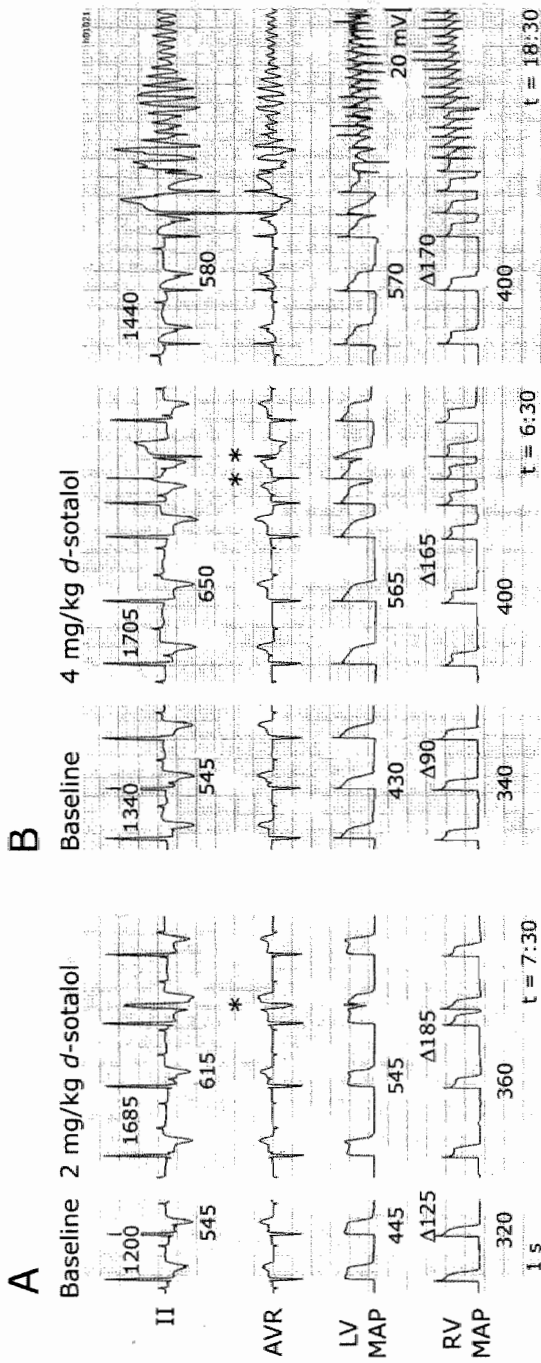
### *Statistical analysis*

Pooled data are expressed as mean  $\pm$  SD unless otherwise stated. Comparisons of EP and lability parameters were performed with a 2-way ANOVA followed by a paired Bonferroni comparison. Countables were tested with a Mann-Whitney rank sum test. Correlations were tested using Pearson product moment correlation. The area under the receiver-operator characteristics was used to assess predictive power of variables. Statistical difference was acknowledged at  $P < 0.05$ .



**Figure 1**

- A:** LV MAPD determination for 30 beats at baseline and after 4 mg/kg *d*-sotalol. After administration, LV MAPD is measured just prior to the first extrasystole (\*).
- B:** Respective Poincaré plots are shown. In association with increase in LV MAPD after *d*-sotalol, there is an expansion of plot area from 198 (left) to 1550 (right) ms<sup>2</sup>. Inset, schematic representation of Poincaré plot area (gray), STV and long-term variability (LTV).
- C:** Areas of LV MAPD Poincaré plot at baseline (left) and after *d*-sotalol (right). In each graph, the long axis represents each of the 8 dogs grouped after their proarrhythmia, with 2 mg/kg experiments in front. Mean area is significantly larger in dogs showing TdP.



**Figure 2**

Representative ECG tracings from two *d*-sotalol experiments in the same CAVB dog. Leads II and aVR are shown in combination with two ventricular MAP signals.  $\Delta$  indicates interventricular dispersion. ECG is calibrated to 1 cm/mV.

**A:** Baseline and first extrasystole (\*) induced by 2 mg/kg *d*-sotalol are shown.

**B:** Baseline, first (multiple) extrasystole (\*\*), and first TdP in experiment with 4 mg/kg are presented. EP parameters are comparable both at baselines and in the presence of *d*-sotalol.

## Results

### *EP and lability parameters*

Baseline EP and lability parameters were similar at the start of the two experiments (Table 1; Figure 1C). There was a dose-dependent difference in the induction of multiple extrasystoles (Table 1) and TdP after *d*-sotalol (2 of 8 after 2 mg/kg versus 6 of 8 after 4 mg/kg). *d*-Sotalol dose-independently prolonged the QT interval and the LV MAPD, which indicates their inability to provide an explanation for the higher TdP incidence at 4 mg/kg *d*-sotalol (Table 1). RR interval and RV MAPD were only significantly prolonged after 4 mg/kg *d*-sotalol; however, these values were not different from those seen with 2 mg/kg *d*-sotalol.

With regard to lability parameters in general, differences between drug treatments were only seen for LV plot area and LV STV (Figure 3; Table 1), while QT plot area and instability<sub>30</sub> were increased from baseline after the high dose. No changes were seen in the other lability parameters, such as all RR or RV MAPD plot areas or variability indexes (e.g. QTVI<sub>30</sub>; Table 1). No correlations were identified between RR plot areas and QT or LV plot areas ( $P = 0.7$  and  $0.4$ , respectively). Table 2 shows that the accuracy of individual predictions in the present study was considerably higher for LV plot area and STV than for temporally averaged QT or LV MAPD. Amiodarone treatment caused prolongation of repolarization (QT; control  $340 \pm 40$  ms, amiodarone  $470 \pm 75$  ms,  $P < 0.05$ ,<sup>3</sup>) whereas STV did not increase ( $2.4 \pm 0.2$  to  $2.4 \pm 0.4$  ms,  $P = \text{NS}$ ; Figure 3), in agreement with the total absence of TdP.

### *Poincaré-plot area or short-term variability*

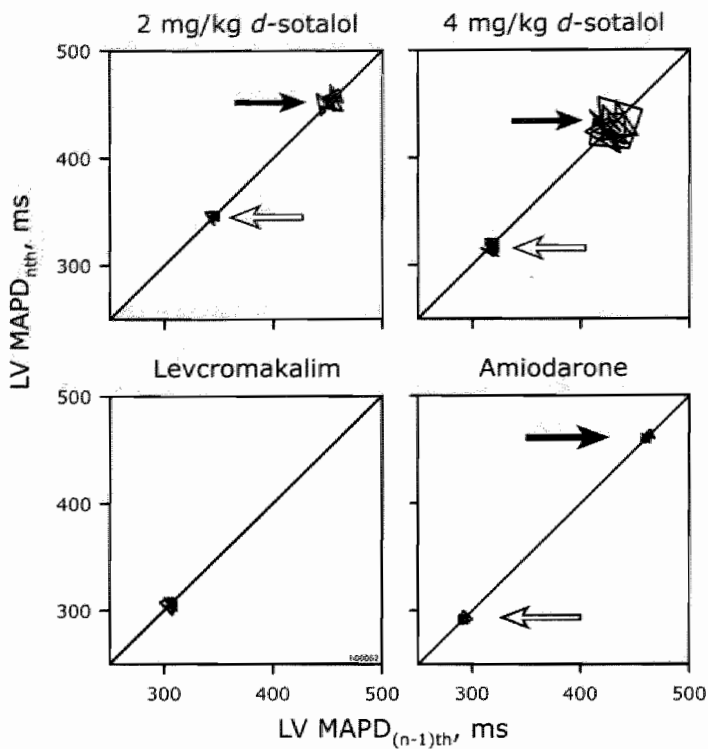
The advantage of STV over plot area is the feasibility to track its development over time by moving the 30-beats window. In Figure 4, this temporal behavior is shown for a representative dog. On average, half-maximal STV was reached  $2.9 \pm 1.3$  minutes earlier than the onset of ectopic beats ( $7 \pm 3$  minutes after start of *d*-sotalol) and  $10 \pm 6$  minutes earlier than the first TdP. All changes in LV STV and plot area were reversible upon  $I_{K,ATP}$  activation with levcromakalim (Figure 3).

In the cells treated with  $I_{Kr}$  blockers, 5 of 15 showed EADs, which divided the population. STV in baseline was similar in these two groups and increased upon  $I_{Kr}$  block (Figure 5). In the presence of  $I_{Kr}$  block, STV was significantly larger in the group with EADs, and the increased STV clearly preceded the occurrence of afterdepolarizations.

**Table 1.** Dose-specific d-sotalol-induced changes in 16 experiments in 8 dogs.

	Baseline 1	d-Sotalol 1 (2 mg/kg)	% Increase from baseline	Baseline 2	d-Sotalol 2 (4 mg/kg)	% Increase from baseline
RR, ms	1272 ± 233	1405 ± 236	10	1258 ± 180	1501 ± 273*	19
QT, ms	433 ± 40	511 ± 63*	18	437 ± 49	527 ± 58*	21
QT <sub>c</sub> , ms	410 ± 37	475 ± 60*	16	415 ± 47	484 ± 52*	17
LV MAPD, ms	393 ± 39	457 ± 49*	16	378 ± 57	464 ± 74*	23
RV MAPD, ms	334 ± 34	367 ± 19	10	325 ± 49	373 ± 36*	15
ΔMAPD, ms	59 ± 27	87 ± 48	47	52 ± 26	91 ± 48	75
RR plot area, ms <sup>2</sup>	479 ± 401	1046 ± 1086	118	527 ± 527	1470 ± 2301	179
QT plot area, ms <sup>2</sup>	448 ± 136	644 ± 333	44	610 ± 221	920 ± 431*	51
LV plot area, ms <sup>2</sup>	221 ± 104	623 ± 283*	182	193 ± 86	1076 ± 683*†	458
RV plot area, ms <sup>2</sup>	159 ± 81	169 ± 84	6	136 ± 76	193 ± 83	42
LV STV, ms	3.5 ± 1.5	5.5 ± 1.6	57	3.0 ± 0.7	8.6 ± 3.8*†	87
LV long-term variability, ms	4.3 ± 1.8	6.5 ± 2.1*	51	3.4 ± 0.5	7.9 ± 2.7*	32
QTVI <sub>30</sub>	0.7 ± 0.6	0.6 ± 1.0	-14	1.0 ± 0.7	0.6 ± 0.7	40
Instability <sub>30</sub> , ms	6.5 ± 3.7	10.0 ± 4.3	54	5.4 ± 2.7	13.0 ± 6.0*	41
Couplets	0	119 ± 137		0	172 ± 141	
Multiples	0	19 ± 28†		0	74 ± 109††	

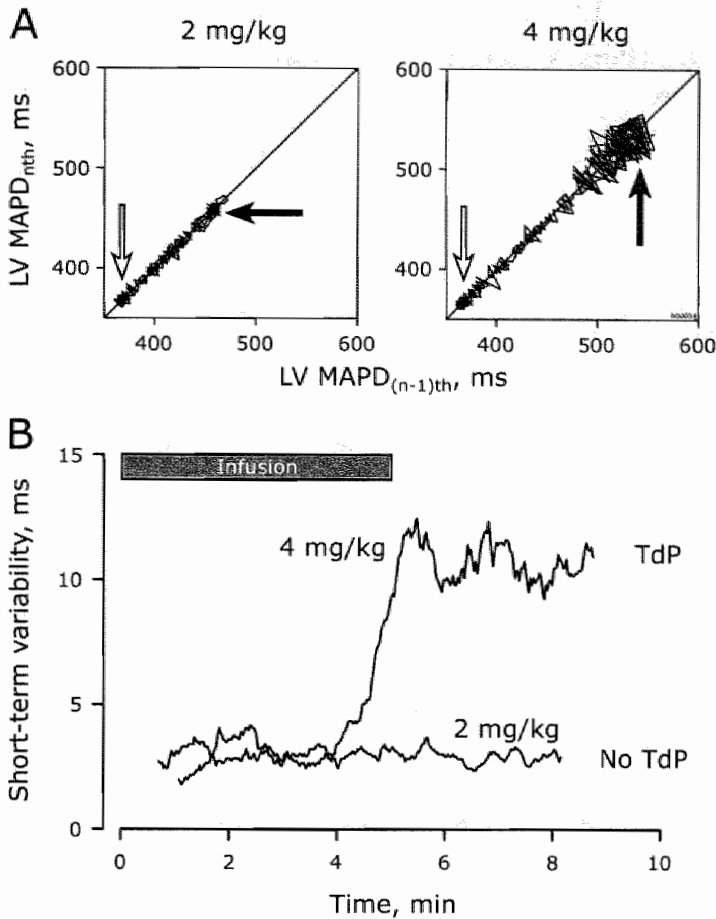
Numbers of couplets and multiples are totals during baseline and 30-minute follow-up. \*,  $P < 0.05$  versus baseline; †,  $P < 0.05$  versus d-sotalol 2 mg/kg; ††,  $P < 0.05$  versus couplets.



**Figure 3**  
Poincaré plots obtained from dogs under influence of various drugs. At baselines (open arrows), plots cluster around the diagonal where mean LV MAPD, plot area and STV are comparable in all experiments. After administration of drug (closed arrows), comparable prolongations of mean LV MAPD are observed for both doses of *d*-sotalol (serial experiments) and for amiodarone. Large plot area, STV and TdP are only seen after 4 mg/kg *d*-sotalol. Levocromakalim administered after 4 mg/kg *d*-sotalol decreased LV MAPD, plot area and STV to baseline levels, in line with total suppression of TdP. Amiodarone was not associated with TdP.

Table 2. Area under the receiver-operator characteristic plot for some study parameters.	
Mean RR, ms	0.78
Mean QT, ms	0.71
Mean LV MAPD, ms	0.70
LV Poincaré-plot area, ms <sup>2</sup>	0.97
LV STV, ms	0.94

Plots of receiver-operator characteristics depict sensitivity versus specificity of a variable to predict TdP irrespective of dose over a wide range of cutoff points. Perfect separation of the groups will have a sensitivity of 100% and specificity of 100% and hence an area of 1. The closer the area for a given parameter is to 1, the better its predictive performance.



**Figure 4**

**A:** Representative Poincaré plots from the same dog are shown to demonstrate development of BVR in two *d*-sotalol experiments from baseline (open arrows) to first extrasystole (closed arrow; 9 minutes 51 seconds and 9 minutes 22 seconds for 2 and 4 mg/kg, respectively).

**B:** Temporal development of STV obtained as 30-beat moving average of the above Poincaré plots. In the experiment with TdP, there is an instantaneous increase of STV 5 minutes after the start of *d*-sotalol administration. This is 14 minutes before TdP occurred.

## Discussion

### *Parameters indicative of proarrhythmia: Lability of repolarization*

Over the years, several EP parameters that set the stage for drug-induced TdP have been suggested. Prolongation of QT interval and increased spatial dispersion of



repolarization have been associated with TdP in patients<sup>19</sup> and in experimental models.<sup>3,7,13,15,20</sup> Still, the predictive power of these parameters is rather low (Table 2) and more sensitive methods have been sought.

As proposed by the groups of Berger<sup>11,21-23</sup> and Hondeghem,<sup>1,2</sup> lability of repolarization could bear important information to determine susceptibility to proarrhythmia in patients or to assess proarrhythmic potential of drugs. It is hypothesized that repolarization becomes labile when insufficient repolarization strength can be generated (decreased repolarization reserve<sup>12</sup>). For us, “lability of repolarization” includes all temporal assessments, regardless of whether they are gathered for strict beat-to-beat analyses (Poincaré plots), for subsequent calculations where the order of beats are rearranged (e.g. QTVI<sup>11</sup>), or for nonconsecutive determinations (e.g. instability<sup>1,2</sup>). We consider the term BVR to be restricted to the quantifications derived from Poincaré plots, in which direct beat-to-beat information is taken into account.

*Increased beat-to-beat variability of repolarization heralds torsades de pointes*

Occurrence of TdP is dependent on the simultaneous presence of a number of different factors. The necessary accumulated magnitude of these factors depends on the underlying substrate. Drugs antagonizing repolarization are examples of such factors. The proarrhythmic substrate consists of various predisposing factors, which may be described as decreases in repolarization reserve.

In the present study, similar values of LV STV and plot area were found at baseline regardless of the proarrhythmic outcome of the drug (Figure 1). Antagonizing repolarization by *d*-sotalol elevated LV STV and plot area in a pattern that corresponded to TdP incidence. Prevention of further TdP by the  $I_{K,ATP}$  opener levcromakalim returned LV STV and area to baseline levels, which indicates that strengthening of repolarization reserve by increasing outward current can decrease STV (Figure 3). The amiodarone data pointed in the same direction, because a prominent and comparable QT prolongation was seen as with other drugs, but LV STV remained low (Figure 3) and TdP was absent.<sup>3</sup>

When the experiments are arbitrarily grouped either by proarrhythmic outcome or by dose (Figure 6), it can be seen that the area of the LV Poincaré plot, which could be substituted with LV STV, is closely associated with TdP incidence. On the other hand, the QT interval was equally increased in all groups and did not correlate with TdP induction. The relationship between sensitivity and specificity of some parameters is illustrated in Table 2, which shows a higher predictive power for LV plot area and LV STV. As mentioned above, we prefer LV STV above plot area,

because relatively minor computational allocations facilitate online calculation of STV (Figure 4).

In the present study,  $QTVI_{30}$  did not provide similar information, whereas  $instability_{30}$  did, to some extent (Table 1). It must be emphasized that we adapted the two methodologies for our 30-beats comparison for methodological reasons.

Table 2 shows that BVR of the LV is superior to the regular EP parameters in the present study. Although not statistically different, one could read a trend toward a dose-dependent increase in RR plot area after *d*-sotalol (Table 1). There was no correlation between the LV plot areas and RR plot areas or regular RR intervals ( $P = 0.34$ ). Thus, any possible influence of heart rate is not evident in the phase before the onset of extrasystoles.

#### *Short-term variability is an early indicator of TdP*

In addition to EP and lability parameters, extrasystoles that cause short-long-short morphology of RR intervals has often been proposed as a signal for proarrhythmia.<sup>13,24</sup> Previously, we demonstrated that TdP can be induced reproducibly by pacing when *d*-sotalol does not provide the trigger.<sup>13</sup> In the present study, we have shown that the multiple extrasystoles appear dose dependently and at similar QT intervals but presumably at higher plasma or tissue levels of *d*-sotalol. Therefore, there appears to be a safety window (Figure 4) during which maximal repolarization times are reached before TdP ensues. If BVR increases, TdP is likely to follow. The increase in BVR before the onset of extrasystolic activity suggests a sequence of events that starts with prolongation of repolarization followed by increased BVR, and later, extrasystolic activity and TdP. Because prolongation of repolarization appears to be a dose-independent prerequisite, BVR is the earliest identified determinant of arrhythmias in the present study. Furthermore, it is illustrated (Figure 4) that an abrupt increase in STV occurs approximately at the end of the infusion, which leaves ~10 minutes response time to prevent TdP.

#### *Repolarization lability is confined to the left ventricle*

In contrast to the LV MAPD, the Poincaré plot area of the QT interval was only significantly increased after 4 mg/kg and was not different from that seen with 2 mg/kg *d*-sotalol (Table 1). The global nature of the QT interval versus the localized subendocardial LV MAP signal could illustrate regional lability of the LV, setting the stage for arrhythmias. Like discordant T-wave alternans,<sup>25</sup> anatomically adjacent regions of the LV with oscillating repolarization durations that are out of phase could

confer substantial dispersion, setting the stage for TdP. A MAP catheter registering one of these regions would show large BVR, whereas a global ECG would reveal the average repolarization time of all these regions and thus a relatively lower BVR.

#### *Cellular origin of BVR*

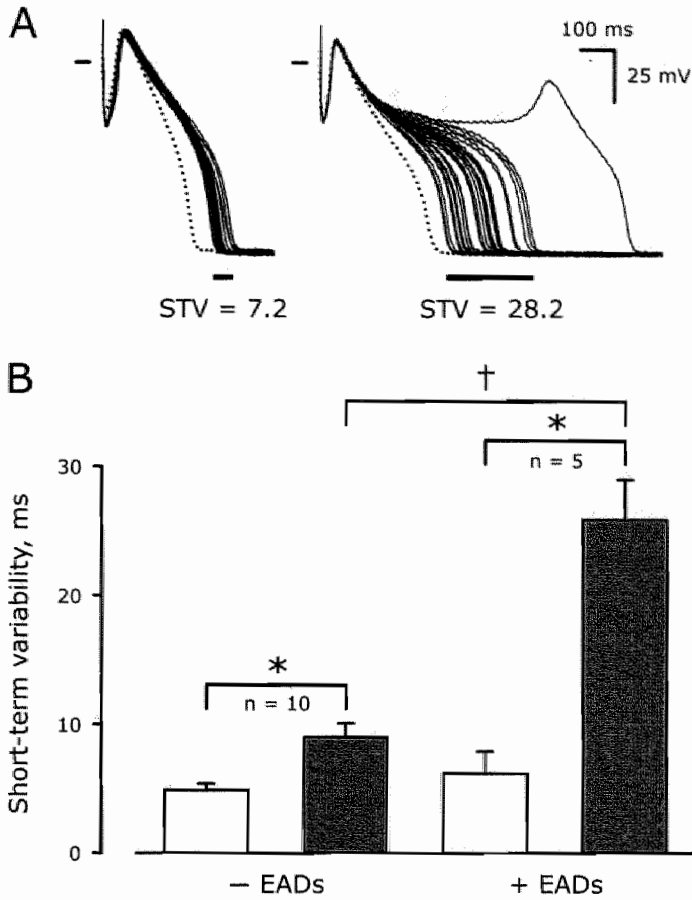
In vivo, we opted to measure BVR before ectopic beats were present. To answer the question of whether BVR has a cellular origin and appears before EADs, we performed single-cell experiments with  $I_{Kr}$ -blocking drugs. We noticed that these drugs increased STV and that STV was increased to higher levels in cells that demonstrated EADs (Figure 5). Hence, we suggest that BVR precedes EADs and that the higher the STV, the greater the likelihood for EADs.

#### *Clinical implications*

This study indicates that increased BVR precedes the induction of TdP arrhythmias in CAVB dogs. Cardiovascular and noncardiovascular drugs that induce TdP in patients with hidden predisposing factors are a major concern because identification of these patients is cumbersome.<sup>19</sup> Assessment of BVR could identify susceptible patients and provide a parameter together with QT intervals. Patients with congenital long-QT syndrome exhibit higher repolarization variability than unaffected family members, despite comparable heart-rate variabilities.<sup>26</sup> This suggests that lability of repolarization may be present both in acquired (drug induced) and hereditary repolarization-reserve deficiencies.

#### *Study limitations*

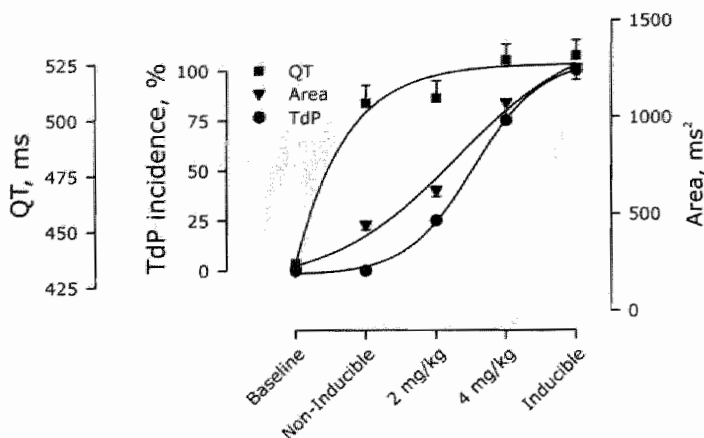
This study limits BVR to invasive, endocardial MAP recordings in anesthetized dogs with a high susceptibility for drug-induced TdP. Whether it can be applied to patients at risk for drug-induced TdP is unknown. It is also unknown whether other noninvasive signals can be used to quantify BVR. Before extrapolations between in vitro and in vivo BVR and proarrhythmia can be made, we must address numerous factors such as adrenergic drive, cellular coupling, electrolyte levels and changes in preload.



**Figure 5**

**A:** Thirty consecutive transmembrane action potentials recorded from two isolated RV myocytes from the same CAVB dog, one representing cells with (right) and without (left) EADs. Paced cycle length is 1500 ms before (dotted) and under the influence of 300 nM dofetilide (solid traces).

**B:** Composite data grouped according to presence of EADs at  $I_{Kr}$  block. STV was measured at baseline (open bars) and during maximal  $I_{Kr}$  block before first EAD (right) or at a comparable point in time (left). \*,  $P < 0.05$  versus baseline; †,  $P < 0.05$  versus absence of EADs. Error bars indicate SEM.



**Figure 6**

Graph summarizing the findings of the *d*-sotalol investigation. Proarrhythmic outcome of the study has been grouped in different arbitrary ways: baseline of 16 experiments, 8 experiments with no TdP irrespective of dose (noninducible: 6 experiments with 2 mg/kg, 2 experiments with 4 mg/kg), 8 dogs receiving 2 mg/kg *d*-sotalol (25% TdP), the same 8 dogs receiving 4 mg/kg (75% TdP) and 8 experiments with 100% TdP incidence irrespective of dose (inducible: 2 experiments with 2 mg/kg, 6 experiments with 4 mg/kg). TdP incidences (●) are closely associated with BVR (▼), whereas QT intervals (■) are not. Sigmoidal fits are for illustration purposes only. Mean  $\pm$  SEM.

### Conclusions

The presence or absence of proarrhythmia is not related to differences in prolongation of repolarization parameters but corresponds with BVR, such as STV of LV MAPD. The increase in STV occurred before extrasystoles *in vivo* and EADs *in vitro*, which indicates that STV is a candidate parameter to predict drug-induced TdP.

### Acknowledgments

M.B. Thomsen and S.C. Verduyn were financially supported by H. Lundbeck, Denmark and Janssen Research, Belgium, respectively. P.G.A. Volders was supported by The Netherlands Organization for Health and Development (ZonMw 906-02-068).

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# Decreasing the Infusion Rate Reduces the Proarrhythmic Risk of NS-7

- Confirming the relevance of short-term  
variability of repolarisation in predicting  
drug-induced torsades de pointes

Elke Detre<sup>1</sup>, Morten B. Thomsen<sup>1,2</sup>, Jet D.M. Beekman<sup>1,2</sup>, Karl-Uwe Petersen<sup>3</sup> and  
Marc A. Vos<sup>1,2</sup>

1. Department of Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands.
2. Department of Medical Physiology, University Medical Center Utrecht, Utrecht University, Netherlands.
3. PAION, Aachen, Germany.



**Abstract**

The rate of infusion has been suggested to be important for drug-induced torsades de pointes arrhythmias (TdP). We investigated the repolarisation-prolonging effects and proarrhythmic properties of NS-7, a neuroprotective drug in development, using two different infusion rates. A fast (5 minutes i.v.) escalating dosing regime (0.3 and 3.0 mg/kg,  $n = 4$ ) of NS-7 was investigated in anaesthetised control dogs in sinus rhythm (SR). This was compared to a slow infusion (60 minutes i.v.) of one dose (3.0 mg/kg,  $n = 4$ ) NS-7. The similar dosing regimes were investigated in anaesthetised dogs with chronic, complete AV block (CAVB), an animal model of TdP ( $n = 6$ ). No electrophysiological effects were seen after 0.3 mg/kg NS-7. Fast infusion of 3.0 mg/kg caused prolongation of repolarisation, e.g.  $QT_c$  interval: in SR:  $6 \pm 1\%$ ; in CAVB:  $10 \pm 7\%$ , which was accompanied by TdP in 3 of 6 CAVB dogs. No TdP were seen in SR dogs. Slow infusion did not cause TdP in the same CAVB dogs, although NS-7 caused repolarisation to prolong with a similar magnitude ( $QT_c$ :  $12 \pm 7\%$ ) as in the fast-infusion experiment. Short-term variability (STV) is a novel parameter for the prediction of drug-induced TdP analysing the beat-to-beat variability of repolarisation. STV was only increased after the fast infusion in CAVB dogs ( $2.6 \pm 0.3$  versus  $6.0 \pm 1.4$  ms,  $P < 0.05$ ), while there was no increase ( $2.1 \pm 0.2$  versus  $2.5 \pm 1.0$  ms) after the slow infusion of NS-7. Peak plasma concentrations attained were lower in slow ( $0.5 \pm 0.1$   $\mu\text{g/ml}$  after 50 minutes) than in fast infusion regimen ( $2.1 \pm 0.4$   $\mu\text{g/ml}$  after 5 minutes;  $P < 0.05$ ). The results support the conclusion that limiting peak plasma concentration by decreasing the rate of infusion of NS-7 reduces the proarrhythmic risk despite comparable prolongation in repolarisation parameters. The relevance of STV in predicting drug-induced TdP was confirmed.

## Introduction

A large number of cardiovascular and non-cardiovascular drugs have been withdrawn from the market in the past decade due to post-marketing reports of clinical drug-induced lethal proarrhythmia.<sup>1-3</sup> Most of these drugs have in common, that they delay the ventricular repolarisation seen as QT prolongation on the ECG.<sup>1,2</sup> However, numerous studies have shown that there is no straightforward relation between prolongation of repolarisation and the potentially lethal arrhythmia known as torsades de pointes (TdP).<sup>4-11</sup> Still, the regulatory authorities require that any new potential drug is investigated to determine both its repolarisation delaying and proarrhythmic properties.

NS-7 (enecadine) is a multichannel blocker ( $I_{Na}$ ,  $I_{Ca}$  and  $I_{K1}$ ) reported to show promising efficacy in animal models of ischemic stroke.<sup>12-17</sup> In preclinical electrophysiological studies, 100  $\mu$ M NS-7 prolonged the ventricular action potential in guinea pigs.<sup>18</sup> In the present study, the electrophysiological and proarrhythmic characteristics of the drug were assessed in anaesthetised dogs with normal and electrically remodelled hearts. For the latter purpose, we used the animal model with chronic, complete atrioventricular block (CAVB) that shows a high susceptibility to drug-induced TdP.<sup>8,19-23</sup>

Previously, the rate of drug administration has been shown to be critical for TdP induction at similar prolongation of the QT intervals in rabbits.<sup>7</sup> Infusion rate has later been included as a risk factor for TdP observed in the clinical setting.<sup>24</sup> Therefore, we employed two different infusion rates of the same total dose in this investigation, along with analysis of beat-to-beat variability of repolarisation (BVR). This methodology was recently demonstrated to be a superior predictor for drug-induced TdP in the preclinical setting.<sup>4,9</sup>

## Methods

Animal handling was in accordance with the European directive for the protection of vertebrate animals used for experimental and other scientific purposes (86/609/EU). The committee for experiments on animals of Maastricht University approved all experiments.

*General*

A total of 28 experiments were performed on 14 anaesthetized mongrel dogs (body weight 22-33 kg) under aseptic conditions. After overnight fasting, anaesthesia was induced by 20 mg/kg sodium pentobarbital i.v. and maintained by 0.5% halothane in a mixture of O<sub>2</sub> and N<sub>2</sub>O (1:2). During artificial ventilation at a frequency of 10-12 per minute, tidal volume (10-15 ml/kg) was adjusted to maintain end-expired CO<sub>2</sub> concentration between 3.5 and 4.0%. A thermal mattress was used to maintain body temperature. To prevent volume depletion, the dog received 0.5 to 1.0 litre 0.9% saline i.v. Postoperative care included antibiotics (1 g ampicillin i.m.) and analgesics (15 µg/kg buprenorphine i.m.).

Ten ECG leads and 2 monophasic action potentials (MAP) were recorded continuously throughout the experiments. MAP catheters (EP technologies, CA) were placed under fluoroscopic guidance on the endocardium of the left and right ventricle. MAP signals were amplified with a customized isolated DC-coupled differential amplifier at a frequency range of 0-500 Hz with a 20-mV calibration pulse. The offset of the amplifier was variable and could be adjusted to the recorded signal. Besides minimal amplitude of 15 mV the MAP was required to have a smooth repolarisation and a stable configuration in time.

*Experimental design*

Eight dogs were studied during SR to determine 1) the dose-dependent electrophysiological effects of NS-7 in physiologically normal hearts, and 2) the associated plasma concentrations of NS-7. NS-7 was administered at a fast infusion (5 minutes) scheme of escalating doses (0.3, 3.0 and 10 mg/kg i.v.; n = 4) separated by 30 minutes. Furthermore, a slow infusion (60 minutes) scheme of 3.0 mg/kg (i.v.; n = 4) was performed.

In 9 dogs, complete atrioventricular block was created by radiofrequency ablation. After  $4 \pm 1$  weeks of atrioventricular block, the dogs underwent an anaesthetized dofetilide-inducibility test (25 µg/kg i.v.) to determine their sensitivity to drug-induced TdP.<sup>25</sup> Because NS-7 could have a low proarrhythmic potential that could escape detection in this model, we opted to exclude dogs that were not susceptible to this positive control.<sup>8</sup> Of 9 dogs with CAVB two failed the dofetilide-inducibility test and one was lost due to drug-induced ventricular fibrillation. Thus, 6 dogs were used for evaluating the electrophysiological and proarrhythmic properties of NS-7 in remodelled hearts.

NS-7 was administered in a fast infusion (5 minutes) scheme of escalating doses

Infusion rate, beat-to-beat variability and torsades de pointes (0.3 and 3.0 mg/kg i.v.) separated by 30 minutes or in a slow infusion (60 minutes) scheme of 3.0 mg/kg (i.v.). This was performed in a serial, random crossover design with 2 weeks between experiments. One dog was lost during a fast-infusion experiment, before the slow-infusion experiment was performed.

In two dogs, the dofetilide challenge was repeated after NS-7 to ascertain preservation of TdP inducibility. NS-7 and dofetilide were provided by PAION. Both drugs were dissolved in equal volumes of 0.9% saline.

### *Plasma concentrations*

Blood samples were drawn from a dedicated venous access at various time points throughout the experiments. Samples were collected in citrate tubes, centrifuged for 10 minutes at 4000 rpm at 4°C and stored at -20°C. NS-7 concentrations were determined by Scope International (Hamburg, Germany).

### *Data analysis*

Applying a custom-made computer programme (ECGview), we measured the following parameters offline at a resolution of 4 ms: RR and QT intervals from a unipolar lead positioned on the sixth intercostal space near the edge of the sternum.<sup>26</sup> Also, the left (LV) and right ventricular (RV) monophasic action potential duration (MAPD) to 50 and 100% repolarisation was determined (MAPD<sub>50</sub> and MAPD<sub>100</sub>, respectively). Heart-rate corrected QT intervals were calculated according to van de Water's formula.<sup>27</sup> Interventricular dispersion of repolarisation ( $\Delta$ MAPD) was defined as LV minus RV MAPD.

Beat-to-beat variability of repolarisation was determined according to an earlier publication.<sup>9</sup> Briefly, Poincaré plots were drawn from 30 consecutive LV MAPD and short-term variability ( $STV = \sum |D_{n+1} - D_n| / [30 \cdot \sqrt{2}]$ , where  $D_n$  represents LV MAPD of beat number  $n$ ), representing the mean orthogonal distance to the line-of-identity, was calculated.

All electrophysiological parameters were measured at maximal QT prolongations, which were 10 and 60 minutes after start of the fast and slow infusion, respectively. The frequency of multiple extrasystoles was quantified in 10-minutes intervals after the administration of NS-7 in CAVB dogs. Extrasystoles were defined as premature ventricular complexes occurring at a coupling interval of less than 600 ms.

TdP was defined as polymorphic ventricular tachycardia of at least 5 beats. A dog was defined as inducible when >3 TdP occurred. If a TdP degenerated into ventricular fibrillation, electrical cardioversion was applied.

Pooled data are expressed as mean  $\pm$  SD unless otherwise stated. Comparisons of electrophysiological data were performed with repeated-measures ANOVA followed by a Bonferroni t-test. Statistical significance was acknowledged at  $P < 0.05$ .

## Results

### *Fast-infusion scheme in control SR dogs*

Infusing NS-7 over 5 minutes resulted in a dose-dependent increase in RR interval (baseline:  $460 \pm 50$  ms; 0.3 mg/kg:  $475 \pm 35$  ms; 3 mg/kg:  $530 \pm 70$  ms ( $P < 0.05$ ) and 10 mg/kg:  $540 \pm 25$  ms ( $P < 0.05$ )). Prolongation of electrophysiological repolarisation parameters was seen only after the higher doses of 3.0 and 10 mg/kg (Figure 1 for  $QT_c$  time and Table 1 for 3.0 mg/kg). Relatively, 3 mg/kg NS-7 caused a  $5.8 \pm 1\%$  prolongation of the  $QT_c$  interval from baseline, whereas 10 mg/kg caused a  $12.6 \pm 2\%$  prolongation. The plasma concentrations over the duration of the experiments are depicted in Figure 1, at peak reaching  $0.2 \pm 0.02$ ,  $2.1 \pm 0.4$  and  $6.4 \pm 3.1$   $\mu\text{g/ml}$  after 0.3, 3.0 and 10 mg/kg NS-7, respectively.

**Table 1.** Electrophysiological data from anaesthetised dogs with normally conducted sinus rhythm ( $n = 4$ ).

	Control	NS-7
RR, ms	$460 \pm 50$	$530 \pm 70^*$
QT, ms	$265 \pm 15$	$290 \pm 20^*$
$QT_c$ , ms	$310 \pm 10$	$330 \pm 15^*$
LV MAPD, ms	$215 \pm 5$	$230 \pm 15^*$
RV MAPD, ms	$210 \pm 5$	$225 \pm 5^*$
$\Delta\text{MAPD}$ , ms	$5 \pm 5$	$5 \pm 5$
STV, ms	$0.8 \pm 0.1$	$1.0 \pm 0.4$

Measurements were performed 10 minutes after the start of the 5-minutes infusion of 3.0 mg/kg NS-7 when the QT was maximally prolonged. \*,  $P < 0.05$  versus control.

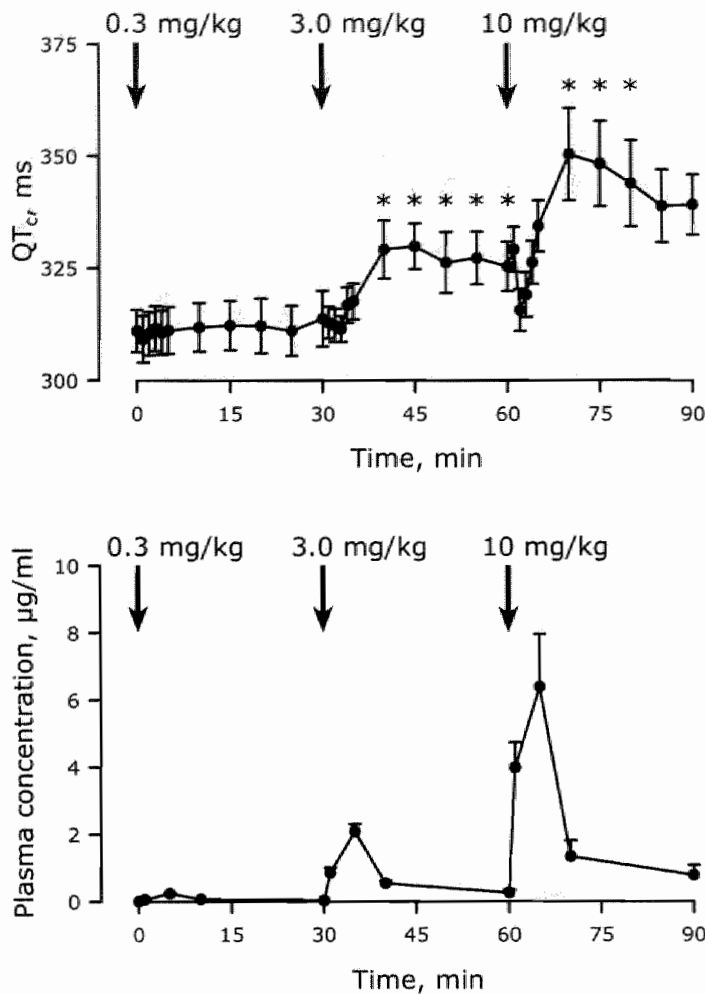
Administration of 10 mg/kg NS-7 caused a brief fall in the  $QT_c$  interval (figure 1) attributable to a consistent drug-induced transient shortening of the RR interval from  $510 \pm 45$  to  $440 \pm 20$  ms ( $P < 0.05$ ). No statistically significant drug-induced increase was seen in the interventricular dispersion ( $\Delta\text{MAPD}$ ) or beat-to-beat variability of repolarisation (STV, Table 1).

*Fast-infusion scheme in proarrhythmic CAVB dogs*

0.3 mg/kg NS-7 caused no proarrhythmia, while 3.0 mg/kg caused reproducible TdP in 3 of 6 CAVB dogs, associated with a  $QT_c$  prolongation of  $1.8 \pm 1\%$  and  $10.3 \pm 7\%$ , respectively. After the fast infusions, the peak plasma concentrations of NS-7 in CAVB dogs ( $0.2 \pm 0.01$  and  $1.6 \pm 1.9$   $\mu\text{g/ml}$  after 0.3 and 3.0 mg/kg NS-7, respectively) were similar to those seen in SR dogs. A representative example of TdP caused by 3.0 mg/kg NS-7 is shown in Figure 2. Representative Poincaré plots of the  $LVMAPD_{100}$  at control and under the influence of 3.0 mg/kg NS-7, either at fast or slow infusion, are also shown in Figure 2. Table 2 summarizes the electrophysiological changes induced by 3.0 mg/kg NS-7. During fast infusion of 3.0 mg/kg NS-7, significant increases in LV  $MAPD_{100}$  and STV were observed. On average  $9 \pm 20$  multiple extrasystoles were encountered within the first ten minutes after administration. One dog was lost after a drug-induced ventricular fibrillation where electrical cardioversion was not feasible.

*Slow-infusion scheme in control SR dogs*

Administering 3.0 mg/kg NS-7 over 60 minutes caused an increase in RR ( $550 \pm 55$  versus  $625 \pm 40$  ms;  $P < 0.05$ ). The  $QT_c$  interval was prolonged to a similar extent as with the fast infusion scheme ( $8.1 \pm 2$  versus  $5.8 \pm 1\%$ ; Figure 3). The maximal values were reached 60 minutes after the start of the slow infusion versus 10-15 minutes in the fast-infusion experiments. The corresponding plasma concentrations of NS-7 (Figure 3) show significant differences in peak levels ( $0.5 \pm 0.1$  versus  $2.1 \pm 0.4$   $\mu\text{g/ml}$  for slow and fast infusion, respectively;  $P < 0.05$ ).



**Figure 1**  
Dose-dependent development in QT<sub>c</sub> interval and plasma concentration after 5-minutes infusions of NS-7 in anaesthetized dogs in sinus rhythm. Three cumulative doses of NS-7 were administered i.v. as indicated by arrows (n = 4 dogs). \*, *P* < 0.05 versus value before last administration. Mean ± SEM.

**Table 2.** Electrophysiological data from serial investigations in anaesthetised dogs with CAVB (n = 5).

	5-minutes infusion		60-minutes infusion	
	Control	NS-7	Control	NS-7
RR, ms	1240 ± 155	1300 ± 115	1255 ± 215	1370 ± 275
QT, ms	440 ± 45	480 ± 50	450 ± 30	495 ± 50
QT <sub>c</sub> , ms	420 ± 40	450 ± 45	425 ± 20	460 ± 30
LV MAPD <sub>100f</sub> , ms	365 ± 50	420 ± 40*	350 ± 10	410 ± 55*
LV MAPD <sub>50f</sub> , ms	285 ± 30	325 ± 50	275 ± 15	295 ± 50
RV MAPD <sub>100f</sub> , ms	300 ± 35	345 ± 35	295 ± 30	340 ± 55
RV MAPD <sub>50f</sub> , ms	245 ± 40	280 ± 35	240 ± 35	280 ± 25
ΔMAPD <sub>100f</sub> , ms	65 ± 40	75 ± 45	55 ± 30	70 ± 10
ΔMAPD <sub>50f</sub> , ms	40 ± 25	45 ± 45	35 ± 30	15 ± 50
STV LV MAPD <sub>100f</sub> , ms	2.6 ± 0.3	6.0 ± 1.4*	2.1 ± 0.2	2.5 ± 1.0†
STV LV MAPD <sub>50f</sub> , ms	2.1 ± 0.7	4.9 ± 1.6*	1.9 ± 0.6	2.1 ± 0.5†

3.0 mg/kg NS-7 was administered over 5 minutes or over 60 minutes. Measurements were performed at 10 and 60 minutes, respectively, when the QT was maximally prolonged.

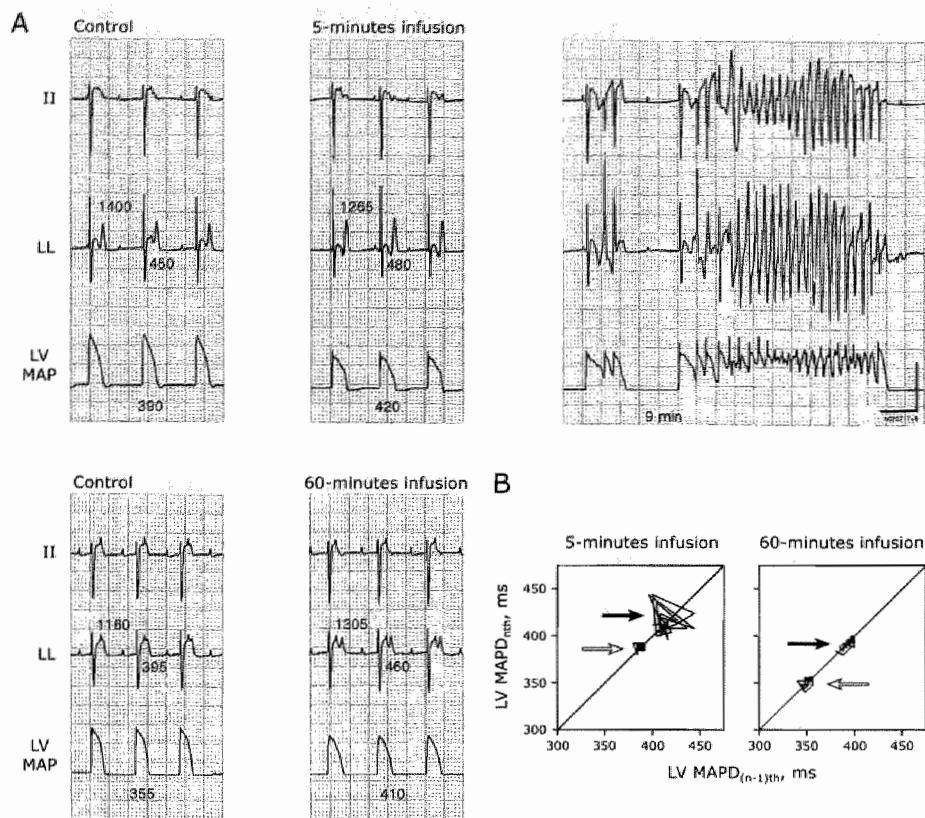
\*,  $P < 0.05$  versus control; †,  $P < 0.05$  versus 5-minutes infusion.

#### *Slow-infusion scheme in proarrhythmic CAVB dogs*

As opposed to the fast-infusion scheme, slow infusion of 3.0 mg/kg caused no TdP although the LV MAPD and QT<sub>c</sub> time ( $11.9 \pm 9\%$  versus  $10.3 \pm 7\%$ ) were prolonged to similar extents (Table 2). The plasma concentration of NS-7 was similar in CAVB and SR dogs after the slow infusions ( $0.4 \pm 0.1$  µg/ml after 3.0 mg/kg NS-7). STV was not altered by the slow infusion of NS-7. Furthermore, STV was significantly higher after a fast administration of 3.0 mg/kg NS-7 than after a slow infusion of the same dose (Table 2). No multiple extrasystoles were observed, however this was not acknowledged as statistically significantly different from the fast infusion, partly due to the very large variation in the frequency in the latter experiments.

Reproducibility of TdP induction with dofetilide in time was confirmed in two experiments.

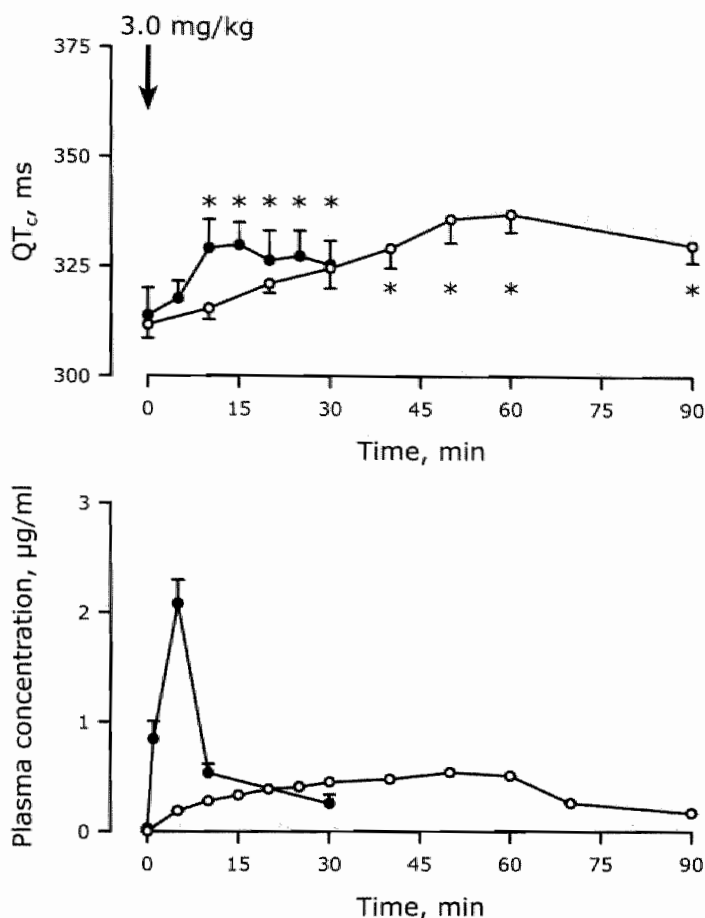




**Figure 2**

**A:** Representative ECG traces before and after administration of 3.0 mg/kg NS-7 in an anaesthetized dog with CAVB. TdP (right-most panel) only occurred after the fast infusion of NS-7. Two ECG leads (II, lead II; LL, precordial lead placed on the left lateral side of the thorax) and LV MAP recordings are shown in each trace. RR intervals are above and QT time below lead LL. MAPD<sub>100</sub> is below the LV MAP trace. ECG calibrated to 1 mV/cm. Vertical scale bar, 20 mV on the MAP signal. Horizontal scale bar, 1 s.

**B:** Poincaré plots of the LV MAPD<sub>100</sub> from the same dog at the two experiments. Open arrow, control. Closed arrow, 3.0 mg/kg NS-7. A substantial increase in plot area is appreciable after fast administration, but not after the slow administration. STV in the fast-infusion experiment increases from 3.0 ms at control to 8.8 ms after NS-7, while STV changes from 2.3 ms to 2.1 ms in the slow-infusion experiment.



**Figure 3**

Comparison of the 5 and 60-minutes infusion of 3.0 mg/kg NS-7 in anaesthetized dogs in sinus rhythm. QT<sub>c</sub> (upper panel) and plasma concentration (lower panel) are depicted over time for the slow (open circles) and the fast (closed circles) i.v. infusion experiments (n = 4 dogs). QT<sub>c</sub> in similarly increased after both infusion schemes, however peak plasma concentrations are higher after the fast infusion. \*, *P* < 0.05 versus 0 minutes. Mean ± SEM.

## Discussion

In this study, we show that decreasing the infusion rate of NS-7 limits the peak plasma concentration and decreases or abolishes the risk of TdP. The only electrophysiological parameter that reflected absence of TdP was beat-to-beat variability of repolarisation, quantified as STV. This confirms the inability of the prolonged QT interval to predict TdP. Furthermore, this study stresses the importance of assessing cardiac electrophysiological safety of drugs in animal

models of reduced repolarisation reserve, because the same dose of NS-7 did not cause proarrhythmia in SR dogs.

#### *Proarrhythmic assessment of NS-7*

NS-7 is under development as a neuroprotective drug after ischemic stroke. The beneficial actions of the drug are thought to be based on block of voltage-activated sodium and calcium channels in neuronal tissue.<sup>12,13,28</sup> Block of  $I_{Kr}$  ( $IC_{50}$ : 0.4  $\mu$ M; PAION; data on file) may underlie the prolongation of action potential duration observed in the present study and in isolated guinea-pig ventricular myocytes.<sup>18</sup> Specifically, block of  $I_{Kr}$  has been associated with an increased risk of repolarisation-dependent proarrhythmia.<sup>3</sup>

Regulatory authorities like the U.S. Food and Drug Administration or the European Medicines Agency encourage that all potential drugs with suspected QT prolonging properties in humans should be tested pre-clinically for their ability to delay repolarisation and for their proarrhythmic characteristics. Drug testing in normal hearts is essential for the analysis of delayed repolarisation in general, however it is not sufficient for the recognition of potential proarrhythmic effects in the diseased heart of a predisposed, vulnerable individual patient. The canine model with CAVB is known to have acquired QT prolongation and a predisposition to TdP and sudden cardiac death.<sup>8,20,22,25,29</sup> The CAVB dogs exposed to NS-7 in this investigation were selected on the basis of a positive dofetilide-inducibility test, increasing the sensitivity of the model.<sup>8</sup> The incidence of dofetilide-induced TdP was 7 of 9 dogs, comparable to earlier investigations,<sup>8,25</sup> and was reproducible in the two dogs which were retested after the NS-7 experiments had been performed.

To be able to compare NS-7 to other drugs in this animal model, we chose our regular infusion time of 5 minutes as the fast rate.<sup>8,20,25</sup> In an approach to the clinical setting, the slow infusion went over a period of 60 minutes, which is still faster than the anticipated rate in humans.

To the best of our knowledge, this is the first study to report prolonged cardiac repolarisation and proarrhythmia by NS-7 in the intact animal. A dose-dependent prolongation of the  $QT_c$  interval is appreciable after fast administration of NS-7 in both normal (Figure 1) and CAVB dogs. Peak plasma concentrations clearly exceeded the putative effective therapeutic plasma concentration of 15 to 29 ng/ml.<sup>30</sup> TdP was only seen after fast infusion of 3.0 mg/kg NS-7 in the remodelled hearts of the CAVB dog. The highest dose (10 mg/kg) was not administered to CAVB dogs, as TdP were already evident at 3.0 mg/kg.

*Relevance of infusion time*

As expected, peak plasma concentrations were markedly lower during slow than during fast infusion. Even so, prolongation of the infusion time did not reduce the effects seen on  $QT_c$  intervals, LV MAPD or interventricular dispersion, neither in control dogs (Figure 3 for  $QT_c$ ) nor in CAVB dogs (Table 2). On the other hand, proarrhythmia was completely absent during the slow infusion. Thus, at two different plasma concentrations of NS-7, repolarization was similarly prolonged, suggesting that a certain drug concentration is sufficient to produce the observed prolongation of repolarisation, but a higher concentration is necessary to destabilise repolarisation, trigger ectopic beats and sustain TdP. This vulnerability is likely restricted to areas of lowest repolarisation reserve.<sup>31</sup> In the CAVB dog, these areas seem to be located in the subendocardial regions of the left ventricle.<sup>9</sup>

Our data confirms the finding of Carlsson et al.<sup>7</sup> who showed that a fast infusion of the  $I_{Kr}$  blocker almokalant (25 nmol/kg/min) produced TdP in 9 of 10 methoxamine-treated anaesthetised rabbits, while a slow infusion (5 nmol/kg/min) gave an inducibility of 1 of 8. This was associated with a 42% increase in  $QT_c$  after the slow infusion but only 30% prolongation after the fast infusion, once more confirming that QT prolongation is not directly convertible into risk of TdP, a conclusion reached by numerous groups.<sup>4,6,9-11</sup> We have compared amiodarone and its non-iodinated successor, dronedarone, in chronically dosed CAVB dogs and demonstrated equal QT prolongations, contrary to a different proarrhythmic outcome.<sup>6</sup> Similar conclusions were drawn from dose-dependent investigations employing the antipsychotic drug, sertindole or the antiarrhythmic drug, *d*-sotalol.<sup>8,9</sup> In isolated rabbit hearts, Hondeghem et al.<sup>4</sup> showed that parameters like instability and triangulation of the action potential were proarrhythmic while action potential prolongation was antiarrhythmic. In a comparison between the macrolide antibiotics erythromycin, clarithromycin, and azithromycin, it was shown that they all caused similar increases in repolarisation duration, however only the latter was devoid of proarrhythmia.<sup>10</sup> Other antibiotics like gatifloxacin and moxifloxacin have developed TdP in conscious CAVB dogs despite the absence of drug-induced QT prolongation.<sup>19</sup> Moreover, the experimental calmodulin inhibitor W-7 was able to suppress drug-induced TdP without shortening QT intervals.<sup>32,33</sup>

*Beat-to-beat variability of repolarisation*

Repolarisation reserve has been introduced as a concept to explain susceptibility to arrhythmia.<sup>31,34</sup> A reduction in repolarisation reserve generates an action

potential that is more vulnerable to additional challenges upon repolarisation, such as drugs with  $I_{Kr}$  blocking properties. Often  $I_{Kr}$  blockers are the final challenge on repolarisation, which unmasks an unidentified predisposition precipitating a lethal arrhythmia. This predisposition can be a congenital (long QT syndrome) or an acquired (metabolic or electrolyte disturbances, heart disease etc.) ion channelopathy. Quantification of the repolarisation reserve and identification of the vulnerable patient are therefore important questions for many investigators.

Beat-to-beat variability of repolarization is a concept that provides data to identify unsafe drugs. With the use of Poincaré plots, STV is one way of quantifying BVR. A dose-dependent TdP occurrence after *d*-sotalol was tightly associated with the elevation of STV, while the absence of TdP after chronic, oral amiodarone was reflected in an unchanged STV.<sup>9</sup> The global nature of the QT interval versus the relatively local recording of an MAP signal possibly explains the low predictive power of beat-to-beat variability of the QT interval. Furthermore, the predominant remodelling of the left ventricle may underlie the absence of drug-induced increases in the BVR of the RV MAPD.<sup>9</sup> With the assumption that it is a population of cells located in the left ventricular sub-endocardium that has the lowest repolarisation reserve, we would not expect to find physiologically significant drug-induced increases of the STV of the epicardial repolarisation.<sup>35</sup> This is the first study to show, that within the STV of the LV MAPD, variability is present at both 50% and 100% repolarisation levels, supporting the hypothesis that BVR arises at the plateau of the action potential rather than at the fast repolarisation.

In the present study, we have applied STV and confirmed our earlier observation, that an increase in BVR predicts TdP. The only NS-7 induced increase in STV was observed in the fast-infusion experiments in the remodelled CAVB dogs.

In normal hearts as well as with the slow infusion of NS-7 in CAVB dogs, STV was not altered and TdP was absent. Thus, BVR is an attractive addition to assess proarrhythmic actions of drugs. Additionally, STV is present prior to drug-induced early afterdepolarisation and extrasystoles, which allows time for preventive antiarrhythmic actions.

#### *Novel parameters in drug screening*

In vivo, repolarisation-dependent arrhythmias have been associated with a QT variability index in humans<sup>36</sup> and with triangulation, spatial dispersion and instability of the MAPD and reverse-use dependency of the drug in isolated rabbit hearts.<sup>4</sup> Transmural dispersion of repolarisation in arterially perfused canine left ventricular wedge preparations also has predictive value in proarrhythmic drug testing.<sup>37,38</sup>

Short-term variability of repolarisation differs from other measures of temporal lability of repolarisation in its consecutiveness. The former evaluates the direct difference between two consecutive beats while QT variability index and instability rearranges the order of beats.

### *Conclusions*

Limiting peak plasma concentrations of NS-7 by decreasing the infusion rate reduces the proarrhythmic risk in dogs with remodelled hearts considerably. This occurs despite similar prolongations of the repolarisation parameters, like QT intervals. Conversely, an increase in short-term variability of MAPD predicted the proarrhythmic outcome.

### **Acknowledgments**

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# Sudden Cardiac Death in Dogs with Remodeled Hearts is Associated with Larger Beat-To-Beat Variability of Repolarization

Morten B. Thomsen<sup>1,2</sup>, Michiel Truin<sup>1</sup>, Jurren van Opstal<sup>1</sup>, Jet D.M. Beekman<sup>1,2</sup>, Paul G.A. Volders<sup>1</sup>, Milan Stengl<sup>1,2</sup> and Marc A. Vos<sup>1,2</sup>

1. Department of Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands.
2. Department of Medical Physiology, University Medical Center Utrecht, Utrecht University, Netherlands.

**Abstract**

Increased proarrhythmia in dogs with chronic AV block (AVB) has been explained by ventricular remodeling causing a decrease in repolarization reserve. Beat-to-beat variability of repolarization (BVR) has been suggested to reflect repolarization reserve, in which high variability represents diminished reserve and larger propensity for repolarization-dependent ventricular arrhythmia. A subset of chronic AVB dogs (10%) suffers sudden cardiac death (SCD). With the assumption that repolarization defects constitute a potentially lethal proarrhythmic substrate, we hypothesized that BVR in SCD dogs are larger than in matched control chronic AVB dogs.

From a population of 200 chronic AVB dogs, initially two groups were chosen retrospectively: 8 dogs that died suddenly (SCD) and 8 control dogs. Control dogs had a longer lifespan after AVB (10 to 18 weeks) than SCD dogs (5 to 10 weeks). All dogs had undergone electrophysiological testing under anesthesia where ECG, left and right ventricular endocardial monophasic action potentials (MAP) were recorded. BVR was assessed from 30 consecutive beats, illustrated by Poincaré plots and was the only parameter discriminating between SCD and control group. All other electrophysiological parameters (RR, QT and MAP durations) were comparable for the two groups. Extending the number of animals and groups confirmed a larger BVR in the SCD group (SCD:  $5.1 \pm 2.7$ ;  $n = 11$  versus control:  $2.5 \pm 0.4$  ms;  $n = 61$ ;  $P < 0.05$ ) and showed reverse-use dependence of BVR. In comparison, dogs with acute AVB had low variability ( $1.3 \pm 0.3$  ms;  $n = 9$ ;  $P < 0.05$  versus chronic AVB).

Cardiac electrical remodeling after AVB is associated with an increase in beat-to-beat variability of repolarization. Chronic AVB dogs displaying further elevated variability of repolarization are prone to arrhythmia-related SCD.

## Introduction

Lability of repolarization has previously been reported to be increased in patients with ventricular heart disease experiencing sudden cardiac death (SCD).<sup>1</sup> However, more than half of all SCD occurs in people without any history of known cardiac disease, while heart failure is present in only 26% of all SCD cases.<sup>2</sup> Hence, the so-called high-risk patients constitute only a fraction of the total population suffering SCD.<sup>3</sup> This stresses the importance of developing better markers to predict individual arrhythmogenic risk among the general population.

The dog model with chronic complete atrioventricular block (AVB) has been used extensively to investigate mechanisms of ventricular arrhythmia. A high susceptibility for repolarization-dependent proarrhythmia has been established: 10% of the dogs die suddenly under conscious circumstances, while class-III drugs induce arrhythmia in 56-67% of the remaining animals under anesthesia.<sup>4,7</sup> This enhanced susceptibility for repolarization-dependent arrhythmias can be attributed to electrical ventricular remodeling.<sup>8</sup> Previously, beat-to-beat variability of repolarization (BVR) was used to quantify variations in action potential duration from Poincaré plots.<sup>9</sup> A drug-induced increase in BVR from the left ventricular monophasic action potential duration (LV MAPD) was strongly associated with subsequent drug-induced torsades de pointes arrhythmia (TdP). Vice versa, no change in BVR was linked to the absence of ventricular arrhythmia, establishing a high power of BVR in predicting drug-induced TdP.

If SCD is associated with repolarization-dependent arrhythmia, we hypothesize that BVR in SCD dogs is larger than in control dogs with chronic AVB. Furthermore, we hypothesize that BVR is increased alongside ventricular remodeling from acute to chronic AVB. The objective of the present study was to establish the applicability of BVR in the prediction of lethal ventricular remodeling under drug-free circumstances.

## Methods

Over the last ten years, AVB has been performed in a population of more than 200 dogs. In this period 22 dogs with chronic AVB have died suddenly unrelated to the studies performed. Any non-cardiac cause of death was excluded by autopsy.

*General*

Animal experiments took place in accordance with the European Directive for the Protection of Vertebrate Animals Used for Experimental and Other Scientific Purposes (86/609/EU) and with the approval of the Committee for Experiments on Animals of Maastricht and Utrecht University, The Netherlands. All experiments were performed under aseptic conditions in anesthetized mongrel dogs of either sex. Full anesthesia was induced by sodium pentobarbital (20 mg/kg i.v.) and maintained by halothane inhalation (0.5% in O<sub>2</sub>/N<sub>2</sub>O (1:2)). Methodological descriptions of the creation of AVB and electrophysiological studies at chronic AVB have been published earlier.<sup>6,8,10</sup>

Six surface ECG leads and monophasic action potentials from the left and right endocardium were recorded simultaneously during experiments at acute and chronic AVB and stored on hard disc. MAP catheters (MAP, EP Technologies, CA) were placed under fluoroscopic guidance on the free wall or in the apices of the ventricles. MAP signals were amplified with a customized isolated DC-coupled differential amplifier at a frequency range of 0-500 Hz with a 20-mV calibration pulse. The offset of the amplifier was variable and could be adjusted to the recorded signal. The position of the MAP catheter was accepted when the following criteria were met: 1, minimal amplitude from plateau to baseline of 15 mV; 2, smoothness of repolarization and; 3, stability in time.

Telemetry recordings were successfully obtained in 10 dogs with chronic AVB, of which 2 died suddenly. For a description of the telemetric device, implantation and recording procedures, we refer to a previous publication.<sup>5</sup>

*Group composition*

Retrospectively, 8 dogs experiencing SCD during follow-up were selected on the basis of the availability of baseline recordings of >30 minutes. These electrophysiological studies took place at  $5 \pm 2$  weeks after AVB, at which electrical remodeling is complete<sup>10,11</sup> while sudden cardiac death occurred at  $7 \pm 2$  weeks after AVB (range 5 to 10). The control population consisted of 8 matched dogs from the chronic AVB group selected on the basis of similar time points of electrophysiological testing, >30 minutes baseline recording and a follow-up that significantly exceeded that of the SCD dogs ( $13 \pm 3$  weeks, range 10 to 18 weeks; from AV-node ablation to experimental sacrifice).

In a larger comparison, 30-minutes baseline recording were no longer an inclusion criteria (see further). Three groups of AVB dogs were selected: 1, acute AVB with

recordings 10 to 30 minutes after AV-node ablation ( $n = 9$ ); 2, chronic AVB with additionally 53 dogs ( $n = 61$ ); 3, all SCD dogs in which an electrophysiological follow-up study with MAP recordings were performed ( $n = 11$ ).

Additionally, 8 dogs were prospectively included in a serial study analyzing the influence of heart rate on BVR. At acute and chronic AVB, steady state pacing (cycle length (CL) 600 and 1400 ms) was performed from the right ventricular MAP catheter.

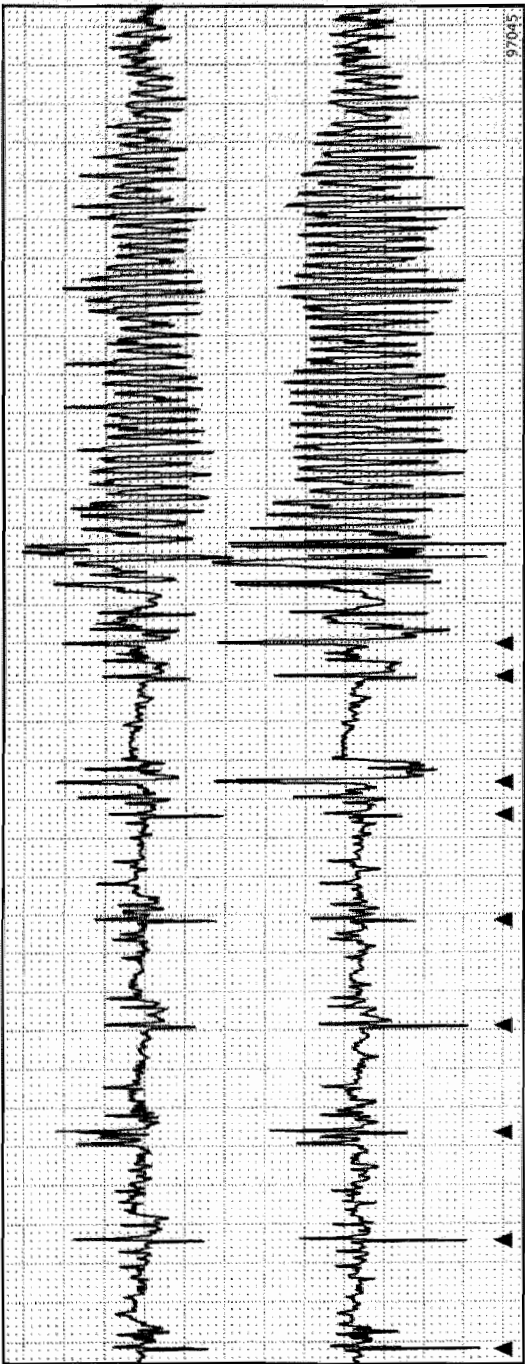
### *Data analysis*

Upon application of a custom-made computer program with an adjustable gain and time scale, the following electrophysiological parameters were measured off line at a resolution of 4 ms: CL of the idioventricular rhythm (RR) and QT interval from lead II and the duration to 100% repolarization of the left and right ventricular MAP (LV and RV MAPD, respectively). The interventricular dispersion of repolarization ( $\Delta\text{MAPD} = \text{LV MAPD} - \text{RV MAPD}$ ) was calculated. Heart-rate corrected QT interval ( $\text{QT}_c$ ) was determined according to Van de Water's formula,<sup>12</sup> which is superior to other rate-correction formulas used in anesthetized bradycardic dogs.

In dogs with 30-minutes recordings, the electrophysiological parameters were measured every 5 minutes and averaged.

Beat-to-beat variability was assessed for each electrophysiological parameter over 30 consecutive beats with a constant ventricular focus. The time periods were randomly chosen and their origins were blinded for the analyzer. The 30 beats were plotted in Poincaré plots,<sup>9,13,14</sup> and short-term variability (STV), defined as the average distance of the points to the diagonal in the Poincaré plot ( $\text{STV} = \sum |D_{n+1} - D_n| / [30 \cdot \sqrt{2}]$ , where  $D$  represents the duration of the electrophysiological parameter) was calculated.<sup>9</sup>

Heart-to-body weight ratios were established upon sacrifice (control chronic AVB group) or autopsy (SCD group) and served as an indicator for hypertrophy and structural remodeling. Of the 61 control dogs, 47 heart-to-body weight ratios were available, while all 11 SCD ratios were obtained. Heart-to-body weight ratios from previous sacrifices of dogs in normally conducted sinus rhythm ( $n = 79$ ) served as representative for the acute AVB group.



**Figure 1**

Telemetry recording showing sudden death in a dog. Under conscious conditions and a stable idioventricular rhythm of 1400 ms, a sudden short-long-short sequence of ventricular systoles initiates a polymorphic ventricular tachyarrhythmia. The arrhythmia degenerates into a lethal ventricular fibrillation. Triangles are aligned with R waves. The noise-to-signal ratios of the telemetry recordings are too large to measure QT intervals. Paper speed: 10 mm/s.

### Statistical analysis

Pooled data are expressed as mean  $\pm$  SD. Comparisons were made using ANOVA followed by a Bonferroni t-test. The area under the curve of receiver-operator characteristics was used to assess the predictive power of variables.  $P < 0.05$  were considered significant.

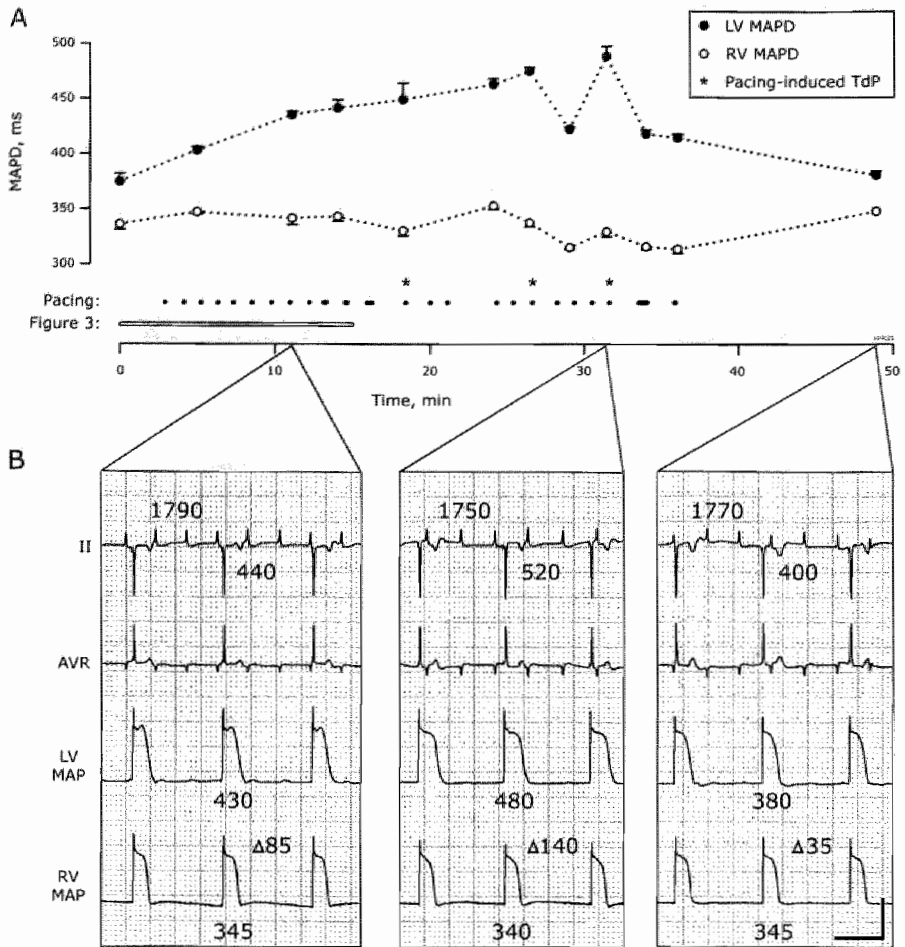
### Results

Figure 1 shows a telemetric recording of the arrhythmia causing death in a dog with chronic AVB. A short-long-short sequence of the RR intervals precedes a polymorphic ventricular tachycardia deteriorating into lethal ventricular fibrillation.

#### *Beat-to-beat variability of repolarization*

The example in Figure 2A illustrates the oscillatory behavior of the LV MAPD in an anesthetized chronic AVB dog that later died suddenly and unexpectedly under conscious circumstances. At a rather stable idioventricular escape rhythm recorded for 50 minutes (1750 - 1850 ms), the LV MAPD changed considerably between 375 and 490 ms. The RV MAPD show lesser degree of fluctuation giving rise to periods with interventricular dispersion exceeding 100 ms. At three time points, the surface ECG and MAP are depicted in Figure 2B. While the ventricular origin of activation remains constant, large changes in the QT interval and LV MAPD are appreciable, associated with slight alterations in T-wave morphology. In Figure 3, 15 minutes of beat-to-beat analysis of the LV MAPD is illustrated from the dog of Figure 2 and compared to a representative control dog with chronic AVB. Large oscillations of LV MAPD seem to be present throughout the whole period in the SCD dog, whereas the LV MAPD of the control dog in a similar time frame showed minimal oscillations. When the 30-minutes temporally averaged electrophysiological parameters (RR, QT, QT<sub>c</sub> and LV-, RV- or  $\Delta$ MAPD) were compared between SCD dogs and the matched dogs with chronic AVB, no differences were observed (Table 1). Also, when the electrophysiological parameters were compared as the mean from 5 consecutive beats at a single time point, being either the start or the end of the observation period, no differences between the two groups were seen (not shown). Only when the maximal electrophysiological values during the observational period were compared, interventricular dispersion was significantly larger in the SCD dogs:  $111 \pm 48$  versus control:  $66 \pm 23$  ms,  $P < 0.05$ .





**Figure 2**

**A:** Left- and right ventricular MAPD displayed at random time points during 50 minutes in an anesthetized dog with chronic AVB, which died 24 days later. Large temporal oscillations of the LV MAPD induce periods of accentuated interventricular dispersion of repolarization. Maximal differences over the 50-minutes observation period were 115, 40 and 125 ms for LV, RV and  $\Delta$ MAPD, respectively. Pacing from the RV MAP catheter to address proarrhythmia and contractile potentiation is indicated along the time axis. Asterisks indicate pacing-induced TdP.

**B:** Three representative tracings of ECG and MAP during the time course in A. In periods between pacing, activation of the ventricles had the same focus, while the repolarization had minor shifts based on changing T-wave morphology. RR and QT intervals are noted above and below lead II, respectively, while MAPD is visualized under each signal.  $\Delta$ : interventricular dispersion. ECG calibrated to 1 mV/cm. Scale bar: 1 second, horizontally versus 20 mV on the MAP, vertically.

**Table 1.** Temporally averaged electrophysiological parameters and short-term variability thereof in dogs suffering SCD (n = 8) and in control dogs with chronic AVB (n = 8).

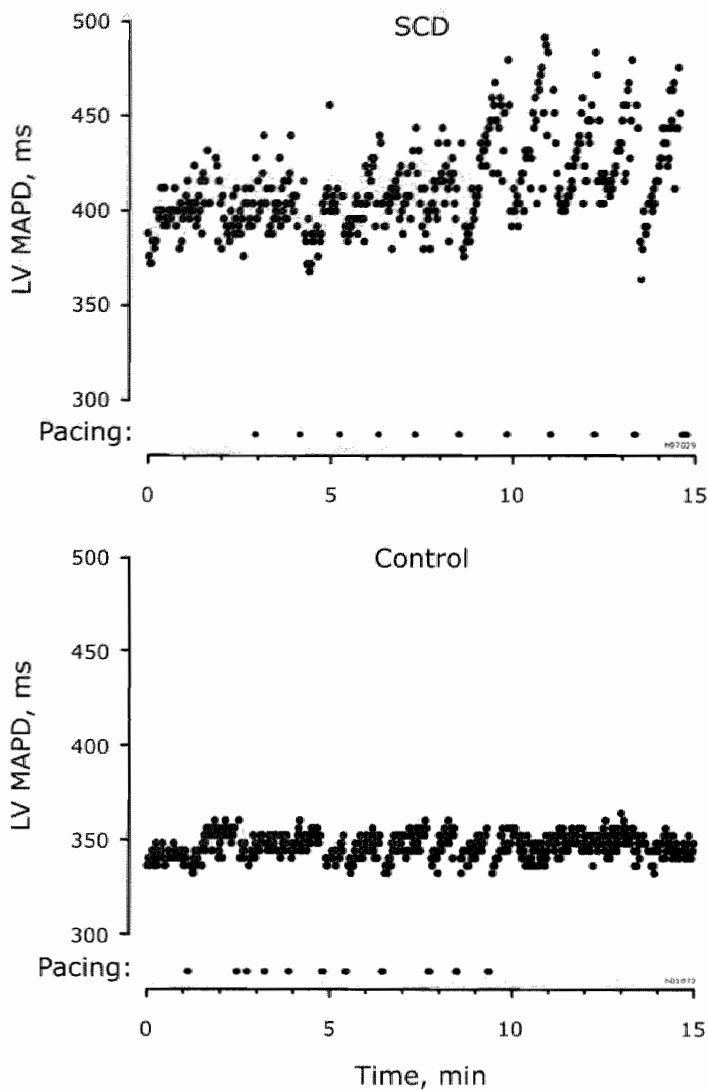
	Electrophysiological parameters		Short-term variability	
	SCD	Control	SCD	Control
RR	1599 ± 293	1534 ± 426	18.0 ± 29.0	11.8 ± 12.7
QT	438 ± 77	403 ± 32	6.3 ± 3.2	4.6 ± 1.7
QT <sub>c</sub>	403 ± 85	356 ± 39	6.9 ± 3.4	5.0 ± 2.1
LV MAPD	407 ± 71	373 ± 18	5.1 ± 2.7	2.5 ± 0.4 *
RV MAPD	339 ± 46	325 ± 29	3.0 ± 1.7	2.9 ± 0.8
ΔMAPD	69 ± 36	49 ± 17	5.8 ± 2.6	4.1 ± 0.8

All measurements in ms. \*,  $P < 0.05$  versus SCD.

Recently we have introduced methods to quantify beat-to-beat variability of repolarization.<sup>9</sup> In Figure 4A, LV MAPD from 30 beats are compared for SCD dogs and control dogs. Although there are large interindividual differences in the mean LV MAPD, the beat-to-beat variability seems to be augmented in the SCD group. By plotting Poincaré plots of the 30 beats (Figure 4B), STV as a measure of the width of the plot quantifies the variability. The STV of all electrophysiological parameters are summarized in Table 1 where only STV of the LV MAPD is significantly higher in the SCD group.

### *Time frame*

Beat-to-beat variability of LV MAPD in the SCD dog in Figure 3 seems to be present over the whole period independent of whether pacing protocols are performed. To further validate STV measurements of 30 beats, we continuously calculated STV over 15 minutes revealing a minimum STV of 5.9 ms (at 5 minutes) in the SCD dog compared with a maximum STV of 4.4 ms (at 6 minutes) in the control dog. Shortening the period over which STV is calculated from 30 to 10 beats results in an STV in the SCD dog that is lower than the maximal STV of the control dog 27% of the time. From 24-beat analysis and longer, STV of the SCD dog is higher than the maximal STV of the control dog constantly during the 15 minutes, supporting our choice of 30 beats.



**Figure 3**  
LV MAPD of every spontaneous beat during 15 minutes in the SCD dog of Figure 2 (upper panel) and a control dog (lower panel). Again, pacing trains are indicated along the time axes. Beat-to-beat variability of repolarization seems to be larger in the SCD dog.

*Short-term variability and cardiac remodeling*

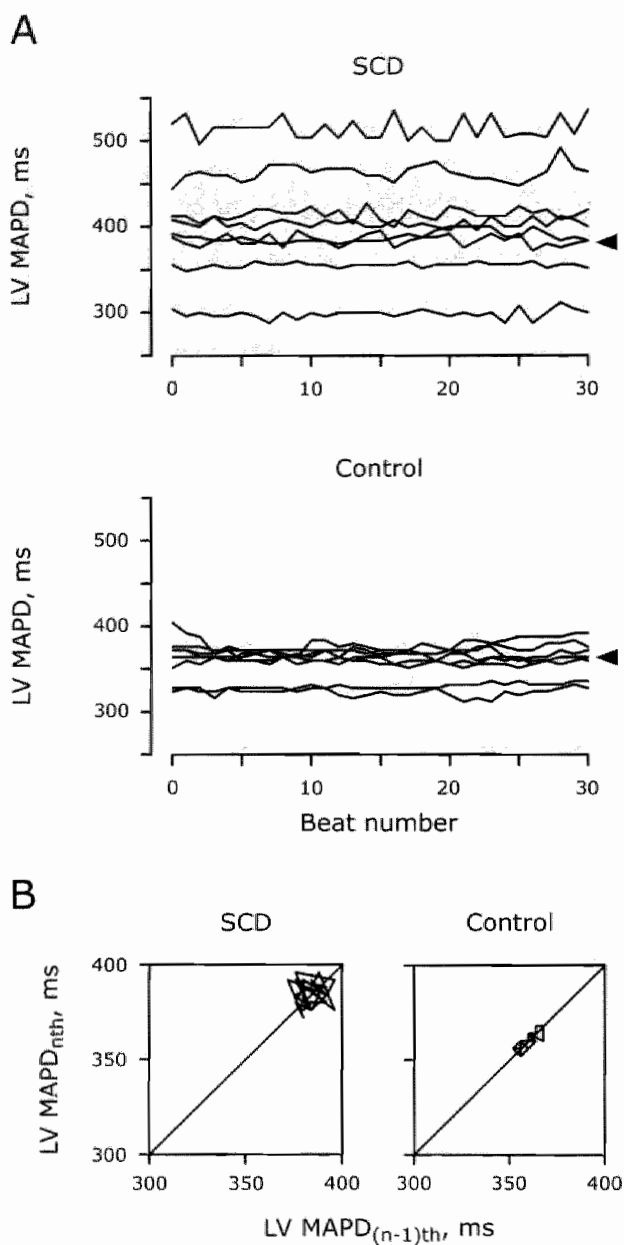
Since availability of 30 minutes is not a prerequisite for analysis of variability we included additional dogs to quantify STV between groups of larger sizes. In Figure 5 it is shown that STV of the LV MAPD increases from  $1.3 \pm 0.3$  ms at acute AVB to  $2.7 \pm 0.9$  at chronic AVB ( $P < 0.001$ ), while the SCD group still has the highest STV ( $5.4 \pm 1.4$  ms;  $P < 0.001$  versus chronic AVB). LV MAPD in these larger groups is not significantly different from the smaller groups in Table 1 (chronic AVB:  $359 \pm 54$ ,  $n = 61$ ; SCD:  $412 \pm 70$  ms,  $n = 11$ ;  $P = \text{NS}$  for both).

The heart-to-body weight ratio was significantly higher in remodeled hearts (chronic AVB:  $11.1 \pm 1.8$  versus acute AVB:  $8.5 \pm 1.1$  g/kg;  $P < 0.01$ ). The heart-to-body weight ratios of the SCD group were comparable to the other chronic AVB dogs ( $12.1 \pm 2.1$  g/kg;  $P = \text{NS}$ ).

Receiver-operator characteristics were used to compare how strongly the parameters would predict SCD among dogs with chronic AVB. With an area under the curve of 0.97, STV was superior to the heart-to-body weight ratio (0.72), LV MAPD (0.71) and RR (0.69) in predicting SCD.

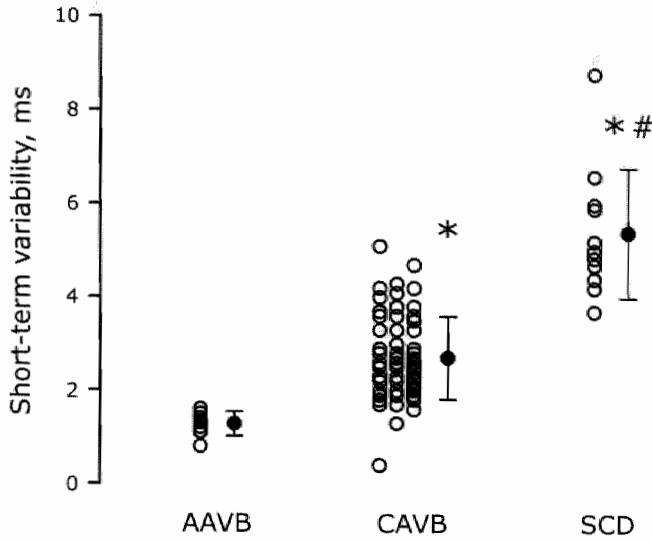
*Frequency dependency of short-term variability*

We performed a prospective serial investigation to evaluate the association between STV at acute and chronic AVB at two different paced CL (Figure 6). There is no rate dependency of STV in the non-remodeled acute AVB dogs. In the remodeled chronic AVB dogs, STV is only elevated at CL approaching the idioventricular rhythm (1400 ms), while there is no difference in STV between acute and chronic AVB at CL comparable to sinus rhythm (600 ms). Changing from an idioventricular rhythm with inherent heart-rate variability to a paced rhythm of fixed CL does not change STV (Figure 6).

**Figure 4**

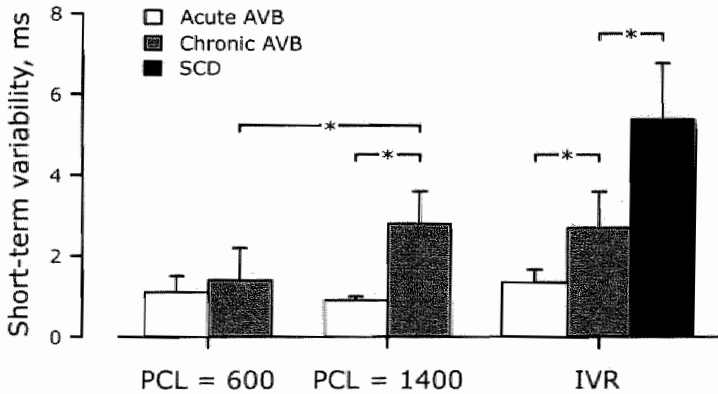
**A:** Individual LV MAPD of 30 consecutive spontaneous beats in the 8 SCD dogs (above) and the 8 control dogs (below).

**B:** The LV MAPD of every beat is plotted against the LV MAPD of the former beat in one Poincaré plot per dog (tracings indicated by arrowheads in A). A larger width of the Poincaré plot can be appreciated in the SCD dog, whereas the mean LV MAPD for the two groups was not different (Table 1).



**Figure 5**

Short-term variability in three phenotypes of dogs at acute AV block (AAVB,  $n = 9$ ), at chronic AVB (CAVB,  $n = 61$ ) and in the SCD group ( $n = 11$ ). \*,  $P < 0.0001$  versus acute AVB; #,  $P < 10^{-11}$  versus chronic AVB.



**Figure 6**

STV of the LV MAPD at paced CL of 600 and 1400 ms in dogs with acute and chronic AVB. For comparison, STV measured under idioventricular rate is provided for acute and chronic AVB dogs and for the SCD group (individual data in Figure 5). \*,  $P < 0.05$ .

## Discussion

In the present study, we show that dogs with remodeled hearts due to chronic AVB have larger BVR than control dogs with normal hearts. Furthermore, BVR is reverse-use dependent in chronic AVB dogs. Finally, dogs with remodeled hearts that die suddenly have larger BVR than surviving chronic AVB dogs.

### *Cardiac remodeling and reduced repolarization reserve*

After AVB, several ventricular remodeling processes occur. Using our historical database, we confirm cardiac hypertrophy at the organ level based on an increased heart-to-body weight ratio.<sup>8,10</sup> On the surface ECG, the QT interval is prolonged and the T-wave morphology changed.<sup>15</sup> Locally, the endocardially-recorded ventricular MAPs are inhomogeneously prolonged, augmenting interventricular dispersion of repolarization. Cellular action-potential prolongation can partly be explained by the downregulation of the delayed rectifier potassium currents and by upregulation of the sodium-calcium exchange current.<sup>15-17</sup> The compensated hemodynamic state is achieved by contractile adaptations in both ventricles.<sup>8</sup> Enhanced sarcoplasmic reticulum calcium release improves contraction, especially at slow rates.<sup>17</sup> These ventricular adaptation processes contribute to an enhanced susceptibility to repolarization-dependent arrhythmia, seen as afterdepolarizations in vitro<sup>18</sup> and afterdepolarization-dependent triggering of arrhythmia in vivo<sup>17,19</sup> In response to infusion of drugs with  $I_{Kr}$ -blocking characteristics, there is a higher propensity of TdP in the dogs with chronic AVB.<sup>6,7</sup> Whereas no drug-induced TdP is seen in dogs with acute AVB, the chronic AVB dogs has a 56-67% risk of TdP after the same drugs.<sup>4,6,7,20</sup> Based on these findings, we believe that compared with acute AVB, at chronic AVB the dogs have a diminished repolarization reserve,<sup>21</sup> by which they are unable to withstand a challenge on repolarization and thereby more vulnerable to TdP.

The 22 dogs that died suddenly constitute a population of the chronic AVB dogs that experience arrhythmias under anesthesia as well as under conscious circumstances (Figures 1, 2 and reference <sup>5</sup>). This is a unique characteristic, since induction of arrhythmia in the majority of the chronic AVB population requires additional hits, e.g. by administration of  $I_{Kr}$  blockers, anesthesia and/or pacing.<sup>4</sup> Earlier studies by our group showed that maximal LV MAPD and interventricular dispersion of repolarization during baselines of variable lengths were significantly larger in SCD dogs than in 78 control dogs with chronic AVB. A number of the SCD dogs were observed to experience syncope followed by death in association with a suspected

increase in adrenergic tone.<sup>5</sup> One possible explanation for the vulnerable substrate is that the reported downregulation of  $I_{Ks}$  induces a loss of repolarisation shortening after  $\beta$ -adrenergic stimulation, which would be most dangerous at fast heart rates or during sudden rate changes.<sup>14,15</sup>

#### *Beat-to-beat variability of repolarization*

From Figure 3 it is appreciable that the variability of repolarization in SCD dogs is not a slow undulating phenomenon, but that it configures as a scatter of large instantaneous changes. Hence, extensive baseline recordings may not be required for an assessment of variability. Earlier quantification of beat-to-beat variability of repolarization was restricted to 30 consecutive beats, which showed to be valuable in predicting the occurrence of drug-induced TdP in anesthetized dogs with chronic AVB.<sup>9</sup> Our preferred quantification of beat-to-beat variability of repolarization is short-term variability (STV). In this analysis, the direct differences in duration of two consecutive beats are averaged over a 30-beat period. In the example of Figure 3, we measured every beat in a 15-minute time frame. It is shown that the STV of an SCD dog is at all times were higher than the maximal STV of a control dog. Thus, in this setting, the analysis of a single epoch of 30 beats gathers enough information to identify the vulnerable animal.

Only the STV of the LV MAPD showed significant differences between SCD dogs and control dogs, whereas the electrophysiological parameters, including RR and QT intervals from the surface ECG, the right ventricular MAPD and the interventricular difference in MAPD did not differ (Table 1). Furthermore, in the statistical analysis of predictive power, STV of the LV MAPD was superior to both temporally averaged LV MAPD and RR intervals. Table 1 also shows, that only the STV of LV MAPD is increased in the SCD population while the STV of other repolarization parameters does not contain similar information. The global nature of the QT interval versus the local recoding of an MAP signal suggests that BVR is a regional phenomenon, giving rise to the hypothesis that local discordant differences in repolarization duration render the tissue susceptible to arrhythmias by the infringement of focally triggered extrasystoles.<sup>20,22</sup> The RV MAPD did not show an increased STV in the SCD population, suggesting a stronger repolarization reserve in the right ventricle, which indeed fits with previous cellular findings of larger repolarizing currents in the right than in the left ventricle.<sup>23-25</sup>

It is tempting to speculate that the genetic nature of individual animals determines whether a dog develops the lethal SCD phenotype or a stable one upon induction of AVB. In the SCD population, instances of increased adrenergic drive during specific



conditions (e.g. feeding or excitement) may profoundly exaggerate BVR leading to arrhythmic death.

*Influence of heart rate on beat-to-beat variability of repolarization*

In the non-remodeled heart, STV appears to be heart-rate independent (Figure 6). A long CL facilitates STV in dogs with chronic AVB, whereas faster pacing decreases STV. The STV at 1400 ms paced CL is comparable to the STV during idioventricular rate, suggesting that the limited heart-rate variability at spontaneous ventricular rhythm does not influence STV. A decrease in STV as heart rate increases argues against proarrhythmia at increased adrenergic drive as the cause of SCD. However, it is possible that the relationship between STV and CL is altered by anesthesia. Furthermore, there is likely to be direct influences of increased adrenergic drive on STV that are not mimicked by ventricular pacing.

*Novel parameters associated with sudden cardiac death*

In the clinic, T-wave alternans and heart-rate variability are promising parameters for identifying the individual at risk.<sup>26-30</sup> A potential new proarrhythmic marker is the QT variability index (QTVI), a non-invasive parameter that normalizes the QT variance for the heart-rate variance over a 5-minute period.<sup>31</sup> Specifically, patients with a history of SCD have a significantly higher QTVI than patients with heart disease without SCD.<sup>1</sup>

Drug-induced repolarization-dependent arrhythmias have previously been associated with early markers like prolongation and instability of the MAPD in the isolated rabbit heart.<sup>13</sup> Recently, other parameters like transmural dispersion of repolarization in ventricular wedge preparations have been very useful for understanding the role of repolarization gradients in proarrhythmia.<sup>32</sup>

In the Western population, reported overall incidences lie between 0.1 and 0.2%. Still, too often SCD is the first manifestation of cardiovascular disease.<sup>33</sup> These aspects strongly support further investigations of these predictive techniques. The present study shows that BVR is increased in dogs that experience SCD, which calls for clinical studies to determine whether elevated BVR could herald SCD in humans too.

### *Study limitations*

In this study, variability of repolarization was limited to invasive, endocardial recordings in anesthetized dogs with remodeled hearts. All experiments were performed under anesthesia, which has profound effects on electrophysiological parameters,<sup>34,35</sup> however the anesthetic treatment was identical in all experiments. Not all sudden deaths were witnessed or recorded through telemetric devices, so we are not able to generalize upon the mode of death. Still, we consider repolarization-dependent arrhythmias as the most probable cause of death. This study established an association between increased BVR and SCD, whereas a prospective design is needed to elucidate possible common denominators.

### *Conclusions*

Electrical ventricular remodeling after AVB is associated with an increase in short-term variability of repolarization, which is reverse-use dependent at chronic AVB. Chronic AVB dogs that suffer SCD have an even higher STV, suggesting that BVR could be a potential additional parameter in the identification of the patient at risk for sudden cardiac death.

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# Beat-to-Beat Variability of Repolarization Determines Proarrhythmic Outcome in Dogs Susceptible to Drug-Induced Torsades de Pointes

Morten B. Thomsen<sup>1,2</sup>, Paul G.A. Volders<sup>2</sup>, Jet D.M. Beekman<sup>1</sup>, Jørgen Matz<sup>3</sup> and Marc A. Vos<sup>2</sup>

1. Department of Medical Physiology, Heart Lung Center Utrecht, University Medical Center Utrecht, Utrecht, Netherlands.
2. Department of Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University, Maastricht, Netherlands.
3. Center of Excellence, Cardiovascular Research, H. Lundbeck, Copenhagen, Denmark.

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## Abstract

Recent results in dogs show that increased beat-to-beat variability of repolarization (BVR) predicts drug-induced torsades de pointes (TdP) more accurately than conventional measures of repolarization prolongation. We investigated whether increasing or decreasing BVR would change proarrhythmic outcome accordingly. The non-cardiovascular,  $I_{K_r}$ -blocking drug sertindole (1.0 mg/kg i.v.) induced TdP in 10 of 13 anesthetized dogs with chronic AV block. At a lower dose (0.2 mg/kg i.v.) no TdP was induced, despite similar increases in QT intervals (1.0 mg/kg:  $400 \pm 60$  to  $495 \pm 65$  ms,  $P < 0.05$  (\*); 0.2 mg/kg:  $400 \pm 60$  to  $475 \pm 85$  ms\*). BVR, quantified as short-term variability (STV) from Poincaré plots ( $STV = \sum |D_n - D_{n+1}| / [30 \cdot \sqrt{2}]$ ,  $D$  = left ventricular monophasic action potential duration (LV MAPD)), was the only parameter that was associated with TdP outcome (1.0 mg/kg:  $2.3 \pm 1$  to  $5.1 \pm 2$ \*; 0.2 mg/kg:  $2.3 \pm 1$  to  $3.2 \pm 1$ ,  $P = NS$ ). Three interventions were used to prevent sertindole-induced TdP. None of these altered the sertindole-induced prolonged QT interval, LV MAPD or interventricular dispersion of MAPD. (1) KCl infused i.v. elevated plasma potassium from  $2.8 \pm 0.3$  to  $4.6 \pm 0.9$  mM\* and reduced the incidence of sertindole-induced TdP from 6 of 7 to 1 of 7 dogs\*. During KCl treatment sertindole-related increase of STV was much lower:  $3.0 \pm 1$  versus  $4.5 \pm 1$  ms\*. (2) Levromakalim ( $I_{K_{ATP}}$  activator, 3  $\mu$ g/kg i.v.) reduced sertindole-induced TdP and decreased STV from  $4.9 \pm 2$  to  $2.6 \pm 1$  ms\*. (3) Steady-state ventricular pacing (60 bpm) momentarily abolished sertindole-induced TdP and decreased STV from  $4.9 \pm 2$  to  $3.2 \pm 1$  ms\*. TdP reappeared upon return to ventricular rhythm. Manipulation of BVR is feasible in the intact dog heart. The magnitude of BVR determines proarrhythmic outcome. BVR proves to be a superior marker for the prediction and prevention of drug-induced TdP.

## Introduction

Drug-induced torsades de pointes arrhythmia (TdP) is an unwanted adverse effect, which by definition is associated with prolonged ventricular repolarization. However, it has been demonstrated that QT prolongation does not have to be proarrhythmic.<sup>1-6</sup> TdP incidences by non-cardiovascular QT-prolonging drugs is very low relative to the number of treated patients.<sup>7</sup> In these few affected patients, it is hypothesized that the drug is the final hit in an already vulnerable heart. This predisposition is thought to be the result of an insufficient repolarization reserve, which can be inherited, acquired or both.<sup>8,9</sup> Identifying the patient at risk and preventing arrhythmia by enhancing his or her repolarization reserve are long-sought medical aspirations. Classical electrophysiological parameters, such as the duration of the QT interval, seem to be of limited value in quantifying repolarization reserve. Recently, beat-to-beat variability of repolarization (BVR) has been introduced as an alternative.<sup>2</sup>

In anesthetized dogs with chronic AV block (CAVB) predisposed for drug-induced TdP,<sup>1,10-12</sup> baseline BVR is increased during electrical remodeling.<sup>13</sup> The highest BVR values were obtained in CAVB dogs that later suffered sudden cardiac death.<sup>13</sup> Furthermore, we showed that a dose-dependent increase in BVR was predicting proarrhythmic outcome after *d*-sotalol administration.<sup>2</sup> Chronic amiodarone administration, a drug considered free of proarrhythmia in patients, did not increase BVR or induce TdP in CAVB dogs.<sup>2,6,14</sup> Similarly, we observed an unchanged BVR and concurrent absence of TdP after increasing the infusion time of NS-7, a drug in development for anti-stroke therapy.<sup>15</sup>

Thus, we believe that BVR, quantified as short-term variability (STV), could be an alternative parameter to detect decreased repolarization reserve. In the present study, we investigated whether increasing or decreasing BVR would change proarrhythmic outcome accordingly. For this purpose, we examined the dose-dependent induction of TdP after administration of the antipsychotic drug sertindole<sup>1</sup> linking this to differential changes of STV. We employed three interventions with the aim of enhancing repolarization reserve to control BVR and prevent or suppress sertindole-induced TdP. During all of these interventions, we examined the value of STV versus other repolarization-prolongation parameters.



## Methods

### *General*

Animal handling was in accordance with the European Directive for the Protection of Vertebrate Animals Used for Experimental and Other Scientific Purposes (86/609/EU). The Committee for Experiments on Animals of Utrecht University approved all experiments. In a preliminary experiment, AV block was induced in 11 dogs (Marshall, NY) by radiofrequency ablation according to methods previously described.<sup>11</sup> Experiments reported here were performed >4 weeks after ablation allowing cardiac remodeling to complete.<sup>11</sup> Three animals died unexpectedly before experiments could be performed. Complete anesthesia was induced by sodium pentobarbital (20 mg/kg i.v.) and maintained by halothane (0.5% in O<sub>2</sub> and N<sub>2</sub>O, 1:2). Besides surface ECG, monophasic action potentials (MAP) placed endocardially on the free walls of the left (LV) and right ventricle (RV), were recorded. Perioperative care, signal processing and data recording have been described in detail previously.<sup>12</sup> All drugs were administered intravenously. Plasma-potassium levels were measured from samples taken from a contra-lateral vein (ABL, Radiometer, Denmark).

### *Dose-dependent induction of TdP*

Five dogs received serially 0.2 and 1.0 mg/kg sertindole in a random-crossover design with two weeks between experiments. Additional 3 dogs received only 1.0 mg/kg. The data set was extended by adding experiments from 9 additional dogs ( $n_{0.2} = 4$ ;  $n_{1.0} = 5$ ) participating in a previously reported sertindole study.<sup>1</sup> Sertindole (purchased from H. Lundbeck, Denmark) was administered over 5 minutes i.v.

### *Prevention of TdP by elevating plasma-potassium concentrations*

Seven dogs received 1.0 mg/kg sertindole with and without potassium-pretreatment in a random-crossover design. 30 to 60 mmol KCl was infused over 2 hours, where after 1.0 mg/kg sertindole was administered as the proarrhythmic challenge. Potassium levels and ECG were monitored every 10 minutes.

*Suppression of drug-induced TdP by levromakalim-induced activation of  $I_{K,ATP}$*

In 7 experiments after sertindole-induced TdP, the  $I_{K,ATP}$  opener levromakalim (3 and 10  $\mu\text{g/kg/3-minutes}$ , i.v.) was administered with a 10-minute interval. Measurements were done 5 to 10 minutes after the start of levromakalim administration. Because the higher dose of levromakalim is antiarrhythmic and shortens repolarization parameters, we also selected the lower dose to possibly dissociate the effects on increased BVR and prolonged repolarization.

*Preventing reappearance of TdP by right ventricular pacing*

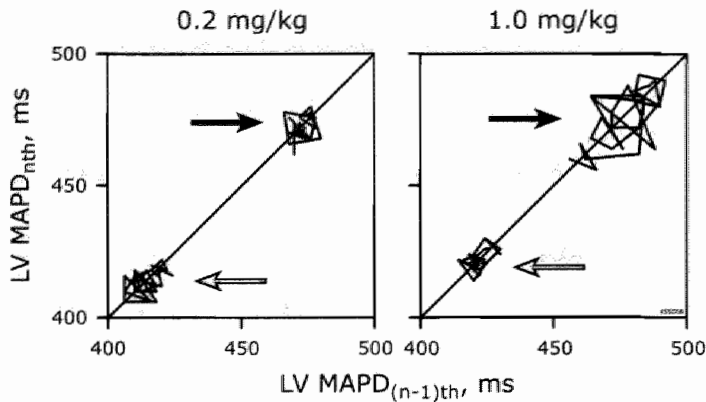
Six dogs were paced from the RV MAP catheter (60 bpm) directly after the reproducible occurrence of sertindole-induced TdP was noted. In this way, the antiarrhythmic effects of controlled heart rate on BVR were evaluated. Pacing intervention was considered successful when no extrasystoles or TdP had occurred for 2 minutes.

*Analysis*

Mean RR and QT intervals from lead II were measured manually (ECGview, Maastricht University). Durations of the MAP to 90% repolarization (MAPD) were determined semi-automatically (ECG-Auto, EMKA Technologies, France). Interventricular dispersion ( $\Delta\text{MAPD}$ ) was defined as LV minus RV MAPD. Measurements were performed during periods without extrasystolic activity as previously described.<sup>2</sup> BVR was assessed from 30 consecutive beats and quantified as short-term variability (STV) describing the mean orthogonal distance to the line-of-identity on a Poincaré plot, as described earlier<sup>2</sup> (Figure 1,  $\text{STV} = \sum |D_{n+1} - D_n| / [30 \cdot \sqrt{2}]$ , where D represents LV MAPD). Dogs were considered inducible when 3 or more TdP consisting of  $>5$  beats were observed.

*Statistical analysis*

Pooled data are expressed as mean  $\pm$  SD. Comparisons were performed with 2-way ANOVA or 1-way repeated measures ANOVA followed by paired Bonferroni comparisons. TdP incidences were compared with a Chi-square test. Statistical difference was acknowledged at  $P < 0.05$ .



**Figure 1**

Poincaré plots obtained from a dog under the influence of low (0.2 mg/kg, left) or high dose (1.0 mg/kg, right) sertindole. At control (open arrows), comparable low BVR (2.3 and 2.5 ms, respectively) and LV MAPD are present. After administration of sertindole (closed arrows), the mean LV MAPD prolongs to similar levels, while STV is only increased after the proarrhythmic high dose (2.6 and 5.2 ms, respectively).

Table 1. Sertindole-induced changes in electrophysiological parameters and TdP.				
	Control 1	0.2 mg/kg	Control 2	1.0 mg/kg
RR, ms	1384 ± 349	1407 ± 318	1427 ± 228	1503 ± 268
QT, ms	400 ± 60	474 ± 85*	398 ± 60	496 ± 65*
QT <sub>c</sub> , ms	367 ± 54	439 ± 78*	361 ± 54	452 ± 63*
LV MAPD, ms	353 ± 51	416 ± 66*	336 ± 48	427 ± 66*
RV MAPD, ms	307 ± 37	354 ± 48*	308 ± 43	370 ± 61*
ΔMAPD, ms	46 ± 36	62 ± 27	27 ± 20	57 ± 45
STV, ms	2.3 ± 0.8	3.2 ± 1.1	2.3 ± 0.7	5.1 ± 2.1*†
TdP	-	0 of 9	-	10 of 13†

There are no differences in values before the two experiments. TdP quantified as the number of inducible dogs relative to group size. \*,  $P < 0.05$  versus baseline; †,  $P < 0.05$  versus 0.2 mg/kg sertindole.

**Results**

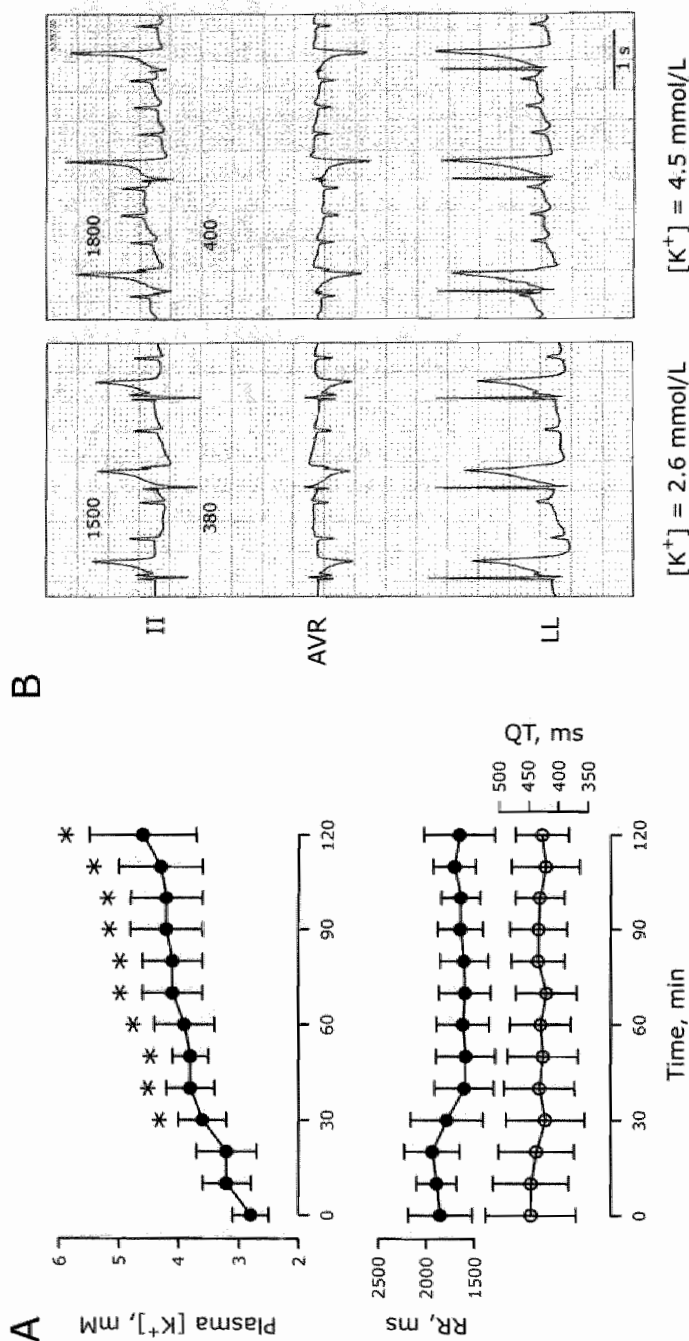
*Dose-dependent induction of TdP*

All electrophysiological parameters were similar at the start of the dose-dependent sertindole experiments. No difference was seen between the serial ( $n=5$ ) and the group comparison (Table 1). No dogs were inducible after the low dose while 10

of 13 dogs showed TdP after 1.0 mg/kg sertindole ( $P < 0.05$ ; Table 1). QT interval, LV and RV MAPD were all significantly increased to comparable levels after the two doses of sertindole (Table 1). There was an increase in STV after 1.0 mg/kg sertindole ( $2.3 \pm 0.7$  to  $5.1 \pm 2.1$  ms,  $P < 0.001$ ), while 0.2 mg/kg sertindole did not change STV ( $2.3 \pm 0.8$  to  $3.2 \pm 1.1$ ,  $P = \text{NS}$ ; Table 1, Figure 1). Furthermore, the STV reached after 1.0 mg/kg sertindole was significantly higher than the STV induced by 0.2 mg/kg sertindole ( $P < 0.05$ ).

#### *Prevention of TdP by elevating plasma-potassium concentration*

Infusion of KCl increased plasma potassium from  $2.8 \pm 0.3$  mmol/L to  $4.6 \pm 0.9$  mmol/L ( $P < 0.05$ ; Figure 2). This did not lead to any changes in the ventricular electrophysiological parameters (Figure 2; QRS width changed from  $81 \pm 16$  to  $88 \pm 15$  ms,  $P = \text{NS}$ ). In the serial comparison, baseline STV was not altered by elevated potassium levels (Figure 3). Potassium pretreatment, however, reduced the sertindole-induced TdP incidence from 6 of 7 to 1 of 7 ( $P < 0.05$ ; Figure 3), which was not associated by differential changes in RR ( $1557 \pm 337$  versus  $1816 \pm 615$  ms; no potassium versus potassium pretreatment, respectively), QT ( $488 \pm 64$  versus  $528 \pm 79$  ms), LV MAPD ( $408 \pm 65$  versus  $432 \pm 72$  ms), RV MAPD ( $372 \pm 71$  versus  $367 \pm 51$  ms) or  $\Delta\text{MAPD}$  ( $37 \pm 43$  versus  $65 \pm 44$  ms,  $P = \text{NS}$  for all). Sertindole increased STV in control experiments ( $2.0 \pm 0.7$  to  $4.5 \pm 1.2$  ms,  $P < 0.001$ ) but not in potassium experiments ( $2.2 \pm 0.7$  to  $3.0 \pm 1.1$  ms,  $P = \text{NS}$ ; Figure 3). Furthermore, the sertindole-induced STV was significantly higher in control experiments when compared to potassium experiments ( $P < 0.05$ ; Figure 3).

**Figure 2**

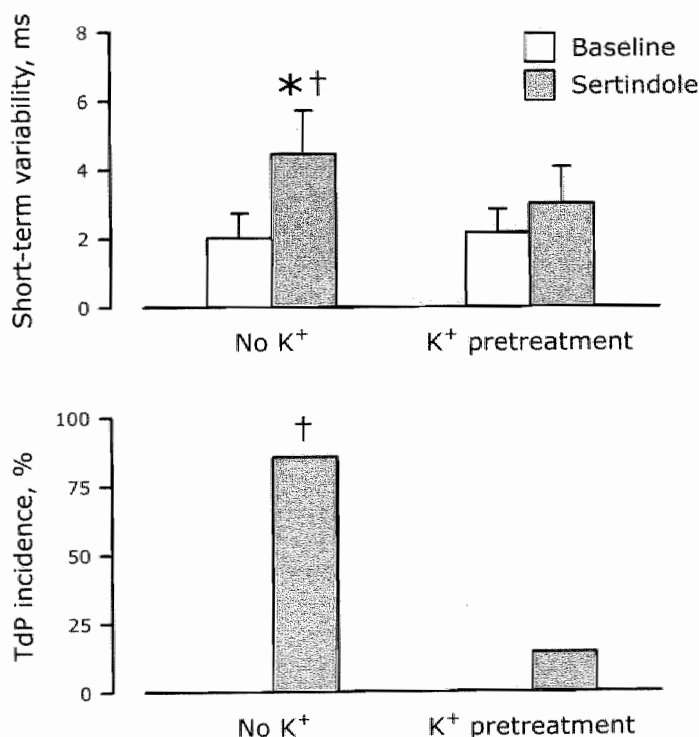
**A:** Time-dependent changes in plasma concentrations of potassium (upper panel), RR and QT intervals (lower panel) during 2 hours KCl infusion ( $n = 7$ ).

Plasma potassium was significantly increased from 30 minutes and forward, while no changes were observed in the RR or QT intervals. \*,  $P < 0.05$  versus baseline.

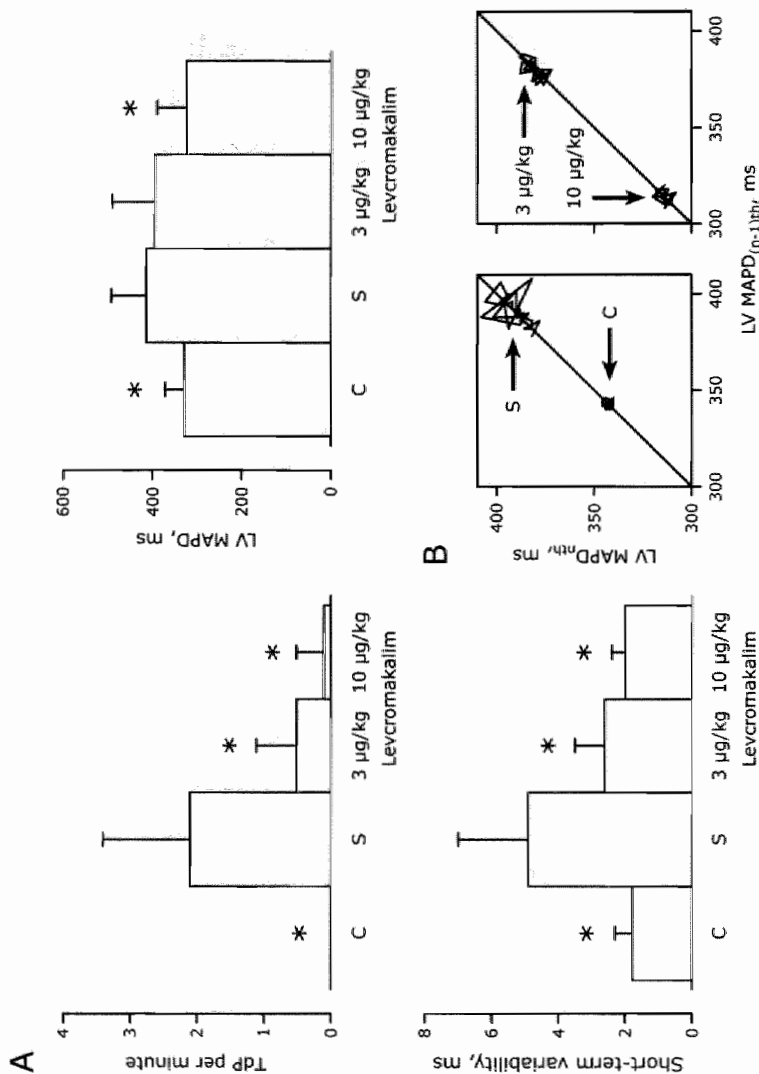
**B:** Representative example of the ECG before and after elevation of plasma potassium. RR and QT intervals are noted above and below lead II. LL refers to a precordial lead placed in the 6th intercostal space on the left lateral side of the thorax. The QRS interval is 60 ms at both time points.

*Suppression of drug-induced TdP by levcromakalim-induced activation of  $I_{K,ATP}$* 

Both 3  $\mu\text{g/kg}$  and additionally 10  $\mu\text{g/kg}$  levcromakalim were effective in preventing further arrhythmia, reducing the sertindole-induced TdP frequency from  $2.1 \pm 1.3$  TdP per minute to  $0.5 \pm 0.6$  ( $P < 0.05$ ; Figure 4) and to  $0.1 \pm 0.4$  TdP per minute ( $P < 0.001$ ; Figure 4), consecutively. While leaving the heart rate unchanged (RR:  $1487 \pm 333$  to  $1277 \pm 190$  ms,  $P = \text{NS}$ ), the high dose abbreviated the sertindole-prolonged QT interval ( $502 \pm 74$  to  $404 \pm 55$  ms,  $P < 0.05$ ), LV MAPD (Figure 4), RV MAPD ( $373 \pm 54$  to  $305 \pm 46$  ms,  $P < 0.05$ ) and decreased STV (Figure 4). The lower dose had no statistical significant effect on heart rate (RR,  $1399 \pm 362$  ms), QT interval ( $496 \pm 74$  ms), LV MAPD (Figure 4) or RV MAPD ( $359 \pm 50$  ms,  $P = \text{NS}$  for all).  $\Delta\text{MAPD}$  was not significantly changed by either dose of levcromakalim. Only STV was decreased by the lower dose ( $4.9 \pm 2.1$  to  $2.6 \pm 0.9$  ms,  $P < 0.05$ ; Figure 4) along with the reduction in proarrhythmia.

**Figure 3**

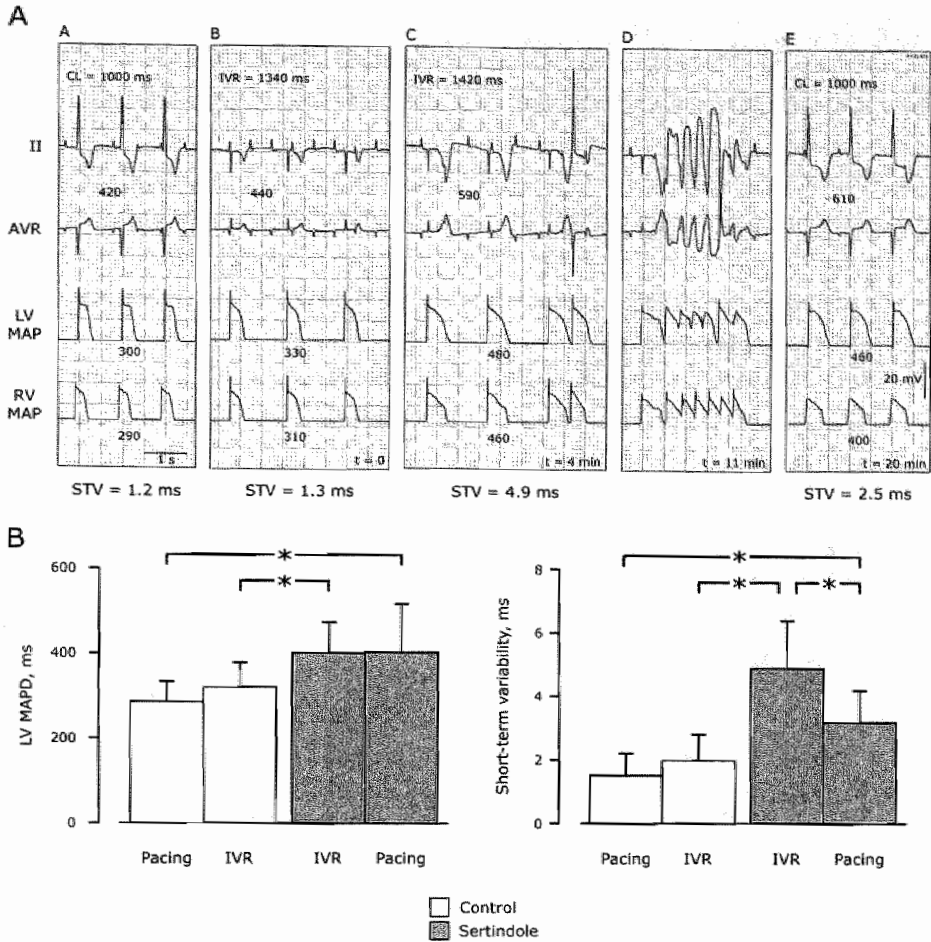
Short-term variability (upper panel) and TdP incidence (lower panel) in sertindole experiments (1.0 mg/kg) with and without potassium pretreatment ( $n = 7$ ). An elevated plasma-potassium concentration has no effect on baseline STV, however it prevents sertindole-induced elevation of STV and the occurrence of TdP. \*,  $P < 0.001$  versus baseline; †,  $P < 0.05$  versus potassium pretreatment.



**Figure 4**

**A:** Proarrhythmia frequency (upper left panel), LV MAPD (upper right) and STV (lower left) at control (C), under the influence of sertindole (S, 1.0 mg/kg), and after administrative frequency of 3 and 10  $\mu\text{g/kg}$  levocromakalim, respectively. \*,  $P < 0.05$  versus sertindole.

**B:** Representative Poincaré plots from the same dog at the four different time points from A. Sertindole increases LV MAPD, STV and induces TdP while 3  $\mu\text{g/kg}$  levocromakalim prevents further TdP, decreases STV but leaves the LV MAPD prolonged. Following 10  $\mu\text{g/kg}$  levocromakalim, the repolarization time is also decreased.



**Figure 5**

**A:** Electrophysiological changes during a representative experiment employing sertindole (1.0 mg/kg) to induce TdP and pacing to prevent further arrhythmia. Two ECG leads (1 mV/cm), LV and RV MAP recordings are shown in each panel at a paper speed of 1 cm/s. Paced cycle length (CL) or idioventricular rhythm (IVR) is shown at the top. QT interval and MAPD are below each signal. Time (t) is relative to start of sertindole administration. STV is noted under each panel. In the control situation (panel B) with an RR interval of 1340 ms and during pacing with a CL of 1000 ms (panel A), STV were low and comparable. Sertindole administration prolonged repolarization, increased STV, induced extrasystoles (panel C), consequently precipitating TdP (panel D). When CL was decreased to 1000 ms, TdP was temporarily prevented and STV decreased along with minor changes in the duration of repolarization (panel E).

**B:** Composite data from 6 experiments where CL was shortened by pacing to suppress TdP. Pacing-induced prevention of TdP was associated with a decrease in the STV, however the LV MAPD remained as long as before extrasystolic activity. \*,  $P < 0.05$ .



*Preventing reappearance of TdP by right ventricular pacing*

At baseline, QT intervals, LV MAPD and STV decreased non-significantly by shortening the ventricular cycle length from  $1398 \pm 207$  to  $1000$  ms (Figure 5). Sertindole prolonged repolarization both at idioventricular rhythm and at  $1000$  ms paced cycle length. Without pacing, sertindole-induced TdP in 5 of 6 dogs, which was momentarily abolished by pacing. When pacing was discontinued, TdP reappeared in all experiments. A representative example of such an experiment is illustrated in Figure 5A. When the effect of pacing was compared to the non-paced period preceding the first drug-induced extrasystole, the QT ( $489 \pm 72$  versus  $486 \pm 89$  ms), LV MAPD (Figure 5B), RV MAPD ( $370 \pm 76$  versus  $351 \pm 77$  ms) and  $\Delta$ MAPD ( $45 \pm 36$  versus  $52 \pm 45$  ms,  $P = \text{NS}$  for all) were all similar. Only the STV was reduced ( $4.9 \pm 1.5$  to  $3.2 \pm 1.0$  ms,  $P < 0.05$ ; Figure 5B) as a consequence pacing.

**Discussion**

In this study, we demonstrated by using various interventions that increasing or decreasing BVR determined the proarrhythmic outcome. BVR proved superior to other repolarization-prolongation parameters in predicting TdP inducibility well before the proarrhythmia precipitated, making prevention feasible.

*Proarrhythmic increase in BVR*

The risk of TdP in humans and animal models is inversely correlated to the ventricular repolarization reserve. As such, the concept of repolarization reserve has been used to describe the inability of the heart to withstand additional challenges on repolarization.<sup>2,8</sup> Based on novel insights, classical electrophysiological parameters such as QT-interval or MAPD prolongation are not capable of detecting repolarization reserve.<sup>1-6</sup> Recently, we have suggested BVR as a concept closely associated with repolarization reserve. This parameter is superior to other repolarization-lability parameters and to the static repolarization parameters in predicting drug-induced TdP in anesthetized dogs with CAVB.<sup>2</sup> So far, beat-to-beat variability of repolarization induced by two class-III drugs (*d*-sotalol and amiodarone) and an anti-stroke compound (NS-7) have been reported.<sup>2,15</sup> In anesthetized CAVB dogs ( $n = 20$ ), baseline STV was  $2.6 \pm 1.1$  ms in the first experiments and  $2.7 \pm 0.8$  in their second experiment ( $P = 0.8$ ), illustrating the

stability of the parameter over time in the CAVB dog. In the present study, baseline STV was at this level (Table 1, Figures 3-5).

The dose-dependent proarrhythmic properties of the antipsychotic drug sertindole were compared to verify that BVR is capable of predicting differences in the induction of TdP by non-cardiovascular drugs. We have shown that sertindole is a selective blocker of  $I_{HERG}$  and native canine  $I_{Kr}$ , which translates into prolongation of repolarization in vitro and in vivo.<sup>1</sup> Although 0.2 and 1.0 mg/kg sertindole gave rise to comparable prolongation of repolarization in sinus-rhythm dogs as well as CAVB dogs, only the high dose induced TdP in the remodeled hearts of the CAVB dogs.<sup>1</sup> This study confirms the presence of elevated STV before the onset of ventricular extrasystoles and minutes before arrhythmia (Figure 5).

The only QT-prolonging drug devoid of BVR increase known to us is amiodarone. At doses below proarrhythmic threshold, *d*-sotalol, NS-7 and sertindole all show non-significant trends towards increasing BVR. Although the results of lower plasma concentrations of the drugs do not show a significant increase in STV, a small elevation could bear important information when drugs are evaluated for latent proarrhythmic potentials.

#### *Potassium levels and repolarization reserve*

Baseline levels of plasma potassium were unexpectedly low in these CAVB dogs ( $2.8 \pm 0.2$  mmol/L).<sup>16</sup> It appear to be a characteristic of these dogs rather than of the AV block, since control dogs in sinus rhythm have similar low levels of potassium ( $2.4 \pm 0.5$  mmol/L;  $n = 6$ ;  $P = \text{NS}$  versus CAVB). In earlier studies with anesthetized CAVB dogs, we have observed higher levels ( $4.2 \pm 0.5$  mmol/L;  $n = 8$ ), excluding the possibility of anesthesia-induced low potassium.<sup>17</sup>

Raising the potassium levels by KCl infusion did not change the ventricular electrophysiological parameters, including RR, QT, QRS or STV (Figures 2 and 3), although T-wave morphology did show slight changes, suggesting an effect of potassium on repolarization (Figure 2B). Overall, we do not consider the pretreatment associated with (toxic) hyperkalemia.

Increasing extracellular potassium concentrations in vitro results in a slower inactivation of  $I_{Kr}$ , thereby enhancing repolarization strength.<sup>18</sup> Humans with adequate cardiac repolarization reserve show no change in QT intervals upon a modest increase in plasma potassium. Only patients with acquired or congenital long-QT syndromes who experience elevation of potassium concentrations, respond by shortening their QT intervals.<sup>19-21</sup> The absence of QT shortening in CAVB dogs, would suggest a physiologically normal repolarization reserve, which is contradicted

by the pathological susceptibility to proarrhythmic drugs and an STV of  $2.6 \pm 1.1$  ms, which is significantly higher than dogs without cardiac electrical remodeling ( $1.3 \pm 0.3$  ms).<sup>13</sup> The behavior of repolarization lability in long-QT patients and controls receiving potassium is unknown. Nevertheless, increasing repolarization reserve by KCl in this study was not recognized in the sertindole-induced prolongation of repolarization parameters, but by controlled STV and reduced proarrhythmia.

It has been shown that drug affinity to the  $I_{Kr}$  channel is altered when potassium concentrations are changed.<sup>18,22</sup> We have no data suggesting if this is also the case in sertindole-treated CAVB dogs, however, since QT prolongation was similar after 1.0 mg/kg sertindole with and without potassium pretreatment, we assume that altered binding kinetics play a minor role in our findings.

### *Decreasing BVR and proarrhythmia*

Earlier we have described that levocromakalim possesses electrophysiological and antiarrhythmic properties presumably by  $I_{K,ATP}$  activation, leading to QT shortening, a decrease in BVR and effective prevention of TdP.<sup>2,23,24</sup> The experiments reported here employed a titration of levocromakalim in order to potentially separate QT abbreviation and BVR reduction and to elucidate which of the two had the closest association to TdP induction. In Figure 4, data is presented that clearly shows a significant decrease in proarrhythmia accompanied by a decrease in STV following 3  $\mu$ g/kg levocromakalim. This was neither accompanied by shortened repolarization (QT interval or LV MAPD) nor by decreased interventricular dispersion of repolarization.

Figure 5B shows a small but non-significant decrease of STV at baseline as a consequence of steady-state pacing at an increased rate. However, when the same pacing is performed under circumstances of sertindole-induced prolonged repolarization, elevated BVR and proarrhythmia, a significant decrease in BVR is noted. Again this was accompanied by a reduction in TdP incidence, but not by an abbreviation of the prolonged repolarization. The latter, which is not the anticipated frequency-dependent response of repolarization, could be due to the relatively slow heart rates at which the repolarization times are determined in this study. In this frequency range, the repolarization has a rather horizontal relationship with heart rate.

Although not statistically significant, administration of sertindole tend to increase RR intervals while levocromakalim tend to decrease the RR interval, raising the question of the influence of heart rate on STV. The longest RR intervals were

seen during the combined influence of potassium and sertindole, which was not associated with elevated STV. Confirming earlier findings, there was no correlation between the RR intervals and STV ( $P = 0.36$ ) in these experiments. Relating fixed cycle-length pacing at control and under the influence of sertindole, also illustrates the rate-independence of STV within the physiological range of heart rates in the CAVB dog. Hence, when controlling for the bradycardic effect inherent to  $I_{Kr}$  blockers, BVR is still increased by proarrhythmic drugs. Furthermore, decreasing the ventricular frequency by pacing under drug-free circumstances did not lead to a significant decrease in STV (Figure 5B). Further experiments will be designed to scrutinize the effects of faster pacing on STV.

### *Clinical implications*

This study shows that manipulation of BVR was the only determinant for the induction of TdP arrhythmia in anesthetized CAVB dogs. This opens the possibility in clinical studies to assess whether BVR can be advantageous in identifying the patient at risk of developing drug-induced TdP. Limiting the increase in BVR may be an effective therapy against increased proarrhythmic risk.

### *Study limitations*

This study limits BVR to invasive, endocardial MAP recordings in anesthetized dogs with high susceptibility for drug-induced TdP. In the present state of our knowledge no adequate explanation can be given for the mechanisms responsible for BVR.

### *Conclusions*

Influencing BVR is feasible in vivo. Interventions that decrease BVR do also suppress proarrhythmia. Conversely, when BVR is critically increased, TdP is likely to ensue. This study confirms once more, that prolongation of repolarization is not proarrhythmic *per se*. BVR proves as a superior marker for the prediction and prevention of drug-induced TdP.

### **Acknowledgments**

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## General Discussion

*Content:*

Introduction

Multiple challenges on the repolarisation reserve

Electrophysiological parameters

Why yet another measure for variability?

Possible mechanisms of beat-to-beat variability of repolarisation duration

Challenges ahead





## Introduction

In 1966, Dessertenne first used the name *torsades de pointes* to describe a polymorphic ventricular tachycardia in a woman with atrioventricular block.<sup>1</sup> Despite major scientific efforts, the mechanisms underlying this potentially lethal cardiac arrhythmia are still not fully understood. Drug-induced *torsades de pointes* were later identified as a serious side-effect of medical treatment. Large efforts from the pharmaceutical industry, academic scientists and regulatory authorities are aimed at identifying precarious drugs before they are introduced to the market. Nevertheless, the methodology behind the testing is neither standardised nor perfect. Abundant results have advocated the need to assess drugs on multiple levels of complexities before a risk/benefit analysis of the potential drug can be made. In chapter 2, we assessed the electrophysiological and proarrhythmic properties of a drug on multiple levels of complexity, from cloned ion-channel to proarrhythmic animal model. Presently, the developing international guidelines on the testing of drugs are concerned with the aspect of delayed repolarisation, which *per se* is not dangerous. Only when multiple predisposing factors are present simultaneously, *torsades de pointes* can precipitate. In chapter 2, we also showed that *torsades de pointes* were only initiated under the concurrent existence of electrical remodelling and high drug dosing. These aspects reflect on a hypothesis that has become known as the hypothesis of the multiple hits on repolarisation reserve. Indeed, this deserves to be incorporated in the developing guidelines. Identification of early parameters predicting proarrhythmic events has long been a medical aspiration. In addition, these parameters can be beneficial in the proarrhythmic assessment of drugs. The availability of new additional surrogate markers for *torsades de pointes* is essential.

## Multiple challenges on the repolarisation reserve

The low incidence of torsades de pointes in healthy humans is likely linked to a strong repolarisation. In chapter 3, we suggest a description of the concept of repolarisation reserve<sup>2</sup> in which we regard it as *the ability of a heart to withstand a challenge on repolarisation*. Thus, the healthy individual can withstand serious challenges on repolarisation. Metabolic or electrolyte disturbances, heart disease and other underlying pathologies can induce acquired QT prolongation, whereas the inherited forms of channelopathies are grouped under the congenital long-QT syndromes. However, a patient with a long-QT syndrome does not necessarily have a prolonged QT on the ECG.<sup>3-6</sup> Both patients with congenital long-QT syndromes and those with acquired QT prolongation are expected to have a lower repolarisation reserve and thus will be more vulnerable to additional repolarisation challenges.<sup>7,8</sup> In this assumption, the different repolarising potassium channels have an overlapping or compensating relationship, in order to safeguard repolarisation. A pharmaceutical agent blocking such a repolarising current can result in drug-induced QT prolongation, regarded as an additional challenge on repolarisation, increasing the risk of torsades de pointes.

Various laboratories have investigated this assumption and attenuated repolarisation by introducing multiple consecutive pharmacological agents.<sup>9-13</sup> Table 1 summarizes several studies in which two potassium currents ( $I_{Kr}$ ,  $I_{Ks}$  or  $I_{K1}$ ) were blocked individually and simultaneously. The investigations were performed in tissues from healthy dogs, so it is assumed that repolarisation at baseline was physiological strong. A single challenge prolonged the action potential considerably in all incidences, however interestingly, the combined challenge increased action potential duration far more than would be expected from simple summation of the two individual effects.

The synergistic relationship of multiple hits is applicable to the clinical situation, where the patient with an already acquired or congenital decreased repolarisation reserve encounters an additional challenge and eventually passes the threshold to potentially develop torsades de pointes. In the person with a sufficient repolarisation reserve this additional challenge would hardly be noticed.

This clinical scenario underscores the importance of including models of reduced repolarisation reserve in the assessment of proarrhythmic potentials of novel treatments. As stated in chapter 1, some models are already available. The studies that served as the basis for thesis employed the use of the dog with chronic complete atrioventricular block, in which the individual components of a decreased repolarisation reserve are well documented.<sup>14-24</sup>

## Electrophysiological and proarrhythmic parameters

A serial, dose-dependent assessment of electrophysiological and proarrhythmic properties of drugs provides several advantages. When the animal serves as its own control, biological variation is decreased. Reproducibility of baseline values can be evaluated and the predictive values of parameters can be assessed with greater certainty. Dose- or concentration-dependent drug effects are basic characteristics of the majority of chemicals affecting a receptor or an ion channel. For example, a pure  $I_{Kr}$  blocker will prolong the cardiac action potential in a concentration dependent manner until  $I_{Kr}$  is fully blocked and no further effect is seen. The effect of dofetilide on action potential duration in isolated canine ventricular myocytes in chapter 2 is an example of such a characteristic. Well-known exceptions from this concentration dependency are found in drugs with multiple actions underlying the measured effect. When the drug has effects on more than one ion channel, all of these effects will be incorporated into the response of the action potential. This can result in amplification, an early plateau effect or even a bell-shaped concentration-response curve of the action potential prolongation.<sup>25</sup> Examples of bell-shaped response curves are reported for multifaced drugs like ranolazine, quinidine, terfenadine and cisapride.<sup>26-31</sup>

**Table 1.** Multiple pharmacological hits on repolarisation reserve.

Preparation	$I_{Kr}$ block	$I_{Ks}$ or $I_{K1}$ block	Combined block	Reference
Tissue slices	100%	10% ( $I_{Ks}$ )	160%	9
Transmural wedges	10%*	20% ( $I_{Ks}$ )	110%*	9
Papillary muscles	25%	5% ( $I_{Ks}$ )	47%	10
Papillary muscles	50%	10% ( $I_{Ks}$ )	90%	11
Papillary muscles	30%	20% ( $I_{K1}$ )	100%*	11
Papillary muscles	9%	14% ( $I_{K1}$ )	35%	12
Isolated myocytes	130%	0% ( $I_{Ks}$ )	217%*	13

Two different repolarising currents were blocked either individually or simultaneously. All studies were performed in canine ventricular tissue. Relative prolongation in action potential duration from baseline is noted. Asterisks indicate the presence of early afterdepolarisations.

Throughout the experimental planning for the previous chapters, the importance of serial, dose-dependent investigations was taken into account. Dose-dependent investigations were performed with sertindole (chapters 2 and 6), *d*-sotalol (chapter 3) and NS-7 (chapter 4). In addition to altering the dose, we also decreased the infusion rate by increasing the infusion time of a fixed dose of NS-7 (chapter 4).

The electrophysiological and proarrhythmic characteristics of these drugs in anaesthetised dogs with chronic atrioventricular block are summarised in Table 2. In this table, the electrophysiological and proarrhythmic effects of the three drugs are summarised and compared to a single dose of dofetilide. At baseline, a high reproducibility of all electrophysiological parameters is present. The drugs are all able to induce torsades de pointes in this model when administered at high dose or fast delivery. The classical electrophysiological parameters (upper part of Table 2) include QT intervals, and left and right ventricular monophasic action potential duration (MAPD). Listed are the averaged absolute values attained at baseline and with the drug administered. With only one exception, are none of these parameters able to differentiate between the proarrhythmic outcomes of the studies. Only with *d*-sotalol are the right ventricular MAPD increased with the high proarrhythmic dose while it was not increased after the low and less proarrhythmic dose. In no instance is there a significant difference between drug-induced effects of the two doses/rates. Also, when the absolute drug-induced increases are compared, none of the effects are significantly different from the other administration protocols (not shown). Hence, in these studies, the serial comparisons are not able to discriminate the hazardous dose based on the repolarisation parameters QT interval, left or right ventricular MAPD.

The lower half of Table 2 covers some of the novel proarrhythmic predictors employed in this thesis. The triggers inducing torsades de pointes have been attributed to early-afterdepolarisation dependent triggered activity observable on the ECG as extrasystoles.<sup>32</sup> In the analysis of the events leading to drug-induced torsades de pointes, regional dispersion of repolarisation, and single and multiple (see chapter 2) extrasystoles are often important players.<sup>15,19</sup> In no instance was the interventricular dispersion of repolarisation, calculated as the absolute difference between left and right ventricular MAPD, able to predict the proarrhythmic outcome. We measured the time duration from the start of drug administration to the occurrence of the first single and multiple extrasystoles to evaluate the aggressiveness of the treatment. Furthermore, we established the frequency of multiple extrasystoles. If prolongation of repolarisation is recognised as the substrate, these extrasystoles can be regarded as triggers, cumulatively increasing the likelihood of initiating torsades de pointes.<sup>32,33</sup> When the substrate is comparable in all incidences (upper part of Table 2), the occurrence and frequency of triggers may be a reasonable indicator for the likelihood of torsades de pointes to ensue. No differences between the time points of occurrence of extrasystolic activity (singles or multiples) are observable, partly due to a large variation between the experiments.

**Table 2.** Electrophysiological parameters from studies employing *d*-sotalolol, sertiindole, NS-7 or dofetilide in anaesthetised dogs with chronic atrioventricular block.

Drug	Dose	Infusion time, minutes	n <sub>dogs</sub>	TdP incidence	RR intervals, ms	QT intervals, ms	Left ventricular MAPD, ms	Right ventricular MAPD, ms
<i>d</i> -Sotalolol	2 mg/kg	5	8	25%	1272 ± 233 → 1405 ± 236	433 ± 40 → 511 ± 63 *	393 ± 39 → 457 ± 49 *	334 ± 34 → 367 ± 19
<i>d</i> -Sotalolol	4 mg/kg	5	8	75%	1258 ± 180 → 1501 ± 273 *	437 ± 49 → 527 ± 58 *	378 ± 58 → 464 ± 74 *	325 ± 49 → 373 ± 36 *
Sertiindole	0.2 mg/kg	5	9	0%	1384 ± 349 → 1407 ± 318	400 ± 60 → 474 ± 85 *	353 ± 51 → 416 ± 66 *	307 ± 37 → 354 ± 48 *
Sertiindole	1.0 mg/kg	5	13	77%	1427 ± 228 → 1503 ± 268	398 ± 60 → 496 ± 65 *	336 ± 48 → 427 ± 66 *	308 ± 43 → 370 ± 61 *
NS-7	3 mg/kg	60	5	0%	1257 ± 215 → 1372 ± 277	448 ± 31 → 493 ± 48	347 ± 11 → 408 ± 53 *	293 ± 30 → 342 ± 57
NS-7	3 mg/kg	5	6	50%	1242 ± 154 → 1299 ± 113	442 ± 47 → 478 ± 50	363 ± 48 → 418 ± 38 *	299 ± 33 → 343 ± 34
Dofetilide	25 µg/kg	5	29	76%	1189 ± 194 → 1308 ± 225 *	380 ± 60 → 475 ± 82 *	317 ± 50 → 392 ± 75 *	289 ± 43 → 338 ± 73 *

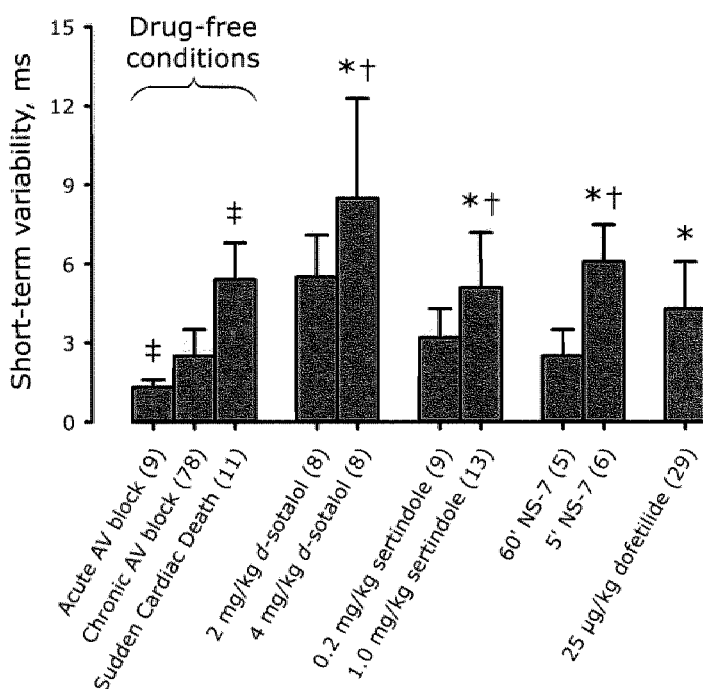
  

Drug	Dose	TdP incidence	Interventricular dispersion of repolarisation, ms	Time to first single extrasystole, minutes	Incidence of multiple extrasystoles	Time to first multiple extrasystole, minutes	Number of multiple extrasystoles in 10 minutes	Left ventricular STV, ms
<i>d</i> -Sotalolol	2 mg/kg	25%	59 ± 27 → 87 ± 48	6 ± 3	6 of 8	10 ± 4	2 ± 5	3.5 ± 1.5 → 5.5 ± 1.6
<i>d</i> -Sotalolol	4 mg/kg	75%	52 ± 26 → 91 ± 48	6 ± 5	8 of 8	5 ± 4	16 ± 24	3.0 ± 0.7 → 8.6 ± 3.8 *†
Sertiindole	0.2 mg/kg	0%	46 ± 36 → 62 ± 27	7 ± 3	0 of 9	-	0 ± 0	2.3 ± 0.8 → 3.2 ± 1.1
Sertiindole	1.0 mg/kg	77%	27 ± 29 → 57 ± 45	4 ± 3	11 of 13	4 ± 2	14 ± 15 †	2.3 ± 0.7 → 5.1 ± 2.1 *†
NS-7	3 mg/kg	0%	55 ± 32 → 72 ± 12	20 ± 12	0 of 5	-	0 ± 0	2.1 ± 0.2 → 2.5 ± 1.0
NS-7	3 mg/kg	50%	63 ± 39 → 74 ± 43	5 ± 2	4 of 6	7 ± 3	9 ± 20	2.6 ± 0.3 → 6.0 ± 1.4 *†
Dofetilide	25 µg/kg	76%	38 ± 27 → 60 ± 48 *	3 ± 1	26 of 29	4 ± 2	21 ± 19	2.4 ± 1.1 → 4.3 ± 1.8 *

Absolute values ± SD before and after drug administrations are indicated. \*,  $P < 0.05$  versus baseline; †,  $P < 0.05$  versus lower dose or infusion rate. MAPD, monophasic action potential duration; TdP, torsades de pointes; STV, short-term variability. Two-way ANOVA was used for comparing dose dependent changes in electrophysiological parameters, while a one-way ANOVA was used for the effects of dofetilide. Numbers of multiple extrasystoles were compared with a Mann-Whitney rank sum test. All parameters were similar at baseline. All drugs were administered intravenously. Electrophysiological parameters were measured before the occurrence of the first drug-induced extrasystole. TdP incidence indicates susceptible dogs relative to group size.

Nevertheless, the absence of multiple extrasystoles after administrations devoid of arrhythmia indicates some predictive value.

The last column of Table 2 summarises the importance of short-term variability of repolarisation observed with the different administration regimens. Contrary to the other repolarisation parameters listed in the table, there are significant differences in short-term variability between proarrhythmic and non-proarrhythmic challenges. This is also the case, when the absolute drug-induced increases are compared (not shown). Thus, it seems to be possible to predict proarrhythmic consequences based on this parameter. Figure 1 graphically compares the short-term variability from Table 2 and chapter 5.



**Figure 1**

Short-term variability (STV) in anaesthetised dogs with chronic atrioventricular block at baseline and under the influence of various cardiovascular and non-cardiovascular drugs. Group sizes are indicated in brackets. Sudden cardiac death refers to a subpopulation of dogs with chronic atrioventricular block that dies suddenly (chapter 5). Both *d*-sotalol and sertindole were analysed in two different doses (5-minutes infusion, chapters 2, 3 and 6), while NS-7 (3 mg/kg) were administered over 60 or 5 minutes (chapters 4). Dofetilide was only tested in one dose. \*,  $P < 0.05$  versus chronic atrioventricular block (serial comparison); †,  $P < 0.05$  versus other dose or rate; ‡,  $P < 0.05$  versus chronic atrioventricular block (group comparison).

To further analyse the proarrhythmic-predictive values of the nine electrophysiological parameters in Table 2, receiver-operator characteristics were plotted and the area under the curve quantified (Table 3). The different electrophysiological parameters at baseline or after drug administration were analysed for their ability to discriminate between experiments with torsades de pointes and those without. Collectively, this analysis includes 43 experiments with reproducible drug-induced torsades de pointes and 35 experiments without. The classical electrophysiological parameters like the QT interval along with left and right ventricular MAPD and interventricular dispersion of repolarisation are not satisfactory in predicting torsades de pointes. A crucial message protruding from the data is that inducing the arrhythmia itself should be a main objective of the assessment of proarrhythmic properties of drugs. The predictive value of multiple extrasystoles seems advantageous, especially the frequency within the first ten minutes. This is compatible with the theory of a comparable substrate in all experiments, while proarrhythmia is related to the frequency of triggers increasing the chance of precipitating runs of torsades de pointes. At baseline, short-term variability does not seem to be superior to the established electrophysiological parameters in predicting a proarrhythmic experiment irrespective of drug or infusion time. However, after the drug is administered, short-term variability is a useful indicator of arrhythmia to develop later on.

As part of the methodology, short-term variability is measured before the first drug-induced extrasystole, which is well in advance of the onset of the triggers (multiple extrasystoles) and torsades de pointes. Hence, in these studies, the earliest known parameter with superior predictive value is short-term variability.

**Table 3.** Proarrhythmic predictive values of the parameters analysed in Table 2.

	Baseline	Drug
RR intervals	0.61	0.61
QT intervals	0.53	0.63
Left ventricular MAPD	0.56	0.58
Right ventricular MAPD	0.46	0.46
Interventricular dispersion	0.49	0.56
Time to 1st single extrasystole	-	0.55
Time to 1st multiple extrasystole	-	0.80
Number of multiples in 10 minutes	-	0.93
Short-term variability	0.58	0.79

Calculated are the areas under the curves of the receiver-operator characteristics for 78 experiments of which 43 showed torsades de pointes.



## Why yet another measure for variability?

Various formulas, algorithms and methods for quantifying variability within a series of measurements are available in the scientific literature. Best known is probably the standard deviation. Specifically for the measure of temporal lability of repolarisation duration, a few other measures have been proposed. In 1997, Berger reported on the QT-variability index<sup>34</sup> while Hondeghem described instability of the action potential in 2001.<sup>35</sup> There are specific discrepancies between the methods. Advantages and limitations should be considered, when the decision is made of which formula to employ. Table 4 summarises the differences between the QT-variability index, instability and short-term variability as presented in this thesis.

There are important differences between these measures of lability and alternans of repolarisation. Alternans is typically occurring at fast ventricular frequencies, has a repetitive T wave or action potential morphology and is mechanistically coupled to intra- and intercellular calcium cycling.<sup>36-39</sup> Lability of repolarisation including beat-to-beat variability is present at slower heart rates and seems chaotic in appearance. Moreover, the underlying mechanism is far less elucidated.

**Table 4.** Comparison of three selected methods for quantifying lability of repolarization.

	<b>QTVI</b>	<b>Instability</b>	<b>STV</b>
Signal	ECG	MAP	MAP
Time duration	5 min	3 min	<1 min
Application	Clinical	Non-clinical	Non-clinical
Consecutiveness in methodology*	-	-	+
Invasive	-	+	+
References	34,40-42	35,43-46	Chapters 3 to 6

\* Beat-to-beat variability of repolarisation analyses the direct difference between two consecutive beats, whereas non-consecutive algorithms disregards or reorder the sequence of beats. QTVI, QT variability index; STV, short-term variability; MAP, monophasic action potentials.

QT-variability index represents the logarithmic ratio between the QT-interval and heart-rate variances, each normalised by their squared means. About 5 minutes ECG is recorded, in which ventricular premature complexes are deleted. Patients with dilated cardiomyopathy,<sup>34,40</sup> ischemia,<sup>41,42</sup> or survivors of sudden cardiac arrest<sup>41</sup> have increased QT variability index.

Instability of the action potential duration to 60% repolarisation ( $APD_{60}$ ) is calculated using the last 20 action potentials each minute for 3 minutes during

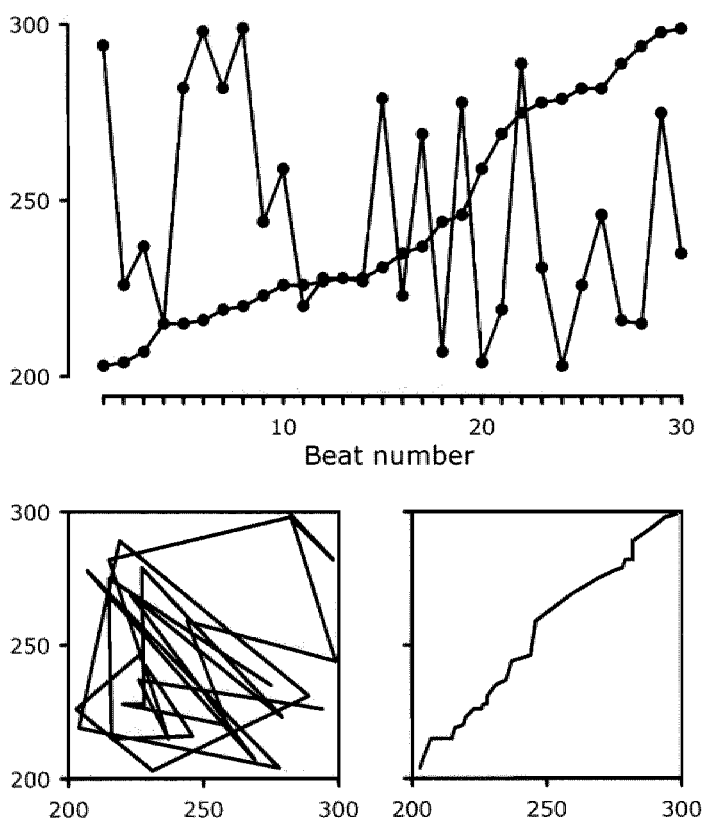
steady-state pacing at a cycle length of 1000 ms. The APD<sub>60</sub>s are then sorted after duration and fitted by linear regression. The instability is the difference between the upper and lower quartile estimates from the regression. The measure is traditionally used on isolated Langendorff-perfused rabbit hearts to predict proarrhythmic potentials of perfused drugs.<sup>35,43-46</sup>

Short-term variability derives from Poincaré plots, which is a simple way to look for deterministic relationships in complex time series. In these plots, the present state (e.g. an APD) is plotted against the previous state (i.e. the former APD). Slow uniform changes tend to follow the line-of-unity, while abrupt changes, e.g. an extrasystole with a short APD, deviates from the diagonal and produces a triangle. More serious multiple extrasystoles and arrhythmias cause polygons on the Poincaré plot. Short-term variability has been defined as *the dispersion of points perpendicular to the line-of-identity*<sup>47</sup> or simply as the average distance of the points to the diagonal. This measure is used on anaesthetised dogs with chronic atrioventricular block to predict proarrhythmic potentials of administered drugs (chapters 3, 4 and 6) and to assess antiarrhythmic interventions or preventions (chapter 6). Furthermore, it is increased in electrically remodelled canine hearts (chapter 5). In these studies, the Poincaré plots were drawn and the short-term variability were calculated before the onset of extrasystolic activity to dissociate drug-induced beat-to-beat variability of repolarisation from extrasystole-induced changes in repolarisation.

To compare the importance of consecutiveness in the methods a theoretical example is presented. Thirty random numbers, artificially representing repolarisation duration of 30 consecutive ventricular complexes, were generated. In the example, aspects of heart-rate changes are not included. Two scenarios were made in which the first characterizes high lability with the random order of points conserved. In the second scenario, consecutiveness is disregarded and the random numbers were ordered from low to high. Figure 2 shows a graphical representation of the two series of identical numbers. Table 5 compares data calculated using the 30 numbers. Obviously, the mean is identical, however also the standard deviation is the same, since it is based on the calculation of variance, which ignores consecutiveness. QT variability is based on variance, so like the standard deviation, it is identical in the two series. The example serves to illustrate the importance of consecutiveness, and since heart rate is defined to be constant, the aspect of heart-rate variability in the QT variability index is disregarded in the present example. Thus, this example should not be extrapolated to situations of physiologically significant heart-rate variability. The method of action-potential instability<sup>35</sup> orders the action potentials after their

duration, so the two series in this example become identical. The only measure that discriminates between the lability of the two series is the short-term variability. As illustrated in the left Poincaré plots of Figure 2, the random numbers make a large plot and the dispersion of points from the line-of-identity is considerable compared to the right Poincaré plot of the ordered points.

As this example is derived from artificially generated numbers, there is no connection to arrhythmia of any kind. Intuitively, the chaotic series is likely to be more proarrhythmic than the gradual “prolongation”, however this remains to be proven in an experimental set-up.



**Figure 2**

Artificially generated example to illustrate the importance of consecutiveness. Thirty numbers between 200 and 300 were created. Either the order was preserved or the series was ordered from lowest to highest. The upper graph illustrates the two series in time. The Poincaré plots below shows one number as a function of the former number for all 30 numbers. The plot to the left, which has the largest area, is derived from the series with conserved order, while the right graph illustrates the ordered numbers.

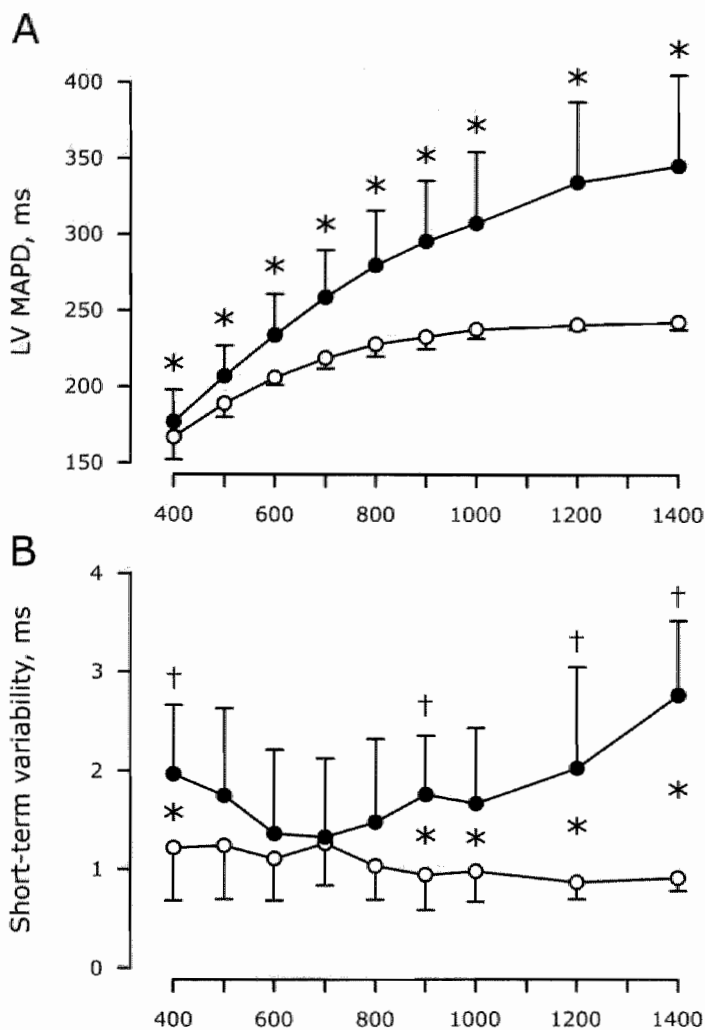
As discussed in the introduction, QT interval measurements are not very reproducible, since the return of the T wave to the isoelectric line is gradual. In that sense, transmembrane action potentials and to a certain limit also the monophasic action potentials are more reproducibly measured, when the duration to 90 or 95% repolarisation is determined. However in principle, the calculations of lability could be applied to all measures of repolarisation. The weakness of short-term variability at this point is that it is dependent on the availability of monophasic action potentials. Besides the invasive nature of monophasic action potential catheters, the recordings are not always as stable in time as one would wish. Throughout the preceding chapters, the minimally accepted amplitude of the monophasic action potentials was 15 mV. Below this amplitude, the signal was not accepted as a measure of the ventricular action potential duration. If the acceptance threshold is set too high, repetitive mechanical manipulation of the catheters is likely to be necessary, which often can induce extrasystoles, possibly influencing the variability measures.

**Table 5.** Comparison of some formulas for assessment of variability of the randomly chosen points of Figure 2.

	Random series	Ordered series
Mean	245	245
Standard deviation	31	31
QTV	-1.8	-1.8
Instability	51.5	51.5
STV	25.4	2.3

QTV:  $\log(QT_{\text{variance}}/QT_{\text{mean}}^2)$ . The linear regression used for instability analysis had an R-squared value of 0.95.

The formula for short-term variability does not include a normalisation for heart rate, which could be an influencing factor. Figure 3 summarises experiments at fixed heart rates in non-remodelled and remodelled anaesthetised dogs with atrioventricular block. The experiments confirm that the left ventricular monophasic action potential duration is rate dependent in both control dogs and in dogs with electrical remodelling. Due to the remodelling processes, the heart-rate dependence of the action potential duration is steeper at chronic atrioventricular block. In the dogs with acute atrioventricular block, short-term variability seems to be independent of heart rate. This reflects the non-remodelled state of the heart, although cardiac stretch and neurohumoral factors may be altered compared to the sinus-rhythm situation, possibly influencing short-term variability. In the remodelled situation at chronic atrioventricular block, the short-term variability is increased at

**Figure 3**

**A:** Left ventricular monophasic action potential duration as a function of paced cycle length at acute (open symbols) and chronic (closed symbols) atrioventricular block. Eight dogs under anaesthesia were paced (>2 minutes) from the right ventricle at acute and chronic atrioventricular block in a serial design.

**B:** Short-term variability of the same action potentials as in A. \*,  $P < 0.05$  acute versus chronic atrioventricular block; †,  $P < 0.05$  versus 700 ms paced cycle length in chronic AV block dogs.

short and long cycle lengths producing a “U” shaped curve. Interestingly, minimal short-term variability short and long cycle is present at paced cycle lengths representative of sinus rate (500 to 800 ms). The increase in short-term variability at 400-ms cycle length suggests a transition towards alternans. At slow cycle lengths, representative of the idioventricular rhythm of the chronic atrioventricular block dogs, there is an increased short-term variability due to remodelling. Thus, within a range of specific heart rates, short-term variability is dependent on ventricular frequency in the remodelled heart. This was used in chapter 6 to intervene with the proarrhythmic outcome of drug-induced torsades de pointes. Finally, the two graphs in Figure 3 propose that short-term variability is independent of the duration of the left ventricular monophasic action potential.

### **Possible mechanisms of beat-to-beat variability of repolarisation duration**

While it is reasonably well documented that repolarisation alternans is closely coupled to inefficient calcium cycling, the mechanism underlying beat-to-beat variability of repolarisation is far less investigated.<sup>37,38,48</sup> We know that beat-to-beat variability of repolarisation is inherent to both the single cardiomyocyte and in the intact heart (chapter 3). Short-term variability generally reaches larger values in the isolated myocytes compared to measures from the whole heart, compatible with a reduction in variability upon intercellular coupling.<sup>49</sup>

Variability of the action potential is likely to derive from an intrinsic stochastic behaviour of one or more ion conductances. Both in in-vivo and in-vitro experiments, beat-to-beat variability is available from the action potential already from 50% repolarisation (chapter 4) indicating that the determinant for the variability should be sought early in the action potential before the onset of fast repolarisation. This would be compatible with the theory that an early ionic current during the plateau (e.g.  $I_{Na}$ ,  $I_{to}$ ,  $I_{Cl}$  or  $I_{CaL}$ ) is mechanistically important. The variability induced by this early current would under normal circumstances be counteracted by currents aiding repolarisation reserve later in the action potential (e.g.  $I_{Kr}$ ,  $I_{Ks}$  or  $I_{K1}$ ). Hence, by blocking repolarising potassium channels, the observed increase in beat-to-beat variability would be unmasked (chapter 3 and references<sup>13,49</sup>). On the other hand,  $I_{Kr}$  or  $I_{Ks}$  block itself could also be the primary cause of beat-to-beat variability of repolarisation.

Using action-potential clamp techniques, we have suggested that variability in calcium-induced calcium release is not the primary cause of action potential variability.<sup>50</sup> However, chelating intracellular calcium reduce repolarisation variability,<sup>49</sup> suggesting that variability in calcium concentrations can induce action-

potential variability possibly through calcium-dependent currents.

Beat-to-beat variability is also decreased by blocking sodium channels.<sup>51</sup>

Intracellular sodium and calcium are tightly regulated by the sodium-calcium exchanger and the sodium-potassium pump, among others. The increased subsarcolemmal sodium concentrations observed in dogs with chronic atrioventricular block<sup>23</sup> along with an increased sodium-calcium exchange current<sup>20</sup> could then possibly explain the larger variability of repolarisation in these dogs (chapter 5).

Thus, it is conceivable that the source of beat-to-beat variability of repolarisation duration lies already in the beginning of the action potential. Additional research is essential before mechanisms can be advocated.

### **Challenges ahead**

Action potential prolongation is probably a prerequisite, but not a sufficient change of cardiac electrophysiology to render the heart susceptible to lethal arrhythmias. Conceivably, prolongation of the action potential is an adaptive safety factor that may even be antiarrhythmic. The levels of accompanying lability and possibly (micro-)spatial dispersion are vital in assessing the vulnerability of the heart. A central question in this thesis has been the evaluation of individual drugs. To which extent is the action potential prolonged, repolarisation reserve decreased and lability enhanced? The underlying basis for action potential prolongation has been elucidated to some extent, however large areas are still unknown. The fundamental in situ, ionic, molecular and genetic source of beat-to-beat variability of repolarisation is even more unexplored. Exciting challenges lie ahead for basic research.

Given the increased beat-to-beat variability of repolarisation in sudden-death prone dogs (chapter 5) together with the possibility to prevent approaching arrhythmia by limiting short-term variability of repolarisation (chapter 6) may create clinical beneficial options. For example, if beat-to-beat variability is detectable in the ventricles of proarrhythmic patients with pacemakers and if pacemakers could detect this variability, the pacemaker could engage antiarrhythmic modes (e.g. by increasing heart rate) once a certain variability threshold is reached. Another likely application is the monitoring of patients receiving infusions of a class-III antiarrhythmic drug to convert atrial fibrillation. Online beat-to-beat variability can be monitored (chapter 3) and precautions against developing torsades de pointes could be taken or assessment of interventional strategies could be performed (chapter 6). Although these examples approach clinical applicability, several

steps are still to be taken. For broad-based clinical utilization, the method would preferably employ a non-invasive signal, like the ECG. Thus, exciting challenges lie ahead for the clinical approach.

The present draft of the regulatory guideline on the safety assessment of new potential drugs encourages interested parties to develop and test proarrhythmic models and novel indices associated with torsades de pointes.<sup>52</sup> Certainly, there already exist well-described animal models with decreased repolarisation reserve that have an increased susceptibility to torsades de pointes. The pharmaceutical industry could benefit importantly from adopting these models and the proarrhythmic predictors that are available. The challenge for doctors, scientists, regulatory experts and industry is to revise current concepts and to surpass guidelines.



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## English Summary

The function of the ventricles of the heart is to mechanically drive blood through the vessels. The ventricles consist mainly of muscular tissue that contracts when activated. For contraction to act synchronised, electrical impulses control the rate and the sequential order of regional activation.

The muscle fibres of the ventricles consist primarily of cardiomyocytes, which are the heart-specific muscle cells. In every single myocyte electrical stimulation initiates an action potential. Charged ions flow through channels in the outer membrane of the cell, causing changes in the voltage difference over the membrane. Upon electrical stimulation of the cardiomyocyte, depolarisation followed by repolarisation shapes the action potential. The combination of all action potentials instigated throughout the heart is the basis of the electrocardiogram.

Changes in the force of depolarisation and/or repolarisation will change the shape of the action potential and when this occurs in a significant fraction of cardiac myocytes, the morphology of the electrocardiogram will change. The present thesis addresses changes in repolarisation, i.e. the electrical “relaxation” of the heart, as a cause of ventricular arrhythmia. If the ionic currents responsible for the repolarisation decrease, repolarisation is delayed, the action potential prolongs and so does the QT interval on the electrocardiogram. Repolarisation is an important cardiac event that enables the heart to be ready for the next cycle. Considerable reserve of the repolarising ion currents is normally present to secure that a fast electrical recovery is maintained. Inhibitions of these currents may deplete repolarisation reserve in such a way that the myocyte will be unable to remain electrical active and contribute to ventricular contraction. Furthermore, since the individual myocytes are intricately connected to each other, the failure of repolarisation in a cell will influence a neighbouring cell and can lead to the initiation of a premature action potential. The fast and timely generation of abnormal impulses may cause depolarising wave fronts that can initiate ventricular tachyarrhythmia. If the ventricles are susceptible to the initiated arrhythmia, it may be sustained. When the ventricular arrhythmia occurs in a setting of reduced repolarisation reserve it usually has a polymorphic appearance on the electrocardiogram with typical twisting around the baseline. If the preceding repolarisation is overtly prolonged this arrhythmia is called torsades de pointes. This term is pleasant for ear and describes a beautiful electrocardiographic feature. Unfortunately, torsades de pointes can be fatal when it deteriorates into ventricular fibrillation.

Decreases in repolarisation reserve can occur as acquired (heart disease, metabolic or electrolyte disturbances), congenital (inherited) or drug-induced syndromes. Pharmaceutical companies, regulatory authorities and scientific communities

are concerned with the latter one, because a number of drugs have been directly connected to a decrease in repolarisation reserve and a risk of lethal torsades de pointes to a level where the drugs are withdrawn from the market.

**Chapter 1** of the present thesis is the general introduction, which describes the current efforts to assess the proarrhythmic potential of drugs before they are tested in humans. Different levels of investigation are described, emphasizing the importance of evaluating potential repolarisation-dependent adverse effects on the level of individual ion currents, integrated action potentials and electrocardiograms. The deficiency of reliable electrophysiological parameters to predict proarrhythmia is discussed and the aims of the thesis are put forward.

In **Chapter 2** the cardiac electrophysiological properties of the antipsychotic agent sertindole are described. By decreasing the repolarisation reserve, sertindole is able to prolong the action potential and QT interval in normal dogs and in dogs with an acquired reduction in their repolarisation reserve. In the latter dogs, torsades de pointes are induced by high doses of sertindole. Thus, an important finding in this study is that ventricular electrical remodelling of the ventricles is a prerequisite for the induction of torsades de pointes. The dose-dependent difference in the induction of torsades de pointes is not reflected in a dose-dependent prolongation of repolarisation, confirming that QT prolongation *per se* is a poor predictor of torsades de pointes.

In **Chapter 3** a novel electrophysiological measure is proposed that is based on temporal differences rather than averaged values of repolarisation duration. The parameter beat-to-beat variability of repolarisation provides information whether the dose of the proarrhythmic agent *d*-sotalol will ultimately induce torsades de pointes in an experiment. Importantly, this information is available early in the experiment, well before the initiation of ventricular extrasystoles, thus enabling the prediction of torsades de pointes with stronger confidence.

In addition to investigating the dose of a proarrhythmic drug, we have also examined the rate of intravenous administration in the studies for **Chapter 4**. Decreasing the rate of infusion of the drug NS-7 creates lower peak blood concentrations of the agent and lesser proarrhythmia. At the same time, the QT interval is equally prolonged while beat-to-beat variability of repolarisation is able to predict differences in the proarrhythmic outcome.

Our historical registry of sudden cardiac death in dogs with ventricular electrical remodelling is analysed in **Chapter 5**. Dogs with a severely reduced repolarisation reserve are so vulnerable to proarrhythmic stimuli that they die suddenly in their cage. These dogs have a very high beat-to-beat variability of repolarisation, which corresponds to a higher incidence of torsades de pointes and sudden death.



Furthermore, alongside cardiac remodelling after atrioventricular block, the beat-to-beat variability of repolarisation increases.

In **Chapter 6** it is described how beat-to-beat variability of repolarisation can be manipulated. When a drug increases beat-to-beat variability, torsades de pointes are expected. Vice versa, when the variability is decreased from an already proarrhythmic level, torsades de pointes can be prevented or stopped.

Finally, in **Chapter 7** the results of all previous chapters are discussed in a wider perspective. The concept of repolarisation reserve is described and beat-to-beat variability of repolarisation is compared to traditional electrophysiological parameters and to other measures of repolarisation variability. Hypothetical mechanistic explanations based on the current knowledge are considered, concluding that additional research is necessary for the full understanding of this phenomenon at the cellular and ionic level. An important conclusion of this thesis is that pathological animal models of proarrhythmia are required for the assessment of proarrhythmia next to existing assays of drug-induced changes in ventricular repolarisation. Furthermore, it is plausible that the magnitude of beat-to-beat variability of repolarisation is closely associated with the amount of remaining repolarisation reserve.

## Nederlandse Samenvatting

De functie van het hart is ervoor te zorgen dat het bloed door de bloedvaten wordt gepompt. De ventrikels bestaan voornamelijk uit spierweefsel dat samentrekt als het geactiveerd wordt. Om de samentrekking georganiseerd te laten gebeuren, bepalen elektrische prikkels het hartritme en de volgorde van activering van bepaalde delen van het hart.

De spierbundels van de ventrikels bestaan voornamelijk uit hartspiercellen. In elke hartspiercel leidt een elektrische prikkel tot een actiepotentiaal. Geladen ionen gaan door kanalen in de buitenste membraan van de cel. Dit leidt tot een voltage verschil over het membraan. Na elektrische stimulatie van de hartspiercel ontstaat depolarisatie gevolgd door repolarisatie, er ontstaat een actiepotentiaal. Alle actiepotentialen van het hart samen vormen de basis voor het elektrocardiogram. Veranderingen in de sterkte van de depolarisatie en/of repolarisatie zullen de actiepotentiaal veranderen. Wanneer dit in een significant deel van de hartspiercellen gebeurt, zal de vorm van het elektrocardiogram veranderen. In dit proefschrift worden veranderingen in de repolarisatie (de elektrische relaxatie van het hart) aangewezen als een oorzaak van ventriculaire ritmestoornissen. Als de ion-stromen die verantwoordelijk zijn voor de repolarisatie afnemen, dan wordt de repolarisatie vertraagd. Hierdoor verlengen zowel de actiepotentiaal als het QT interval op het elektrocardiogram. Repolarisatie zorgt ervoor dat het hart weer tijdig "klaar" is voor de volgende samentrekking. Onder normale omstandigheden is voldoende repolarisatie-reserve stroom aanwezig, wat ervoor zorgt dat een snel elektrisch herstel gehandhaafd blijft. Afname van deze stromen kunnen de repolarisatie-reserve zodanig verstoren dat een hartspiercel niet in staat zal zijn elektrisch actief te blijven en bij te dragen aan ventriculaire contractie. Aangezien de hartspiercellen op een complexe manier aan elkaar gekoppeld zijn, zal de repolarisatiestoornis van één cel de omliggende cellen beïnvloeden en kan dit leiden tot het ontstaan van een vroegtijdige actiepotentiaal. Het snelle en vroegtijdige ontstaan van abnormale impulsen kan depolariserende golven veroorzaken die snelle ventriculaire ritmestoornissen tot gevolg kunnen hebben. Als de ventrikels gevoelig zijn voor de beginnende ritmestoornissen, dan zijn deze ritmestoornissen aanhoudend. Als deze ventriculaire ritmestoornis plaats vindt op basis van verminderd repolarisatievermogen, dan uit zich dit in het elektrocardiogram meestal "polymorf", met een kenmerkende draaiing rond de basislijn van het elektrocardiogram. Als de voorafgaande repolarisatie duidelijk verlengd is, dan noemt men deze ritmestoornis torsades de pointes. Deze mooi klinkende naam beschrijft een mooi elektrocardiografisch kenmerk van het hart. Helaas kan torsades de pointes echter dodelijk zijn als het eindigt in kamerfibrilleren.

Verminderde repolarisatie-reserve kan verschillende achtergronden hebben: het kan

verkregen zijn (hartziekte, metabole of elektrolytische veranderingen), aangeboren zijn (geërfd), of door medicijnen worden geïnduceerd. De geneesmiddelenindustrie, de overheid en wetenschappelijke instanties zijn bezorgd om de laatstgenoemde, aangezien van een aantal geneesmiddelen is aangetoond dat ze rechtstreeks de repolarisatie-reserve verminderen en op die manier het risico op torsades de pointes ritmestoornissen zodanig vergroten dat de geneesmiddelen van de markt moesten worden gehaald.

**Hoofdstuk 1** van dit proefschrift is de algemene introductie. Hierin worden de huidige pogingen beschreven die gedaan worden om het vermogen van medicamenten om ritmestoornissen te veroorzaken in kaart te brengen voordat deze op mensen worden getest. Er zijn al diverse onderzoeken beschreven die de nadruk leggen op het belang van het testen van mogelijke repolarisatie-afhankelijke nadelige effecten op ionkanaal-, actiepotentiaal- en electrocardiogramniveau. Het ontbreken van betrouwbare elektrofysiologische parameters die gevoeligheid voor ritmestoornissen kunnen voorspellen wordt in dit hoofdstuk bediscussieerd. Tevens wordt hier het doel van dit proefschrift beschreven.

In **Hoofdstuk 2** worden de elektrofysiologische eigenschappen van het antipsychotische medicament sertindole beschreven. In zowel normale honden als honden met een verkregen vermindering van de repolarisatie kan sertindole de actiepotentiaalduur en de QT tijd verlengen. In die laatste groep honden kan een hoge dosis sertindole torsades de pointes ritmestoornissen opwekken. Een belangrijke bevinding in deze studie is dan ook dat ventriculaire remodelering van de ventrikels vereist is voor het opwekken van torsades de pointes ritmestoornissen. Het dosis-afhankelijke verschil in het voorkomen van torsades de pointes ritmestoornissen is niet terug te vinden als een dosis-afhankelijke verlenging van de repolarisatie. Dit bevestigt dat QT-tijd verlenging alléén voor torsades de pointes ritmestoornissen een slechte voorspeller is.

In **Hoofdstuk 3** wordt een nieuwe elektrofysiologische maat voorgesteld die is gebaseerd op temporele verschillen in plaats van op gemiddelde waarden van repolarisatieduur. De parameter slag-op-slag variabiliteit van repolarisatie (*beat-to-beat variability of repolarisation*) geeft informatie over het feit of een dosis van het pro-aritmogene medicament *d*-sotalol uiteindelijk tot torsades de pointes zal leiden in een experiment. Het is van belang dat deze informatie op een vroeg punt in een experiment beschikbaar is, en wel vóór het ontstaan van extra ventriculaire slagen, om op deze manier met grote zekerheid torsades de pointes ritmestoornissen te kunnen voorspellen.

In **Hoofdstuk 4** wordt vervolgens de snelheid van intraveneuze toediening van pro-aritmische medicamenten onderzocht. Tragere infusie van het medicament

NS-7 levert lagere maximale bloedconcentraties van dit medicament op en minder ritmestoornissen. De QT tijd is hierbij gelijkmatig verlengd terwijl slag-op-slag variabiliteit van repolarisatie de verschillen in gevoeligheid voor ritmestoornissen kan voorspellen.

Onze historische registratie van plotse hartdood in honden met ventriculaire elektrische remodelering wordt geanalyseerd in *Hoofdstuk 5*. Honden met een ernstig verminderde repolarisatie-reserve zijn zo vatbaar voor pro-aritmogene stimuli, dat ze plotseling kunnen overlijden in hun hok. Deze honden hebben een zeer hoge slag-op-slag variabiliteit van repolarisatie, wat overeenkomt met een hogere incidentie van torsades de pointes ritmestoornissen en plotse hartdood. Verder groeit de slag-op-slag variabiliteit van repolarisatie naast de remodelering van het hart na compleet hartblok.

In *Hoofdstuk 6* wordt beschreven hoe slag-op-slag variabiliteit van repolarisatie kan worden gemanipuleerd. Als een medicament de variabiliteit van repolarisatie verhoogt, kunnen torsades de pointes ritmestoornissen worden verwacht. Door slag-op-slag variabiliteit van repolarisatie te verlagen van een pro-aritmogeen niveau tot een non-aritmogeen niveau, kunnen torsades de pointes ritmestoornissen worden voorkomen of gestopt.

Uiteindelijk zullen in *Hoofdstuk 7* de resultaten van alle voorafgaande hoofdstukken in een breder perspectief worden neergezet. Het concept van repolarisatie-reserve wordt beschreven en slag-op-slag variabiliteit van repolarisatie wordt vergeleken met traditionele elektrofysiologische parameters en met andere maten voor variabiliteit van de repolarisatie. Hypothetische mechanistische verklaringen, gebaseerd op de huidige kennis, zijn in overweging genomen, waarbij geconcludeerd wordt dat verder onderzoek noodzakelijk is om dit fenomeen volledig op cellulair en ionkanaalniveau te kunnen verklaren. Een belangrijke conclusie in dit proefschrift is dat pathologische pro-aritmogene diermodellen nodig zijn om aanvullende informatie te krijgen over pro-aritmogene eigenschappen van medicamenten, naast de reeds bestaande testen voor medicament-gerelateerde veranderingen in de ventriculaire repolarisatie. Verder is het zeer waarschijnlijk dat de grootte van de slag-op-slag variabiliteit van repolarisatie nauw gerelateerd is aan de aanwezige repolarisatie-reserve.

Dansk Resumé

Hjertekamrenes funktion er at pumpe kroppens blod gennem blodårerne ud til kroppen. Hjertekamrene består af muskulatur, der kontraherer når det aktiveres. For at kontraheringen er synkroniseret, kontrollerer elektriske impulser rytmen og den regionale rækkefølge af aktiveringen.

Muskelfibrene i hjertekamrene består af kardiomyocytter, der er specialiserede hjerte-muskelceller. En elektrisk impuls starter et aktionspotentiale i hver kardiomyocyt. Elektrisk ladede ioner strømmer gennem den ydre cellemembran, hvilket forårsager en ændring af spændingspotentialet over membranen.

Depolarisering efterfulgt af repolarisering former aktionspotentialet efter kardiomyocytten er blevet aktiveret. Alle aktionspotentialer initieret i hjertet er ophav til elektrokardiogrammet.

Ændringer i styrken af depolarisering og/eller repolarisering vil ændre formen af aktionspotentialet og når dette sker i tilstrækkeligt mange kardiomyocytter vil elektrokardiogrammet også ændres. Denne afhandling beskæftiger sig med ændringer i repolariseringen, med andre ord den elektriske "afslappelse" af hjertet, som baggrund for rytmeforstyrrelser i hjertekamrene. Hvis ion-strømmene, der er årsag til repolariseringen forringes, forlænges repolariseringen, hvilket bevirker at aktionspotentialet og QT intervallet på elektrokardiogrammet forlænges.

Repolariseringen er en vigtig del af hjertets rytme, fordi det medvirker til, at hjertet er klar til at pumpe den næste portion blod ud i kroppen. Betragtelig reserve af ion-strømme er normalt til stede, hvilket sikrer en hurtig repolarisering. Hvis ion-strømmene er nedsat kan reserven blive opbrugt således at kardiomyocytten bliver elektrisk inaktiv og dermed ikke er i stand til at bidrage til sammentrækningen af hjertemuskulaturen. Da alle kardiomyocytterne er tæt koblet til hinanden vil en celle, der ikke formår at repolarisere påvirke nabocellerne, hvilket kan give anledning til et for tidligt og usynkroniseret aktionspotentiale. Tidlige aktionspotentialer, der opstår på sårbare tidspunkter kan være ophav til depolariserende bølger, der kan starte en rytmeforstyrrelse. Hvis hjertekamrene er modtagelige for denne rytmeforstyrrelse, kan denne blive opretholdt. Hvis rytmeforstyrrelsen opstår i en situation, hvor repolariseringsreserven er nedsat har den typisk et polymorft udseende på elektrokardiogrammet med typiske drejninger omkring sin egen akse. Hvis den forudgående repolarisering er åbenlyst forlænget, kalder man rytmeforstyrrelsen torsades de pointes. Dette navn lyder godt og beskriver et flot elektrokardiografisk fænomen. Desværre kan torsades de pointes være dødbringende, hvis den forværrer til fibrillering i hjertekamrene.

Nedsat repolariseringsreserve kan være erhvervet (hjerte sygdomme, metabolit eller elektrolyt forstyrrelser), medfødt (genetisk disponering) eller medicin-induceret. Medicin industrien, sundhedsstyrelsen og videnskabelige grupper er interesserede

i de medicin-inducerede tilfælde af nedsat repolariseringsreserve, fordi en række produkter er blevet direkte forbundet med nedsat repolariseringsreserve og risiko for dødelig torsades de pointes til en sådan grad, at de er blevet taget af markedet.

**Kapitel 1** af denne afhandling er en general introduktion, der beskriver de undersøgelser, der bliver gjort før ny medicin bliver afprøvet i mennesker.

Forskellige undersøgelser bliver beskrevet med vægt lagt på at evaluere den ny medicins bivirkninger på repolariseringen på ion-strøm niveau, på aktionspotentiale niveau og på elektrokardiogram niveau. Mangelen på pålidelige elektrofysiologiske parametre, som kan forudsige rytmeforstyrrelser er diskuteret og målsætningen med denne afhandling er formuleret.

I **Kapitel 2** er de elektrofysiologiske bivirkninger af det antipsykotiske medicin sertindole beskrevet. Ved at nedsætte repolariseringsreserven kan sertindole forlænge aktionspotentialt og QT intervallet på elektrokardiogrammet i normale hunde og i hunde med erhvervet nedsat repolariseringsreserve. I de sidste hunde kan høje doser af sertindole starte torsades de pointes rytmeforstyrrelser. En vigtig konklusion i denne afhandling er, at et disponeret hjerte med nedsat repolariseringsreserve er nødvendigt for at inducere rytmeforstyrrelsen. Den dosis-afhængige torsades de pointes induktion er ikke reflekteret i den dosis-afhængige forlængelse af repolariseringen, hvilket bekræfter at QT forlængelse på elektrokardiogrammet er en upålidelig parameter når torsades de pointes skal forudsiges.

**Kapitel 3** beskriver en ny elektrofysiologisk parameter, som er baseret på tidsafhængige forskelle i stedet for gennemsnitlige værdier for repolarisering. Den nye parameter kaldes slag-til-slag variabilitet af repolarisering (*beat-to-beat variability of repolarisation*) og informerer om, hvorvidt en dosis af det rytmeforstyrrende medicin *d-sotalol* giver rytmeforstyrrelser senere i undersøgelsen. Denne information er tilstede tidligt i undersøgelsen, før de tidlige aktionspotentialer opstår, og man er således i stand til at forudsige torsades de pointes med større sikkerhed.

Foruden at undersøge dosis-afhængigheden af et rytmeforstyrrende medicin, undersøgte vi også effekten af at ændre hastigheden af intravenøs administration i studierne bag **Kapitel 4**. Ved at nedsætte infusionshastigheden af medicinen NS-7 fik vi lavere blodkoncentrationer af dette stof og færre rytmeforstyrrelser. Samtidigt var forlængelsen af repolarisering ens, mens slag-til-slag variabiliteten af repolariseringen kunne forudsige, hvorvidt rytmeforstyrrelser ville blive induceret. Vores historiske arkiv af pludseligt hjertestop hos hunde, der er disponeret for hjerterytmeforstyrrelser, er analyseret i **Kapitel 5**. Hunde med stor nedsættelse af repolariseringsreserven er så sårbare overfor rytmeforstyrrende stimuli, at de får hjertestop i deres bure. Disse hunde har en meget høj slag-til-slag variabilitet



af repolariseringen, hvilket er i overensstemmelse med højere risiko for torsades de pointes og pludseligt hjertestop. Endvidere øges slag-til-slag variabiliteten af repolariseringen samtidigt med, at hundene bliver disponeret for rytmeforstyrrelser efter atrio-ventrikulær blokade.

I **Kapitel 6** beskrives, hvorledes slag-til-slag variabiliteten af repolariseringen kan ændres. Torsades de pointes er forventet, hvis en medicin øger slag-til-slag variabiliteten af repolariseringen. På den anden side, hvis slag-til-slag variabiliteten af repolariseringen bliver nedsat fra et højt rytmeforstyrrende niveau, kan torsades de pointes forebygges eller stoppes.

Til sidst, i **Kapitel 7** er resultaterne fra de forgående kapitler diskuteret i et bredere perspektiv. Repolariseringsreserven som koncept er beskrevet og slag-til-slag variabiliteten af repolariseringen er sammenlignet med traditionelle elektrofysiologiske parametre og andre metoder til at måle variabilitet af repolarisering. Hypotetiske mekanistiske forklaringer baseret på den tilstedeværende viden er drøftet, konkluderende at yderligere forskning er nødvendig før slag-til-slag variabilitet af repolarisering kan forstås på cellulært og ion-strøm niveau. En vigtig konklusion af denne afhandling er, at patologiske dyremodeller for rytmeforstyrrelser er et nødvendigt supplement til eksisterende undersøgelser af medicin-forårsaget ændringer af hjertets repolarisering. Endvidere er det sandsynligt at graden af slag-til-slag variabilitet af repolarisering er tæt forbundet med mængden af tilbageværende repolariseringsreserve.

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# Curriculum vitae

June 25th, 1975	Born in Aarhus, Denmark
1994 - 1997	Bachelor of Science (Biology), University of Aarhus, Denmark
1997 - 2000	Master of Science (Human Biology), University of Copenhagen, Denmark
2001 - 2005	PhD, Department of Cardiology, Cardiovascular Research Institute Maastricht, Maastricht University, Netherlands
2003 - 2005	PhD, Department of Medical Physiology, Heart Lung Centre Utrecht, Utrecht, Netherlands



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